

Neuromuscular Junction Transmission is Effected by Quantum Entanglement of Ion Transition States

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Abstract

Neuromuscular Junction (NMJ) is the place where the neuron meets with muscle fiber crating a synapse to propagate the electrochemical signals. The infolds of the endplate of muscle fiber play a vital role containing a huge number of sodium channels in contraction of NMJ transmission mechanism. We have studied here the entanglement of sodium channel activation particle ('m' particle). Through the simulation results we confirm that the entanglement of 'm' particle effects the initiation time, amplitude and the rate of change of membrane potential.

1 Introduction

The junction between the terminal of a motor neuron and a muscle fiber where the neurons meets to ensure a rapid and efficient transmission of an action potential into depolarization of the postsynaptic target muscle by transmitting electro chemically excitation and causing the muscle to contract is called the Neuromuscular Junction (NMJ). The mechanism of neurotransmitter conduction has studied extensively [1-6]. At the NMJ the presynaptic neuron carries the impulse and the postsynaptic membrane undergoes a potential change eventually triggering the action potential. The opening of voltage-dependent calcium channels causes the release of neurotransmitters (ACh) that diffuse at the synaptic cleft and bind with Acetylcholine Receptors (AChR) causing inflow of sodium ions and outflow of potassium ions generating the end-plate synaptic potential (EPSP) at the post-synaptic membrane initiating an action potential [7].

The flow of current along the synaptic cleft (15–200 nm, [8]) affects the local extracellular potential, in turn affecting the voltage-dependent processes in the adjacent membranes. This phenomenon of current flow through weakly opened Na⁺ channels causing potential drop at the extracellular space by boosting channels activation and positive feedback. According to this hypothesis, the drop of the voltage which is generated the cleft may modify the voltages across the muscle membrane which affects the conductance of voltage-gated ion channels, thus increasing the probability of opening the voltage-gated ion channels. [9]

At NMJ a motoneuron meets muscle fibres creating a synapse to control the muscle contraction, in turn our movements. This electrochemical signal based communication takes place by activating and inactivating the ion channels at the junction's adjacent membranes. The large density of voltage gated sodium channels at the postsynaptic infolds plays the most vital role to stimulate the synaptic activation. [7, 8, 10]

The Hodgkin-Huxley Model (HHM) is the most widely accepted physiological model of single neuron. It describes the permissive and non-permissive states of the voltage gated ion channels and their mechanisms [11]. The classical HHM is a rate theory model that deal with gating particles of role playing ions. The rate theory model incorporating the atomic determination of the ion molecules may improvise the classical concept. Bernroider et al [12] has modified the classical HHM sodium ion gating probability to three similar but independent quantum correlated probabilistic mechanism where the sodium ion gating states during conduction are involved in entanglement of different degree of freedom. The incorporation of entanglement in sodium channel probability leads the gating mechanism slow down or rise.

In this work a realistic model mimicking the transmission process of NMJ was considered. This model takes into account the flow of current at junction due to the weakly opened sodium channels which affects the voltage-dependent processes at the adjacent membranes and boosts the postsynaptic membrane potential by a positive feedback. The sodium channel kinetics was calculated using the classical HHM using realistic physiological parameters. Entanglement of activation particles (m-gating) in terms of their quantum distribution was introduced using quantum theoretic approach which was adopted from Bernroider et al [12]. A current clamp simulation was performed to study the entanglement of Na⁺ channel activation particle effects on action potential properties. The entangled relationship of m-gating particles changes the Na⁺ channel activation by modifying sodium-ions activity in the voltage dependent ion-channels. Due to the change in the activation profile, the sodium current generated in the muscle endplate is changed which modifies the junction potential of the cleft. The subsequent result is the change of the cleft resistivity and action potential dynamics during the NMJ transmission process.

2 The model and parameters

The NMJ was designed using a 50 μm diameter and 500 μm long barrel shaped muscle fiber. Physiological parameters of rat NMJ were used in simulating the transmission process.

A circular axon terminal of 10 μm radius (a_j) [8] was connected to the muscle fiber membrane ($7.85 \times 10^{-8} \text{ m}^2$) to mimic the synapse. The maximum conductance (g_{jm}) of voltage-gated sodium channels at the endplate was determined considering 9 pS / channel [13] with a channel density of 3700 channels/ μm^2 [14].

The potential at the neuromuscular junction cleft (V_j) is calculated iteratively using equation 1 from the G_{jm} and other contributors, such as V_j itself, the sodium-specific reversal potential V_0 (50 mV) [10], the global resistance of the cleft (R_j) (eq. 5), the intracellular potential (V_m) (Fig. 1).

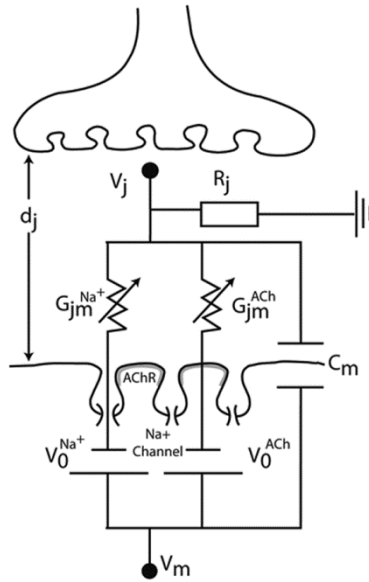


fig. 1. Equivalent electrical model of the NMJ. R_j , global resistance of the synaptic cleft; d_j , pre-to-postsynaptic membrane distance; G_{jm} (AChR) and G_{jm} (Na_v), global membrane conductances of AChR and Na_v channels at the endplate with related reversal potentials V_0 (AChR) and V_0 (Na_v); C_m , membrane capacitance; V_m , muscle fiber intracellular potential.

$$V_{j+1} = G_{jm} \times R_j \frac{V_m - V_j - V_0}{1 + (R_j \cdot G_{jm})} \quad (1)$$

The global sodium conductance (G_{jm}) of the otonuron and the sodium conductance (g_{jm}) at the endplate are computed using eq. 2 and eq. 3, respectively.

$$G_{jm} = g_{jm} \cdot \pi a_j^2 \quad (2)$$

$$g_{jm} = \bar{g}_{jm} \cdot m^3 \cdot h \quad (3)$$

The endplate sodium current (EPI_{Na}) is calculated by eq. 4, where E_{Na} is the Nernst equilibrium potential.

$$\text{EPI}_{\text{Na}} = G_{jm} \cdot (V_m - V_j - E_{\text{Na}}) \quad (4)$$

The global resistance R_j (eq. 5) is derived using cable equation and point contact model [9, 15-18].

$$R_j = \frac{r_j}{z_0^2 \pi} \left(\frac{24z_0^2 + 2z_0^4}{192 + 24z_0^2 + z_0^4} \right), z_0 = a_j \sqrt{r_j \cdot g_{jm}}, r_j = \frac{\rho_j}{d_j} \quad (5)$$

The AChR current (I_{AChR}) (eq. 6), generated in the cleft is modeled as a double exponential function.

$$I_{\text{AChR}} = C_j \cdot V_m \cdot \left(\exp\left(-\frac{t}{\tau_d}\right) - \exp\left(-\frac{t}{\tau_r}\right) \right) \quad (6)$$

C_j is the total AChR conductance at the cleft (59.1 pS / channel [19]). The number of active AChRs is 10000 AChR channels / μm^2 [19]. We considered 2% of the channels open at the time of synaptic activation with decay and rise time constants are τ_d and τ_r (0.564 & 0.162 ms, respectively [20]).

As shown in fig. 1, the I_{AChR} together with the EPI_{Na} act as stimulus current (eq. 7) to carry out the Hodgkin-Huxley speculation for triggering an action potential (eq. 8).

$$I_{\text{stim}} = I_{\text{AChR}} + \text{EPI}_{\text{Na}} \quad (7)$$

$$V_m = -1/C_m \cdot (I_{\text{Na}} + I_{\text{K}} + I_{\text{L}} + I_{\text{stim}}) \quad (8)$$

Where the membrane capacitance C_m is 4 $\mu\text{F} / \text{cm}^2$ [14]. The sodium, potassium and leakage current are calculated using classical Hodgkin-Huxley formalism [11] using \bar{g}_{Na} (45 mS/ cm^2 [10]), \bar{g}_{K} (29.9 mS/ cm^2 [21]), \bar{g}_{L} (1 mS/ cm^2) as the maximum conductances, and E_{Na} (45 mV [10]), E_{K} (-73 mV [21]), E_{L} (-90 mV [14]) as the reversal potentials for sodium, potassium, and leakage, respectively.

Adopting the quantum entanglement of sodium ion activation particle from Bernroider et al [12] the degree of freedom of ' m ' particle is redefined as

$$0 \leq \delta^2 \leq \frac{1}{1-3m+3m^2} \quad (9)$$

To have the quantum mechanical correction for the HHM, the term ' m^3 ' is replaced by the term $\delta^2 m^3$. Another variable ' k ' is incorporated to control the degree of freedom. $k=0$ is the classical HHM condition without any entanglement and the positive values of k results an increased conduction rate of sodium channels. $k=1$ is the maximum positive entanglement with $\delta^2 = \frac{1}{1-3m+3m^2}$. In the case of negative entanglement the term k is defined as $k := \delta^2 - 1$. So,

$$\text{Case I: if } k \geq 0, \quad \delta^2 = 1 + k \frac{3m(1-m)}{1-3m(1-m)}$$

$$\text{Case II: if } k < 0, \quad \delta^2 = 1 + k$$

3 Simulated results and discussion

Voltage-clamp experiments were simulated in MATLAB through scripting (version: R2009b; www.mathworks.com).

At the rat NMJ to simulate the action potential 400nA/cm² constant current was applied for different k (fig 2). For $k=0$ (classical HHM situation) it takes 2.9 ms to reach the threshold of -57.37 mV to initiate the action potential and reaches the maximum of 35.5 mV at 3.75 ms. Whereas for $k=1$ (maximum positive entanglement) it reaches the threshold (-60.66 mV) at 2.665 ms and maximum (39.5 mV) at 3.285 ms.

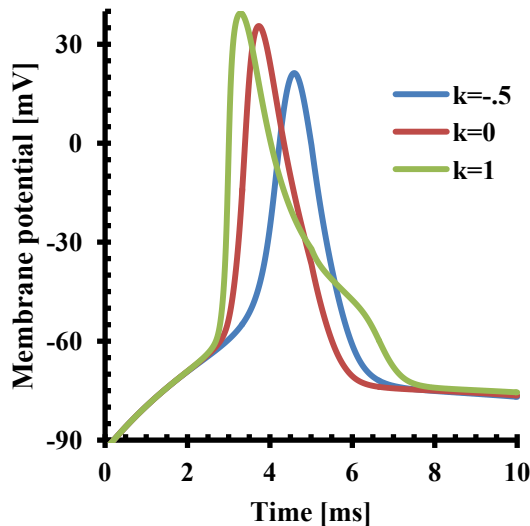


Fig 2: Action potential generated at the NMJ for different value of k .

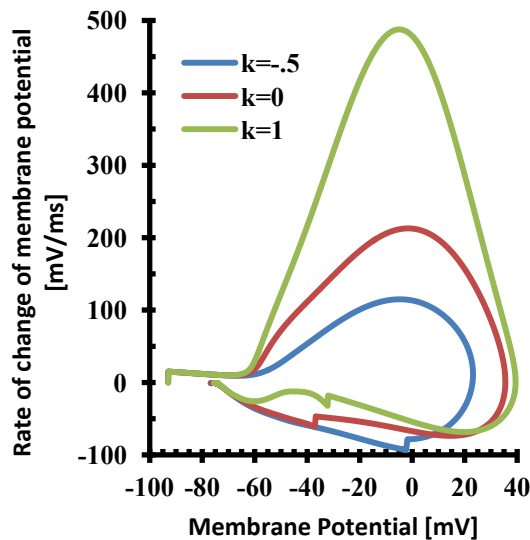


Fig 3: Phase plot for different value of k .

Figure 3 is showing the phase plot of the rate of change of membrane potential. For maximum positive entanglement ($k=1$) the maximum rate of rise of action potential is 487.4 mV/ms. In the classical HHM case ($k=0$) this is 212 mV/ms.

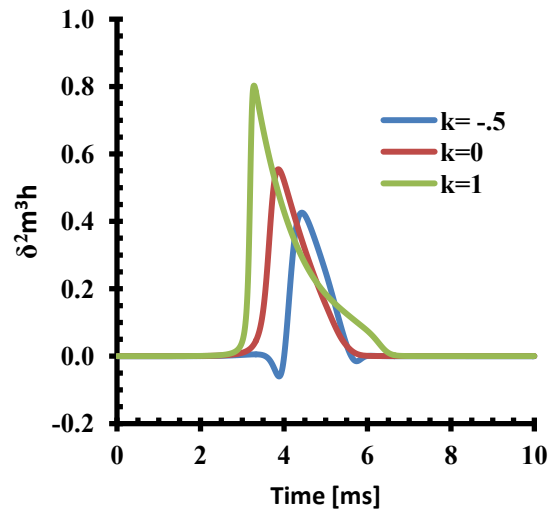


Fig 4: Resulting probability ($\delta^2 m^3 h$) of sodium channel gating kinetics for different value of k .

According to the classical HHM, the sodium channel contains three identical, rapidly responding, activation gates of type 'm' and a single, slower responding, inactivation gate of type 'h'. Therefore, $m^3 h$ is the resultant probability of the sodium channel opening at any time instant. In our case incorporating the entanglement of the activation gates of type 'm' the resultant probability is $\delta^2 m^3 h$. Figure 4 is showing the resultant probability of the sodium channel gating kinetics for different degree of freedom. At $k=0$, the maximum resultant probability is 0.5724 at 3.62 ms where as this is 0.814 at 3.08 ms for $k=1$. And for negative entanglement the maximum resultant probability is 0.414 at 4.45 ms.

From this simulation results it is clear that in the case of maximum positive entanglement the action potential initiates at a 5% less threshold value and to reach the peak amplitude it takes 13.5% less time than classical HHM condition. For $k=-0.5$ it is showing the reverse effect. The rate of change of membrane potential simulation is also showing the similar consequences. From the resultant probability simulation it shows that in the case of maximum positive entanglement it is 17.5 % faster and 42.3 % more activation than the classical HHM case.

The earlier and faster onset at positive entanglement condition in principle is exhibiting the higher reliability and more efficiency of transmission mechanism. The entangled relationship of m-gating particles changes the Na⁺ channel activation by modifying sodium-ions activity in the voltage dependent ion-channels. Due to the change in the activation profile, the sodium current generated in the muscle endplate is changed which modifies the junction potential of the cleft. The subsequent result is the change of the cleft resistivity and action potential dynamics during the NMJ transmission process.

4 Conclusion

Till today the Hodgkin-Huxley model is the most biophysically realistic and meaningful model to mock-up from a single neuron to a large neural network. The voltage-dependent ion-channels cause an action potential to be initiated. According to the classical HHM, the sodium channel contains three identical, rapidly responding, activation gates of type 'm'. In this work, we have presented a realistic NMJ model taking into account the quantum entanglement of the activation particles that modifies the channel kinetics, in turn the transmission process of the NMJ. This effect may play a role in designing efficient artificial NMJ for neuroprosthetic applications.

5 References

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