

Polarization Gating based on Mueller matrices

Angel Lizana,^{a,*} Albert Van Eeckhout,^a Kamil Adamczyk,^a Carla Rodríguez,^a Juan Carlos Escalera,^a Enric Garcia-Caurel,^b Ignacio Moreno,^c Juan Campos^a

^aUniversitat Autònoma de Barcelona, Grup d'Òptica, Physics Department, Bellaterra, Spain, 08193

^bLPICM, CNRS, École Polytechnique, Université Paris-Saclay, Palaiseau, France, 91128

^cUniversidad Miguel Hernández, Dept. of Materials Science, Optics and Electronics Technology, Elche, Spain, 03202

Abstract. We present mathematical formulae generalizing polarization gating techniques. Polarization gating refers to a collection of imaging methods based on the combination of different controlled polarization channels. In particular, we show how using the measured Mueller matrix of a sample, a widespread number of polarization gating configurations can be evaluated just from analytical expressions based on the Mueller matrix coefficients. We also show the interest of controlling the helicity of the states of polarization used for polarization gating based metrology, as this parameter has an impact in the image contrast of samples. In addition, we highlight as well the interest of combining polarization gating techniques with tools of data analysis related to the Mueller matrix formalism, such as the well-known Mueller matrix decompositions. The method discussed in this work is illustrated with the results of polarimetric measurements done on artificial phantoms and real *ex-vivo* tissues.

Keywords: polarization gating, Mueller matrix, biological tissue, polarimetric image contrast.

*First Author, E-mail: angel.lizana@uab.es

1 Introduction

In the last decades, polarimetric information has proven to be useful for biological tissues inspection [1-3]. As a result, polarimetric based techniques are nowadays being applied in multiple scenarios, as for instance, for cancer detection and stage identification [4-8], to enhance image contrast in skin diseases [9-11], for human eye examination [12, 13], for diabetes diagnosis as well as therapy [14, 15], etc.

There are different ways to extract sample information from polarimetric measurements (as surface roughness, tissue spatial inhomogeneities, biological material recognition, optical properties of turbid tissues, tissue depth metrology, sub-surface examination, etc.), as well as to enhance the contrast of images taken from the sample. A widespread polarimetric technique

applied for biological tissues inspection is the so-called Polarization Gating (PG) [16-20]. In essence, PG techniques exploit the fact that samples respond differently depending on the polarization state of the light used to probe it. The basic PG configuration consists of using linear polarization for illumination and detection (Linear Polarization Gating, LPG) stage. Then, LPG images can be combined to provide a new processed image, for instance by subtracting the images captured with parallel and with crossed polarizers. To further improve image contrast, recent studies have provided the interest of generalizing LPG techniques with the use of elliptical polarization, i.e., Elliptical Polarization Gating (EPG) [17, 19].

Another group of polarimetric methods are based on the measurement of the Mueller matrix (MM) of the sample, and the subsequent analysis of the polarimetric content encoded in the corresponding 16 real MM coefficients [21]. These techniques, which provide in principle a different polarimetric approach than those given by PG techniques, are used by a number of authors for biological tissue inspection [5, 7, 8, 12, 13].

In this paper, we demonstrate that information provided by polarization gating techniques can be alternatively obtained from the experimental Mueller matrix of the sample. In particular, we derive an analytical expression which consists of a linear combination of different Mueller coefficients and we show how a set of PG configurations can be considered as particular cases of the derived analytical expression. The desired PG configuration is then obtained by properly tuning some control parameters, as the azimuth or the ellipticity of the input and analyzing states of polarization. In addition, we highlight the interest of using Mueller matrices measurements instead of particular PG configurations. Firstly, thanks to the MM based analytical expression we provide in this work, we can extract the polarimetric information of a sample corresponding to multiple polarization gating configurations without the necessity of experimentally measuring

each one of them. Instead of this, only the measurement of the experimental Mueller matrix of the sample is required with our method. Secondly, Mueller measurements not only allow building a more general analytical expression, but also give access to extra channels of data processing, such as those provided by the different product Mueller matrix decompositions schemes [21-23] or even further, by applying recently developed methods as those based on the differential Mueller matrix [21, 23-26].

The method proposed in this paper is experimentally tested by using an imaging Mueller matrix polarimeter based on Liquid Crystal panels. This allows the system to dynamically perform the experimental measurements without the necessity of mechanical movements. The commutation rate of the used Liquid Crystal panels is of ~ 60 Hz, and the exposure time of the CCD camera used to register the intensity images is adapted for each sample analyzed to capture the maximum intensity without saturating the camera (the exposure time range used for measurements is between 0.004 and 0.12 seconds). With this experimental configuration, full polarimetric measurements can be done in few (0.4 to 2.2) seconds, which may be of interest in real-time applications. Indeed, if the methods discussed in this manuscript would be considered to be applied for real-time applications, the experimental set-up could be further optimized by using ferro-electric liquid crystal displays or photo-elastic modulators [27, 28]. Another interesting application for the methods discussed here is standard scanning microscopy adapted to polarimetric metrology. If these latter applications should to be performed in real-time, the high-speed imaging Mueller polarimeter provided in Ref. [29] can be used, which works at the time scale of a scanning microscope.

In a sense, we think that the methods proposed in this work bring together two mathematical tools for polarimetric sample analysis (PG and MM based methods) that traditionally have been unlinked and may be of interest in biological applications [16-20, 30-32].

The outline of this manuscript is as follows. In Section 2, we first briefly describe some of the more commonly used PG configurations (Sec. 2.1). Afterwards, in Sec. 2.2, we derive a general expression based on the Mueller matrix coefficients of the studied sample, from which the different PG configurations described in Sec. 2.2 become individual solutions. In particular, each different PG configuration is achieved from the proposed general expression by properly tuning two control parameters in the mathematical formula, these parameters representing the azimuth and ellipticity values of the polarizations illuminating and analyzing the sample. In Section 3, we describe the optical scheme used to measure the Mueller matrix of different samples, from which different PG configurations are achieved (Sec. 3.1). In addition, the description of the different samples inspected in this work is also provided (Sec. 3.2). In Section 4, we provide the equivalence between standard PG and PG configurations obtained from MM metrology (Sec. 4.1). Next, in Sec. 4.2 we highlight the interest of combining PG configurations with well-known MM analytical tools. Finally, the main conclusions of the work are given in Section 5.

2 Polarization gating configurations derived from Mueller matrix data

In this section we briefly describe some Polarization Gating (PG) configurations currently used for tissue inspection and we discuss some of the strengths and drawbacks related to them (Sec. 2.1). The nomenclature used to label the different PG configurations described in this subsection 2.1 is that followed in Ref. [19]. Afterwards, we derive an analytical expression that consists on a linear combination of different functions which depend on several of the MM coefficients of the

measured sample (Sec. 2.2). Note that such relation can be interpreted as a generalization of multiple PG configurations.

2.1 Polarization gating techniques

When polarized light interacts with biological tissues, the characteristics of the produced scattered light strongly depend on different parameters, such as the sample molecules size, the polarization of the input light, the wavelength, the sample depth probed, among others.

One typical measuring configuration (let us call it as configuration C1), consists in illuminating the analyzed sample with linear polarization and to project the scattered light to the same input polarization (i.e., parallel polarizer-analyzer). When illuminating the sample with a linear polarization, a mixed contribution of different kind of photons is observed when measuring out of the ballistic direction [19, 33]. We can subgroup them as photons reflected at the tissue surface (surface-reflected photons, S_L), photons penetrating to the sub-surface but maintaining the original polarization (polarization maintaining photons, P_L), and photons reaching deeper layers of the sample, and which are fully depolarized by multiple scattering events (depolarized photons, D_L).

Therefore, the C1 configuration leads to a mixture of all these three kinds of S_L , P_L and D_L photons contributions. However, as P_L photons are those that usually provide the most significant information of the studied sample, different strategies can be applied to remove the image background and to improve the image contrast, by eliminating as much as possible the non-desired S_L and D_L contributions. To this aim, some authors have proposed to combine the C1 configuration with a second measurement where the sample is illuminated with linear polarized light and scattered light is imaged through the corresponding orthogonal linear polarization (cross linear configuration, here labeled as C2). Images recorded by using the C2 configuration

(crossed polarizers) are mainly based on D_L photons, because P_L and S_L photons are efficiently filtered by the linear analyzer [19]. Under this scenario, by simply performing the difference $C1-C2$ (let us call this PG configuration as Linear Configuration, LConfig), we obtain polarimetric images which are only due to P_L and S_L photons (D_L photons are removed), and thus, the image quality is improved when compared with $C1$ configuration by itself. However, by using the LConfig, the contribution of S_L photons still degrades the image contrast to a certain extent.

To improve the final image, recent studies have suggested the interest of generalizing Linear Polarization Gating (LPG) with the use of elliptical polarization, i.e., Elliptical Polarization Gating (EPG) [19, 33-35]. In particular, EPG present two main benefits when compared with LPG. First, elliptical states change the sense of rotation by surface-reflection, and thus, specular reflection is eliminated by using a co-elliptical configuration for detection. Second, elliptically polarized light holds its polarization state for a larger number of scattering events than linearly polarized light, so it is suitable to study sub-substrate structures [19]. In particular, when illuminating a sample with an elliptical polarization out of the ballistic direction, a mixed contribution of photons (elliptical polarization maintaining photons, P_E ; and depolarized photons, D_E) are observed for a co-elliptical configuration (let us call it configuration $C3$) [19, 33]. Note that by using the co-elliptical configuration S_E photons are removed because they undergo a change in helicity by reflection [19, 35]. On the other hand, by using a cross-elliptical configuration (i.e., illuminating with a given elliptical polarization and detecting with the orthogonal one; configuration $C4$), a mix of surface-reflected elliptical photons, S_E , and D_E photons are obtained, as P_E photons are removed in the cross-elliptical configuration [19, 35]. Thus, analogously to the LPG case (LConfig), by simply subtracting the $C3$ and $C4$ channels (i.e., $C3-C4$), the obtained images are mainly produced by P_E and S_E photons, as the non-desired

contribution of D_E photons is removed by subtraction. Let us label this PG configuration (C3-C4) as Elliptical Configuration (EConfig). Nevertheless, by using the EConfig the contribution of S_E photons is still present and degrades somewhat the final image contrast.

Other PG approaches can be found in literature to improve the final image contrast. For instance, a clever approximation is derived in Ref. [19]. The authors provide an analytical function that combines the above-described (C1-C2) and (C3-C4) PG configurations. This leads to a mixture of surface reflected and polarization maintaining photons from linear and elliptical polarizations ($P_L+S_L+P_E-S_E$). Note that in general, the flux for the S_L and S_E photons is different, because of the portion of input light projected to the plane of incidence is different for the linear and elliptical polarization cases. However, by normalizing the amount of reflected light projected in the plane of incidence for the elliptical to that of the linear channel by a factor β , such that $S_E=\beta S_L$, the influence of S_L and S_E photons in the final processed image can be avoided. In particular, this function, here labeled as function f , can be calculated as follows [19],

$$f = (C3 - C4) + \beta (C1 - C2) , \quad (1)$$

where the numerical parameter β corrects the differences in the amount of light projected to the components parallel (p -polarized) and perpendicular (s -polarized) to the plane of incidence when using different ellipticities for the input state of polarization. This parameter β has to be experimentally determined for each particular elliptical configuration (C3-C4) applied in the function f [19].

Note that by using the function f , the photons contributing on the final image are mainly those maintaining the polarization, P_L and P_E photons, while the background, related to D_L , D_E , S_E and S_L photons, is removed.

2.2 Polarization Gating configurations described using the Mueller matrix formalism

In this section we derive an analytical expression, which depends on several MM coefficients, that allows performing a number of polarization gating configurations by properly setting a few control parameters. To this aim, we adopt the well-known Stokes-Mueller formalism [21, 22]. Accordingly, the state of polarization of a fully, partial or un-polarized light beam is described by four intensity values, usually arranged in column-form in the so-called Stokes vector. In turn, the polarimetric response of any sample can be described by its 4x4 MM, whose 16 real coefficients encode the polarimetric information of the sample. In this framework, a MM can be understood as the polarization transfer function of the medium and the interaction of light with the medium is described by the following linear system [21, 22],

$$S_{out} = M S_{input} = \begin{pmatrix} m_{00} & m_{01} & m_{02} & m_{03} \\ m_{10} & m_{11} & m_{12} & m_{13} \\ m_{20} & m_{21} & m_{22} & m_{23} \\ m_{30} & m_{31} & m_{32} & m_{33} \end{pmatrix} \begin{pmatrix} S_0 \\ S_1 \\ S_2 \\ S_3 \end{pmatrix}, \quad (2)$$

where m_{ik} are the coefficients of the MM and S_i are the different channels of the Stokes vector.

When dealing with fully polarized light beams, the normalized Stokes vector can be written as a function of the polarization angles of the polarization ellipse, i.e., the azimuth (α) and the ellipticity (ε) angles [22],

$$S = \begin{pmatrix} 1 \\ \cos 2\varepsilon \cos 2\alpha \\ \cos 2\varepsilon \sin 2\alpha \\ \sin 2\varepsilon \end{pmatrix} \quad (3)$$

Note that by properly selecting the values for α and ε in Eq. (3), any fully polarized state of polarization can be described. According to Eqs.(2) and (3), when a fully polarized light beam

interacts with a sample, the state of polarization S_{out} of the output (transmitted, reflected or scattered) light beam can be written as,

$$S_{out} = \begin{pmatrix} m_{00} + m_{01} \cos 2\varepsilon \cos 2\alpha + m_{02} \cos 2\varepsilon \sin 2\alpha + m_{03} \sin 2\varepsilon \\ m_{10} + m_{11} \cos 2\varepsilon \cos 2\alpha + m_{12} \cos 2\varepsilon \sin 2\alpha + m_{13} \sin 2\varepsilon \\ m_{20} + m_{21} \cos 2\varepsilon \cos 2\alpha + m_{22} \cos 2\varepsilon \sin 2\alpha + m_{23} \sin 2\varepsilon \\ m_{30} + m_{31} \cos 2\varepsilon \cos 2\alpha + m_{32} \cos 2\varepsilon \sin 2\alpha + m_{33} \sin 2\varepsilon \end{pmatrix} \quad (4)$$

Afterwards, we can project (i.e., analyze) this output light beam, S_{out} , on a polarization detector system setting a polarization analyzer (let us call it S_{PSD}) equal to the input polarization (i.e., that set in Eq. (3)). This situation represents a co-elliptical measurement and leads to,

$$I_{co-elliptical} = S_{PSD}^T \cdot S_{out} = m_{00} + m_{01} \cos 2\varepsilon \cos 2\alpha + m_{02} \cos 2\varepsilon \sin 2\alpha + m_{03} \sin 2\varepsilon + m_{10} \cos 2\varepsilon \cos 2\alpha + m_{11} (\cos 2\varepsilon \cos 2\alpha)^2 + m_{12} (\cos 2\varepsilon)^2 \cos 2\alpha \sin 2\alpha + m_{13} \cos 2\varepsilon \cos 2\alpha \sin 2\varepsilon + m_{20} \cos 2\varepsilon \sin 2\alpha + m_{21} (\cos 2\varepsilon)^2 \cos 2\alpha \sin 2\alpha + m_{22} (\cos 2\varepsilon \sin 2\alpha)^2 + m_{23} \cos 2\varepsilon \sin 2\alpha \sin 2\varepsilon + m_{30} \sin 2\varepsilon + m_{31} \cos 2\varepsilon \cos 2\alpha \sin 2\varepsilon + m_{32} \cos 2\varepsilon \sin 2\alpha \sin 2\varepsilon + m_{33} (\sin 2\varepsilon)^2, \quad (5)$$

where the superscript T denotes transpose and where $I_{co-elliptical}$ is the intensity corresponding to the projection of S_{out} on S_{PSD} , i.e., for the co-elliptical configuration.

Afterwards, we operate in the same way, but now, we project S_{out} onto a polarization detector system configuring the orthogonal polarization, S_{PSD}^\perp . To obtain the orthogonal polarization, it is sufficient to apply the following transformations to the polarization angles: $\varepsilon \rightarrow -\varepsilon$ and $\alpha \rightarrow \alpha + (\pi/2)$. Under this scenario, the intensity resulting from the projection of S_{out} on S_{PSD}^\perp (i.e., cross-elliptical configuration), becomes,

$$I_{cross-elliptical} = (S_{PSD}^{\perp,T}) \cdot S_{out} = (1 \quad -\cos 2\varepsilon \cos 2\alpha \quad -\cos 2\varepsilon \sin 2\alpha \quad -\sin 2\varepsilon) \cdot S_{out} = m_{00} + m_{01} \cos 2\varepsilon \cos 2\alpha + m_{02} \cos 2\varepsilon \sin 2\alpha + m_{03} \sin 2\varepsilon - m_{10} \cos 2\varepsilon \cos 2\alpha - m_{11} (\cos 2\varepsilon \cos 2\alpha)^2 - m_{12} (\cos 2\varepsilon)^2 \cos 2\alpha \sin 2\alpha - m_{13} \cos 2\varepsilon \cos 2\alpha \sin 2\varepsilon - m_{20} \cos 2\varepsilon \sin 2\alpha - m_{21} (\cos 2\varepsilon)^2 \cos 2\alpha \sin 2\alpha - m_{22} (\cos 2\varepsilon \sin 2\alpha)^2 - m_{23} \cos 2\varepsilon \sin 2\alpha \sin 2\varepsilon - m_{30} \sin 2\varepsilon - m_{31} \cos 2\varepsilon \cos 2\alpha \sin 2\varepsilon - m_{32} \cos 2\varepsilon \sin 2\alpha \sin 2\varepsilon - m_{33} (\sin 2\varepsilon)^2.$$

(6)

Finally, we perform the difference between Eqs. (5) and (6), this leading to,

$$\begin{aligned}
I_{\text{co-elliptical}} - I_{\text{cross-elliptical}} &= 2 \cos 2\varepsilon [m_{10} \cos 2\alpha + m_{20} \sin 2\alpha] + \\
&2(\cos 2\varepsilon)^2 [m_{11} (\cos 2\alpha)^2 + m_{22} (\sin 2\alpha)^2 + \cos 2\alpha \sin 2\alpha (m_{12} + m_{21})] + \\
&+ 2 \cos 2\varepsilon \sin 2\varepsilon [\cos 2\alpha (m_{13} + m_{31}) + \sin 2\alpha (m_{23} + m_{32})] + 2 \sin 2\varepsilon [m_{30} + m_{33} \sin 2\varepsilon].
\end{aligned} \tag{7}$$

Therefore, by measuring the experimental Mueller matrix of a sample and by using the Eqs. (5)-(7), it is possible to retrieve multiple polarization gating configurations just by setting the proper values for α and ε . Note that once the MM is measured, multiple PG configurations are numerically derived without the necessity of experimentally implementing each one of them.

In the following we derive the PG configurations described in Sec. 2.1 using the MM-based formalism. First, setting $\alpha=0^\circ$ and $\varepsilon=0^\circ$ (linear polarization oriented at the lab. vertical) in Eqs. (5) and (6), they yield respectively,

$$I_{\text{co-linear}} = C1 = m_{00} + m_{01} + m_{10} + m_{11}, \tag{8}$$

and

$$I_{\text{cross-linear}} = C2 = m_{00} + m_{01} - m_{10} - m_{11}. \tag{9}$$

Note that Eqs. (8) and (9) are respectively equivalent to the configurations C1 and C2 explained in Sec. 2.1. Accordingly, LConfig is:

$$I_{\text{co-linear}} - I_{\text{cross-linear}} = C1 - C2 = 2[m_{10} + m_{11}]. \tag{10}$$

Next, we select PG configurations based on elliptical polarizations with arbitrary ellipticity, ε , and the corresponding major axis parallel to one of the laboratory frame axis represented by $\alpha=0^\circ$ in Eqs. (5) and (6). Thus, they are reduced respectively to,

$$\begin{aligned}
I_{\text{co-elliptical}} &= C3 = \\
&m_{00} + \cos 2\varepsilon [m_{01} + m_{10}] + \sin 2\varepsilon [m_{03} + m_{30}] + \cos 2\varepsilon \sin 2\varepsilon [m_{13} + m_{31}] + m_{11} (\cos 2\varepsilon)^2 + m_{33} (\sin 2\varepsilon)^2,
\end{aligned} \tag{11}$$

and

$$I_{\text{cross-elliptical}} = C4 = m_{00} + \cos 2\varepsilon [m_{01} - m_{10}] + \sin 2\varepsilon [m_{03} - m_{30}] - \cos 2\varepsilon \sin 2\varepsilon [m_{13} + m_{31}] - m_{11} (\cos 2\varepsilon)^2 - m_{33} (\sin 2\varepsilon)^2. \quad (12)$$

Note that Eqs. (11) and (12) are equivalent to the configurations C3 and C4 respectively for EPG, explained in Sec. 2.1. Accordingly, different ellipticities can be set by properly selecting the angle ε . Logically, for $\varepsilon=0$ we end up in the linear case, and thus, Eqs. (11) and (12) reduce to Eqs. (8) and (9), respectively.

The EConfig. described in Sec. 2.1 can be obtained by subtracting these two relations as,

$$I_{\text{co-elliptical}} - I_{\text{cross-elliptical}} = C3 - C4 = 2 \cos 2\varepsilon [m_{10} + m_{11} \cos 2\varepsilon] + 2 \cos 2\varepsilon \sin 2\varepsilon [m_{13} + m_{31}] + 2 \sin 2\varepsilon [m_{30} + m_{33} \sin 2\varepsilon], \quad (13)$$

Note that we can select an arbitrary EConfig simply by changing the ε parameter in Eq. (13).

Finally, from the above-described formulation we can also obtain the function f defined in Eq. (1) and derived in Ref. [19]. To avoid the requirement of performing extra experimental measurements for the determination of the parameter β in Eq. (1), we set $\alpha=45^\circ$. By using this configuration, the amount of light projected to the p -polarized and s -polarized components is always the same, independently of the chosen ellipticity. Thus, the factor β equals to 1 in such a case. Accordingly Eq. (7) becomes,

$$I(\alpha = 45^\circ)_{\text{co-elliptical}} - I(\alpha = 45^\circ)_{\text{cross-elliptical}} = 2 \cos 2\varepsilon [m_{20} + m_{22} \cos 2\varepsilon] + 2 \cos 2\varepsilon \sin 2\varepsilon [m_{23} + m_{32}] + 2 \sin 2\varepsilon [m_{30} + m_{33} \sin 2\varepsilon]. \quad (14)$$

Moreover, if $\varepsilon=0^\circ$ in Eq. (14), it reduces to the linear case,

$$I(\alpha = 45^\circ; \varepsilon = 0^\circ)_{\text{co-elliptical}} - I(\alpha = 45^\circ; \varepsilon = 0^\circ)_{\text{cross-elliptical}} = 2[m_{20} + m_{22}]. \quad (15)$$

Finally, adding Eqs. (14) and (15) leads to,

$$f_{MM} = (C3 - C4)|_{\alpha=45} + (C1 - C2)|_{\alpha=45} = 2[m_{20} + m_{22}] + 2 \cos 2\varepsilon [m_{20} + m_{22} \cos 2\varepsilon] + 2 \cos 2\varepsilon \sin 2\varepsilon [m_{23} + m_{32}] + 2 \sin 2\varepsilon [m_{30} + m_{33} \sin 2\varepsilon], \quad (16)$$

which provides the function f as a function of the MM coefficients.

Note that in practice, many samples present spatial dependence of their polarimetric properties, as birefringent samples that possess a principal direction. In such cases, larger image contrast may be obtained by illuminating the sample with a different azimuth angle. If this is the case, the parameter β should be experimentally determined as described in Ref. [19].

3 Imaging Mueller polarimeter and sample description

In this section we describe the optical arrangement used to measure the Mueller matrix of samples (Sec. 3.1), and we describe the different samples we study in the forthcoming experimental section (Sec. 3.2).

3.1 Optical scheme: Imaging Mueller Polarimeter

The optical set-up used to measure MMs of different samples is a complete imaging Mueller matrix polarimeter [36] based on Parallel Aligned Liquid Crystal (PA-LC) retarders. The set-up, sketched in Fig. 1, is analogous to that described in Ref. [37] but adapted for imaging polarimetry.

First, a light source illuminates a Polarization State Generator (PSG, marked with a green rectangle in Fig. 1), which includes a linear polarizer at 0° degrees to the laboratory vertical reference axis, a first PA-LC panel (PA1), oriented at 45° to the laboratory vertical, and a second PA-LC panel oriented at 0° to the laboratory vertical (PA2). As discussed in Ref. [37], any fully polarized state of polarization can be generated with this system by adjusting the retardances of the two PA-LC panels. Then, the input light with controlled polarization illuminates a sample holder, where the sample is set, with an incident angle of approximately 60° . The sample holder can be mechanically displaced in the z direction for imaging purposes. Then, the light scattered by the sample is measured with a Polarization State Detector (PSD, marked with a blue rectangle

in Fig. 1), which is constructed with the same optical elements than those in the PSG but with inverse order. Finally, a convergent lens images the sample on a CCD camera with certain magnification.

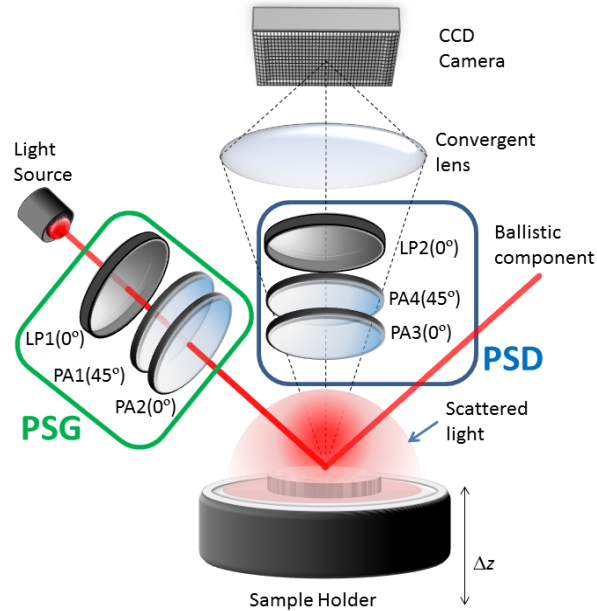


Fig. 1 Optical scheme of the used Mueller polarimeter.

Under this scenario, and by properly generating a basis of known input polarizations with the PSG, and measuring the corresponding Stokes vector of the scattered light with the Stokes polarimeter (PSD system), we construct a linear system (see Eq. (2)) from which the experimental Mueller matrix (MM) of the sample can be obtained by applying an inversion method, discussed in Refs. [21, 38].

All experimental results shown and analyzed in a forthcoming section (Sec. 4) were obtained by experimentally implementing the optical scheme sketched in Fig. 1. The experimental set-up is shown in Fig. 2(a). As a light source we used a 4-Wavelength High-Power LED Source (Operated by DC4104 drivers distributed by Thorlabs). In particular, the color channels used in this work for conducting the different experimental measurements were the red channel (with a central wavelength of 625 nm and a spectral bandwidth (FWHM) of 18 nm) and the blue channel

(central wavelength of 470 nm and a FWHM of 10 nm respectively), with a maximum output power of 240 mW and 250 mW respectively. To achieve a FWHM of 10 nm with the blue channel, a dielectric bandwidth filter (by Thorlabs) was used. The linear polarizer in the PSG (LP1) is a Glan-Thompson prism based polarizer (by CASIX). The linear polarizer at the PSD (LP2) is a dichroic sheet polarizer (by Meadowlark Optics). For the liquid crystal panels in the PSG and PSA, we used four Parallel Aligned (PA) Liquid Crystal Variable Retarders with Temperature Control (LVR-200-400-700-1LTSC by Meadowlark Optics). Finally, a microscope objective images the selected sample ROI on a CCD camera. The convergent lens in Fig. 1 was a TECHSPEC® High Resolution objective, distributed by Edmund Optics, with a focal length of 35 mm. The camera is an Allied Vision Manta G-504B. It is a 5 Megapixel GigE Vision camera with the Sony ICX655 CCD sensor, with a 2452(H) × 2056(V) resolution and a cell size of 3.45 μm × 3.45 μm. As shown in Fig. 2(a), the PSG and PSD systems were assembled in two black holders made with a 3D printer. These holders were designed to configure a robust and feasible full-Muller imaging polarimeter in which the optical elements were protected from the environment (dust, misalignments, stray light, scratches, etc.).

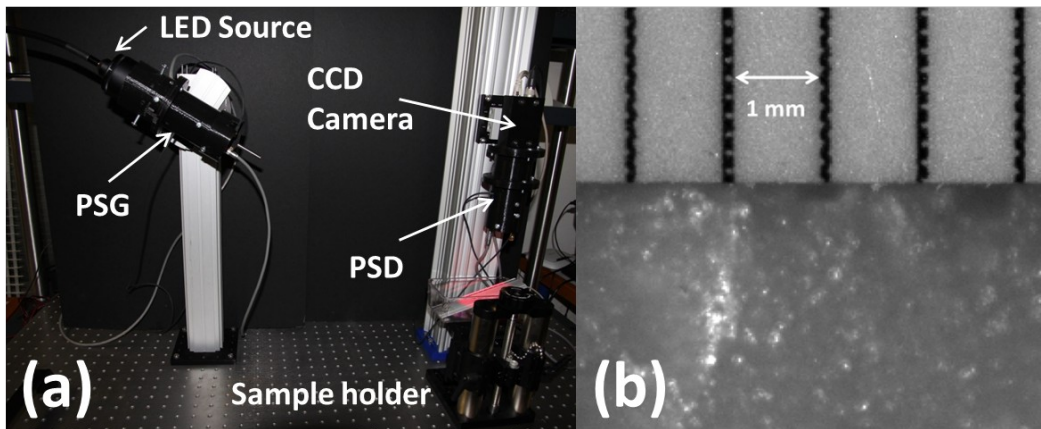


Fig. 2 (a) Picture of the experimental system; (b) Image of a ruler placed on a slice of pork, for image resolution calculation.

The resolution selected for the conducted experimental measurements is described in the following. In Fig. 2(b) we picture a ruler placed on a thick slice of pork tissue. The distance between different lines is of 1 mm. This distance corresponds to 52 pixels of the recorded image, this leading to a spatial resolution of $\sim 19 \mu\text{m}$. If more resolution is desired, the sample holder can be brought closer to the objective by performing an axial displacement Δz as indicated in Fig. 1.

3.2 Sample description: Phantom experiment and ex-vivo measurement

To prove that the above discussed PG configurations can be obtained from Mueller measurements, we have performed two different experiments.

First, we have reproduced the phantom experiment described in Ref. [19]. Let us call it Sample A. In particular, a metallic ruler is placed obliquely on a plastic tank (15.5 cm x 7.5 cm x 5 cm). Then, the tank is filled with Intralipid (20%, Sigma-Aldrich, France) diluted in water (see Fig. 3(a)). Intralipid is a lipid emulsion currently used for human intravenous use. In particular, Intralipid is an emulsion of soy bean oil, egg phospholipids and glycerin, and is available in 10%, 20% and 30% concentrations. In the current work, this Intralipid is diluted in water to a concentration of 0.1%, and, the dilution is used to mimic the interaction of light with scattering tissues. For this concentration, the reduced scattering coefficient μ'_s for the red and blue channels

is estimated to be of $\mu'_s|_{625 \text{ nm}} = 0.63 \text{ cm}^{-1}$ and $\mu'_s|_{470 \text{ nm}} = 0.46 \text{ cm}^{-1}$. According to Ref. [39], the

corresponding anisotropy factor g of Intralipid is $g=0.73$ and $g=0.83$ (for the 625 nm and 470 nm respectively). The corresponding mean free paths (MFP) are of $MFP|_{625 \text{ nm}} = 4.3 \text{ mm}$ and

$MFP|_{470 \text{ nm}} = 3.7 \text{ mm}$. According to the experimental results observed and described in a

forthcoming section, with this configuration we can perform macroscopic measurements with a sample penetration depth at the millimeter scale.

The second experiment is performed on an *ex-vivo* tissue (let us call it Sample B). In particular, we have studied a region of interest (ROI) of a chicken neck, where different biological structures, as muscles and nerves, are observed (see red square in Fig. 3(b)). We want to emphasize that the region selected for measurements is fairly flat, avoiding possible image quality losses related to defocused planes.

Concerning the stability of the optical properties of the Intralipid, a complementary experience, not discussed in this work, showed that the structure of an Intralipid emulsion left still over time can evolve because spontaneous phase segregation (lipid/water) takes place. The process of phase segregation is very slow with a characteristic time of a few hours. Since the experiences reported here were performed in a time scale of seconds, we can, therefore, assume that the polarimetric properties of the samples remained constant along the measurement time.

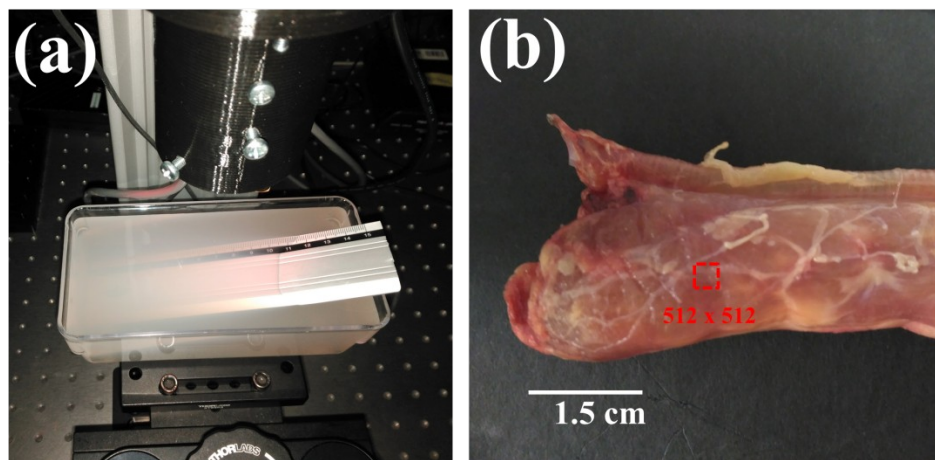


Fig. 3 (a) Tank filled with Intralipid diluted in water and the metallic ruler (Sample A). The sample is located in a sample-holder to be measured with the polarimeter. The scattering effect is clearly observed; (b) Chicken neck for the *ex-vivo* experiment. The red square shows the measured ROI.

4 Experimental results

In this section we provide the equivalence between the Polarization Gating (PG) configurations and those deduced from Mueller matrix (MM) (Sec. 4.1). In addition, the potential of using MM to perform PG based analysis is highlighted in Sec. 4.2, as MM channels provide extra polarimetric information that can be combined with PG techniques.

To this aim, we show and discuss experimental data obtained from measurements on the samples described in Sec. 3.2 (see Fig. 3). In particular, different measurements of the samples were performed under different PG configurations. For comparison with formulation given in Sec. 2.2, the corresponding MMs of the samples were also measured. The two sets of measurements (i.e., PG configurations and MM measurements) were obtained by using the experimental set-up described in Sec. 3.1.

4.1 Polarization Gating configurations derived from Mueller measurements

In this sub-section, we provide the equivalence between different PG configurations (Sec. 2.1) and those obtained from MM measurements (Sec. 2.2). To this aim, we have used the Sample A described in Sec. 3.2. All the images provided in this sub-section present a resolution of 1024x512 pixels and are obtained by illuminating the samples with the red channel (625 nm).

First, the MM of the sample was experimentally obtained by using the Mueller polarimeter sketched in Fig. 1. To this aim, we used a basis of 6 states of polarization both for illumination and detection: linear polarizations oriented at 0, 45, 90 and 135 degrees to the laboratory vertical, and two circular polarizations (right-handed and left-handed polarizations). The selected polarization basis above-stated is commonly used due to its simplicity and because it leads to the minimum possible condition number (mathematical indicator that can be used to estimate the

quality of a PSG-PSD system in terms of noise amplification) for polarimetric systems (CN = 1.73).

We want to note that some authors [40, 41] have proved that the intensity contrast of a particular sample can be enhanced by selecting a direct gating configuration where the PSG-PSD polarizations are optimized. To make this selection of the optimal PSG-PSD channels, we need to know some *a priori* polarimetric information of the sample or measure its Mueller matrix. In the latter case, from the measured Mueller matrix, by applying an optimization method, one can find the PSG-PSD channels that maximize the image contrast. Note that the MM based approach we propose not only can be combined with PG configurations, but also could be used to perform the optimizations proposed in Refs. [40, 41].

From the measured MM, different polarization gating configurations were calculated according to the formulation described in Sec. 2.2. As an example, Fig. 4 shows the results obtained for some of the PG configurations described in Sec. 2.1, obtained by using the experimental MM coefficients: configurations C1 (Fig. 4(a)), C2 (Fig. 4(c)), C3 (Fig. 4(e)), C4 (Fig. 4(g)), C1-C2 (Fig. 4(i)) and C3-C4 (Fig. 4(k)).

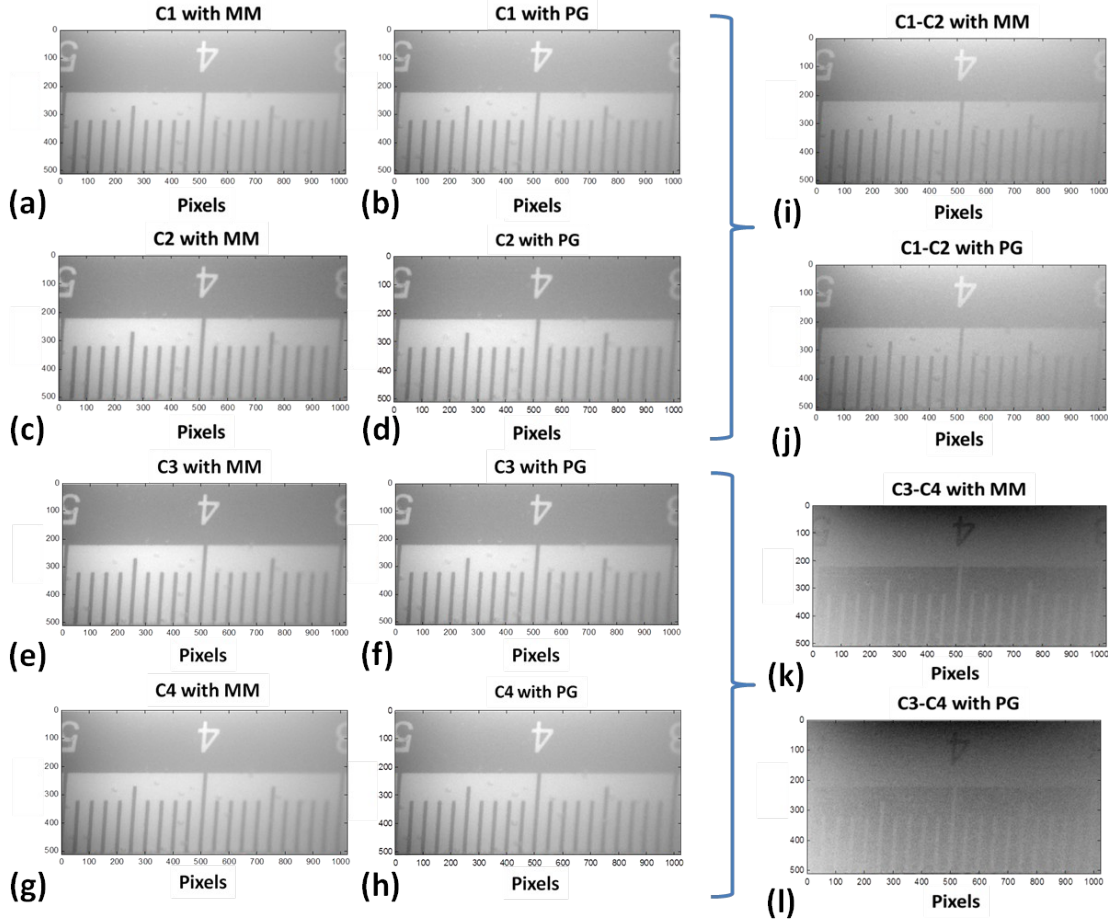


Fig. 4 Comparison between different PG configurations obtained from: MM coefficients (a, c, e, g, i and k); and from standard PG procedures (b, d, f, h, j and l).

For comparison, the same configurations were obtained by using standard PG procedures, i.e., by setting the proper PSG-PSA configurations and recording the corresponding intensity images. Results are given in: C1 (Fig. 4(b)), C2 (Fig. 4(d)), C3 (Fig. 4(f)), C4 (Fig. 4(h)), C1-C2 (Fig. 4(j)) and C3-C4 (Fig. 4(l)).

We see that the results obtained from MM or from standard PG techniques lead in all cases to equivalent information, because the final intensity images are very similar. To further quantify this similarity, Fig. 5 shows the absolute difference between the intensity images obtained from MM and from PG techniques for the C1 (Fig. 5(a)), C3 (Fig. 5(b)), C4(Fig. 5(c)) and C3-C4 (Fig. 5(d)) cases.

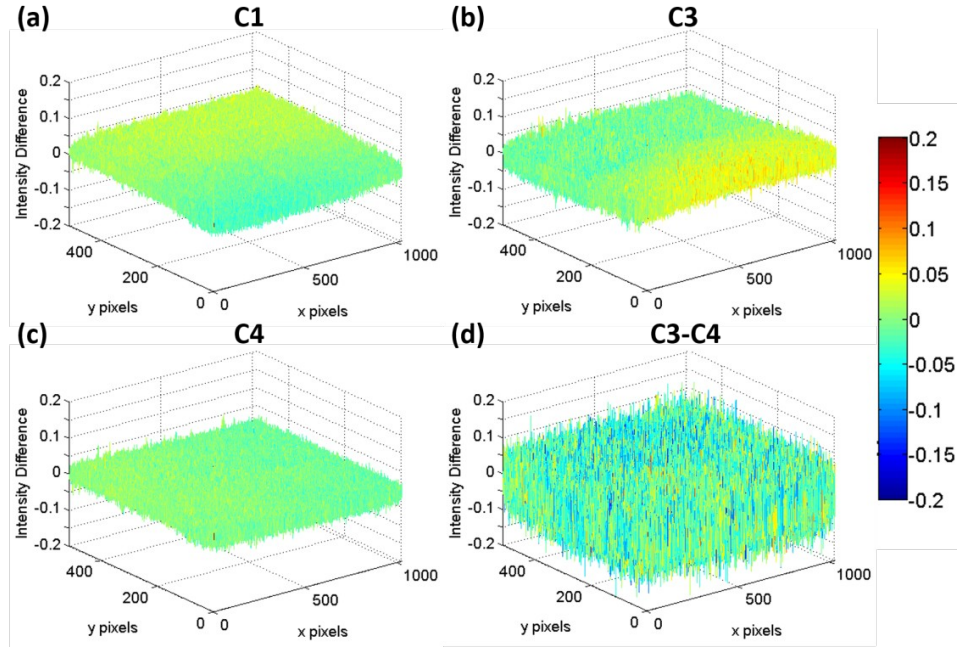


Fig. 5 Intensity absolute differences for the PG configurations: (a) C1, (b) C3, (c) C4; (d) and C3-C4.

For polarization configurations obtained from a single measurement, i.e., the C1, C2, C3 and C4 channels, the absolute error calculations were conducted as follows: (1) The $C_i(\text{PG})$ image is obtained from PG measurements (the subscript i is equal to 1, 2, 3 or 4 for the C1, C2, C3 and C4 cases, respectively); (2) The $C_i(\text{MM})$ image is obtained from MM measurements; (3) $C_i(\text{PG})$ and $C_i(\text{MM})$ are normalized to 1; and (4) The absolute error between images ($C_i(\text{PG}) - C_i(\text{MM})$) is obtained pixel to pixel.

For polarization configurations obtained from image processing, e.g., C1-C2 and C3-C4 channels, the absolute error calculations were conducted as follows: (1) The $C_j(\text{PG})$ image is obtained from PG measurements (the subscript j is equal to 1 or to 3 for the C1-C2 or the C3-C4 cases, respectively); (2) The $C_j(\text{MM})$ image is obtained from MM measurements; (3)

The $C_{j+1}(\text{PG})$ image is obtained from PG measurements; (4) The $C_{j+1}(\text{MM})$ image is obtained from MM measurements; (5) The $C_j - C_{j+1}$ channels are obtained in each case:

$A=C_j(\text{PG})-C_{j+1}(\text{PG})$ and $B= C_j(\text{MM})-C_{j+1}(\text{MM})$; (6) The processed images A and B are normalized to 1; and (7) The absolute error between A and B is calculated as $A-B$.

In addition, the mean absolute errors and standard deviations (σ) values corresponding to all the experiments shown in Fig. 4 are also provided in Table 1.

Note that for direct PG channels, i.e. C1, C2, C3 and C4 configurations, the absolute differences (Fig. 5(a)-(c)) and the mean absolute differences (Table 1) are always smaller than 0.05. This leads to absolute differences smaller than 5% if taking into account the full images intensity range [0-1], and they can be mainly attributed to random noise at the intensity measurements. The case of PG channels obtained from image subtraction processing is also studied. We analyzed two different configurations: (i) the C1-C2 channel (i.e., “C1-C2 with MM” – “C1-C2 with PG”); and (ii) the C3-C4 channel (i.e., “C3-C4 with MM” – “C3-C4 with PG”). The absolute errors between channels are always smaller than 0.1 (10%) (e.g., Fig. 5(d)). In addition, the mean absolute errors were 0.021 and 0.041 respectively (Table 1), and thus, smaller than 0.05 (5%).

Note that the above-shown error values ensure the equivalence between standard PG configurations and PG configurations obtained from Mueller matrices. If required, these error values could be even reduced by time-averaging different intensity images.

Finally, we want to highlight that by implementing PG configurations from MM measurements, we do not need to perform any new experiment for each extra PG configuration to be implemented. In fact, by using the mathematical formalism detailed in Sec. 2.2, a widespread number of PG configurations can be analytically obtained based on the MM coefficients.

Table 1 Mean absolute difference and standard deviation σ for different PG channels.

Channel	Mean Absolute Difference	σ
C1	0.015	0.010
C2	0.026	0.019
C1-C2	0.021	0.016
C3	0.020	0.014
C4	0.012	0.009
C3-C4	0.041	0.031

As an example, we show the results obtained when implementing the function f_{MM} , detailed in Eq. (16), from the MM coefficients measured for the phantom experiment (i.e. ruler submerged into a tank with Intralipid diluted in water; see Sample A description in Sec. 3.2). Note that the ellipticity angle ε is a control parameter in Eq. (16). Therefore, in contrast to traditional PG experiments, where each ellipticity value to be tested (i.e. ellipticity for the generated and analyzed polarizations) has to be experimentally implemented, we can readily obtain such information channel with an arbitrary ε from measured MM coefficients (Eq. (16)). This situation is highlighted in the [Video 1](#), where different frames show the Sample A image obtained by processing the function f_{MM} as a function of the ε value, from $\varepsilon=-45^\circ$ to $\varepsilon=+45^\circ$, with steps of 1° .

Images of [Video 1](#) show the ruler submerged into the diluted Intralipid and the different ruler numbers observed (i.e. 3-4-5) are related to different depths in the liquid (see Fig. 3(a)). In particular, the number 5 is the number closer to the surface and the number 3 is the one more in depth. In agreement with other studies [17, 19], we see that larger ellipticity values ($\varepsilon \sim \pm 45$ degrees) lead to a larger quantity of photons coming from deeper parts of the sample, as the number of scattering events taking place in a particular length depend on the polarization. This can be observed in [Video1](#) as clearer ($\varepsilon \sim +45^\circ$) or darker ($\varepsilon \sim 0^\circ$) image frames.

To quantify the different contrast provided by selecting different ellipticities in Eq. (16) for the phantom experiment (variations observed in [Video1](#)), we have calculated the visibility

$$V = \frac{I_{max} - I_{min}}{I_{max} + I_{min}}$$
 for the two cross-sections shown in Fig. 6(a) (blue line for the four number and red line for the ruler tick mark), where I_{max} and I_{min} are the maximum and minimum values in the cross-section selected. We want to note that the best visibility values are obtained for an elliptical state of polarization ($\sim 30^\circ$). In general, polarization gating configurations based on linear and circular polarizations are commonly used for its simplicity to be experimentally implemented. However, as shown in Fig. 6(b), these configurations not always lead to the best contrast. If another ellipticity wants to be tested, by using standard PG measurements each new configuration has to be experimentally implemented, this leading to a blind process. However, by using the method described in Sec. 2.2, such information can be analytically obtained, as shown in Fig. 6(b).

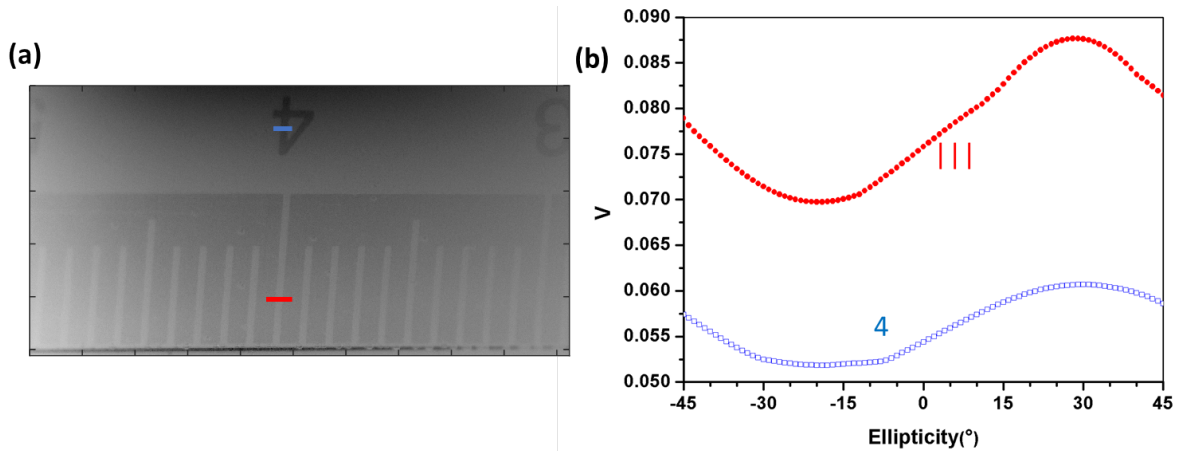


Fig. 6 (a) Cross-sections selected for the 4 number (blue line) and a ruler millimeter tick mark (red line); (b) Visibility (V) as a function of the ellipticity angle.

Note that [Video1](#) and data in Fig. 6 show the potential of rapidly implementing standard PG configurations from MM measurements, as this method constitutes a more general approach.

4.2 Polarization Gating and Mueller processing combination

In this section we show the interest of performing polarimetric analysis of biological samples using MM data because this method not only allows to set multiple Polarization Gating (PG) configurations from analytical expressions (as shown in Sec. 4.1), but also provides new information channels (Mueller matrices, Matrix decompositions, differential matrices, etc). In addition, the study provided in this section also highlights the interest of combining MM analysis tools with PG configurations.

4.2.1 Phantom experiment

We first performed a modification on the Sample A by considering also retardance. The Intralipid-ruler based experiment discussed above tries to mimic the scattering response of biological tissues. However, in general, other polarimetric responses simultaneously occur when light interacts with biological tissues. For instance, most biological tissues contain collagen fibers, which are part of the extracellular matrix and provide structural and biochemical support to the surrounding cells. Depending on the collagen degree of mineralization, collagen tissues may be rigid (e.g. bone), flexible (e.g. tendon), or present a gradient from rigid to flexible (e.g. cartilage). Moreover, collagen fibers are birefringent materials that present different retardation values for different biological structures [42], as those present in nerves, muscles, bones, ligaments, etc. Thus, image contrast between different tissues may be enhanced by considering polarimetric information. Some studies show that collagen fibers appear curly and anisotropic in normal stroma [43], but they appear more stretched during early cancer progression, and they tend to be aligned parallel to the tumour border [44]. Therefore, retardation content is a valuable parameter for enhancing image contrast for biological and medical applications.

To take this fact into account and to include some retardance in the sample, the Intralipid-ruler based experiment was repeated but by sticking two cellophane tape films on the ruler with different orientations respectively, (let us call it Sample C; see Fig. 7(a)). Note that the cellophane tape films act as linear retarders due to the stress applied on their constituent polymers during the fabrication process.

First, we have measured the Sample C by using traditional PG experimental techniques with the 625 nm light channel. In particular, Fig. 7(c) shows the image obtained by performing the standard PG configuration labelled as C3-C4 in Sec. 2.1, by using right-handed circular polarization for illumination. By contrast, Fig. 7(d) shows the same PG configuration but this time for a left-handed circular illumination. We can see well-differentiated zones with different intensity structures in Sample C as a consequence of the polarization variations induced by the cellophane retardance. Note that these differences are not present in Figs. 4 (k) and (l) (same PG configuration but applied on Sample A). In addition, we observe that image contrast is significantly different by using right-handed (Fig. 7(c)) or left-handed (Fig. 7(d)) polarizations.

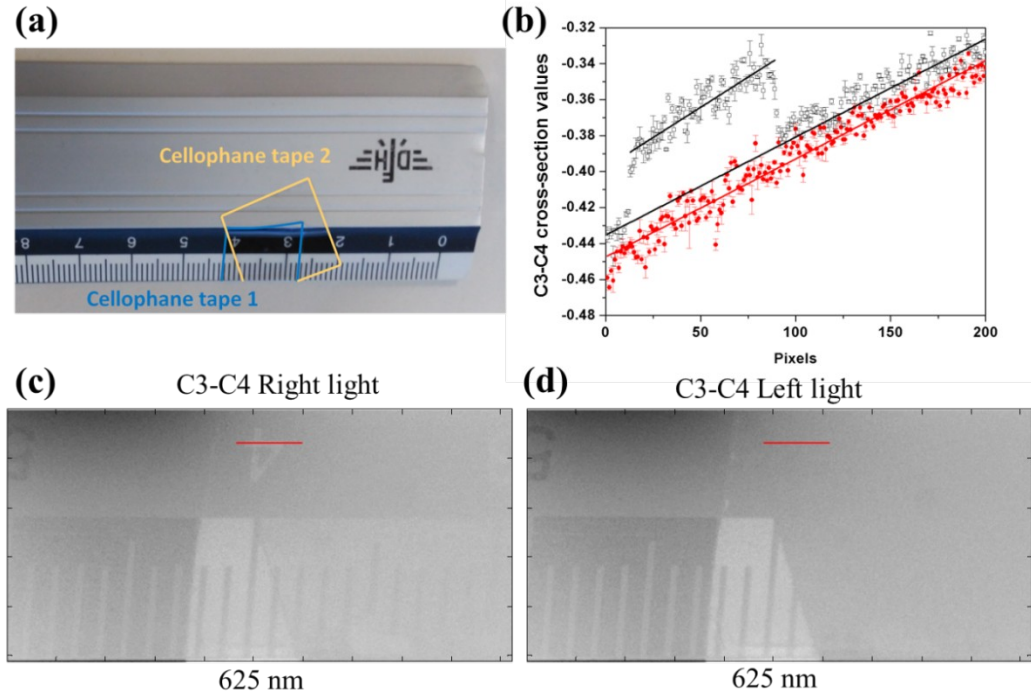


Fig. 7 (a) Ruler with stuck scotch types (Sample C); (b) Cross-section values of the red line in Fig. 7(c) (black empty squares) and Fig. 7(d) (red circles) ;(c) C3-C4 PG image for right-handed circular light; and (d) C3-C4 PG image for left-handed circular light.

For example, the number 4 is not visible for the left-handed polarization, but it is clearly visible when using the right-handed polarization. This fact is highlighted in Fig. 7(b) where the cross-section corresponding to the red lines marked in Figs. 7(c) and (d) are shown. The cross-section values related to red line in Fig. 7(c) (right-handed polarization case) goes linearly to zero as we go inside the Intralipid-water solution (see red circles). The linear tendency is shown by the calculated linear regression drawn as a continuous line (red line). In turn, the cross-section values for the red line in Fig. 7(d) (left-handed polarization case) has the same behaviour, but shows a sharp jump in the image contrast for the pixels related to the four number (see black squares). This situation occurs because of elliptical states of polarization are modified in a different way depending on the retardation and orientation of the cellophane tape. Thus, although some authors have pointed out the interest of using elliptical polarizations to test deeper

structures in biological tissues, data shown in Fig. 7 also shows the interest of optimizing the helicity of the selected polarization, because of such parameter can be important to enhance image contrast in biological tissues.

Afterwards, we have calculated the Mueller matrix (MM) of the sample C for 625 nm. The corresponding 16 real images are shown in Fig. 8. We want to note that image coefficients pictured in Fig. 8 are normalized in each case by its corresponding maximum coefficient value, thus maximizing the image contrast for each particular coefficient. However, this representation does not allow us to visualize the relative intensity differences between Mueller coefficients. Thus, a matrix showing the maximum intensity value for each MM element when being normalized by the maximum value of the MM00 element is also provided as a bar chart at the left part of Fig. 8. This information allows us to identify the relative intensity magnitude between channels.

Note that the MM by itself provides different polarimetric information (MM coefficients in Fig. 8) than those related to the standard PG configurations, and thus, MM coefficients provide further information that can be used and combined to enhance the sample image contrast [45]. In addition, Mueller matrix analysis allows performing a physical interpretation of the sample [21, 22]. In a rough approximation, the MM coefficients in the first row and column of the matrix can be linked with the diattenuation and polarizing capabilities of the sample respectively (in the case of the Sample C, mainly related to light reflections on the metallic surface of the ruler), the diagonal coefficients encode the depolarizing capability of the sample (for the Sample C, mainly related with scattering events produced due to the fats present in the Intralipid-water dissolution), and the bottom-right 3x3 submatrix can be linked with the retardance introduced by the sample (in Sample C, due to the cellophane birefringence values).

In addition, the polarimetric content encoded on the MM of the sample can be further quantified by performing a physical model where the properties of the sample are thought as a combination of different pure polarimetric samples, typically, a diattenuator, a retarder and a depolarizer. In other words, the sample can be further inspected by using well-known Mueller matrix analytical tools, as for instance, by applying MM decompositions [21, 22, 46].

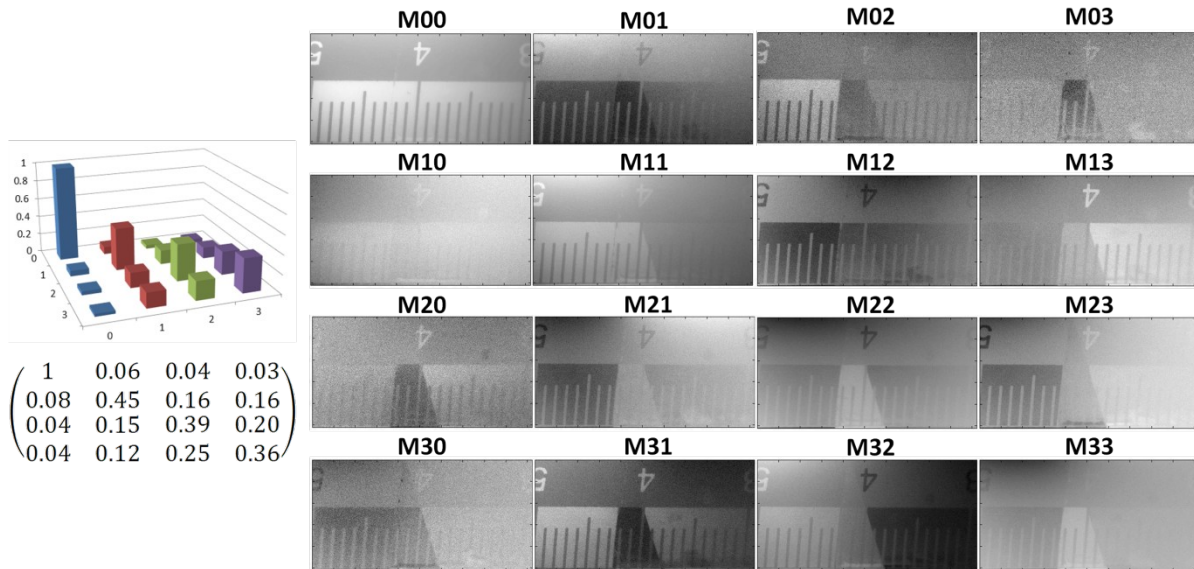


Fig. 8 Experimental Mueller matrix of the Sample C measured at 625 nm.

4.2.2 Ex-vivo experiment

Finally, to discuss a case which is closer to real experience than the phantom previously shown, the ex-vivo tissue labeled as Sample B (see Sec. 3.2) was analyzed. To this aim, the Mueller matrix of the sample was measured using the 470 nm channel. Some authors have provided the dependence of light penetration in biological tissues with the wavelength used [47]. In the visible range, larger wavelengths enter deeper into the skin than shorter ones. Therefore, we have chosen the shorter available wavelength for illumination to mainly inspect biological structures at the sample surface.

The experimental MM for the Sample B is shown in Fig. 9(a). As can be observed from the coefficient M00, which is related to the sample irradiance, the selected Region of Interest (ROI) (see Fig. 3(b)) includes different biological structures, as muscles and nerves. It can be observed that different image coefficients lead to different contrast levels between the biological structures present in the sample (Fig. 9(a)).

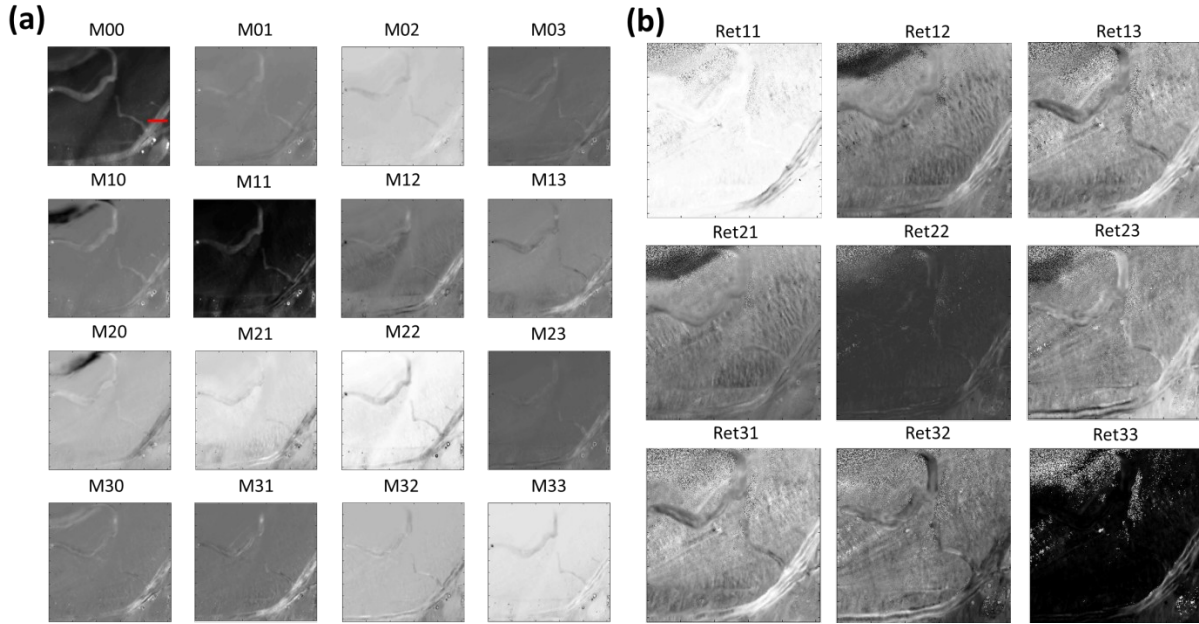


Fig. 9 (a) Experimental Mueller matrix of the Sample B measured at 470 nm. (b) 3x3 Mueller sub-matrix of the equivalent linear retarder for the Sample B.

In addition, to highlight the interest of using MM based analytical tools, we have also applied the Lu-Chipman decomposition [22], which allows us to decompose the Mueller matrix of a sample as a product of three basic MMs: the MM of a diattenuator (Di), the MM of a retarder (Ret), and the MM of a depolarizer (De). As an example, the MM of the retarder (Ret) for the Sample B is also provided in Fig. 9(b). For a better visualization of the Ret matrix, the first row and column coefficients are removed in Fig. 9(b) because they are always zero in linear retarders. Thus, significant polarimetric content in the Ret matrix is at the 3x3 sub-matrix shown in Fig. 9(b).

Note that the matrix Ret only provides the retardance information of the sample (other polarimetric content has been already extracted by means of the matrix decomposition), and thus, the image contrast observed in the Ret matrix channels is mainly due to retardance features of the sample. In other words, contrast obtained from the retarder matrix of biological tissues is related to retardance created by different sample structures, for instance, due to the different collagen fibers density, mineralization degree, or orientation at the different biological structures. For the Sample B particular case (Fig. 9(b)), we see that the retardance content of the sample provides a noticeable contrast of the nerve ramification along the muscle in the chicken neck, this being specially highlighted in the Ret_{13} , Ret_{31} , Ret_{23} and Ret_{32} coefficients of the Ret matrix. In addition, the Mueller matrix of the depolarizer (De) and the Diattenuator (Di) have been calculated as well, leading in this case to less contrast than the M and the Re matrices.

To quantify the above-stated discussion, in Fig. 10 we show the cross-sections related to the red line shown in Fig. 9 (see coefficient M_{00} in Fig. 9(a)). In particular, we have calculated the visibility corresponding to the cross-line above-stated for all the Mueller coefficients and for all the coefficients of the decomposed matrices (Di , De and Re cases), always for the same line of the sample. The largest visibility in each case has been obtained for the M_{33} , Re_{33} , De_{21} and Di_{30} coefficients. The corresponding cross-sections are provided in Fig. 10.

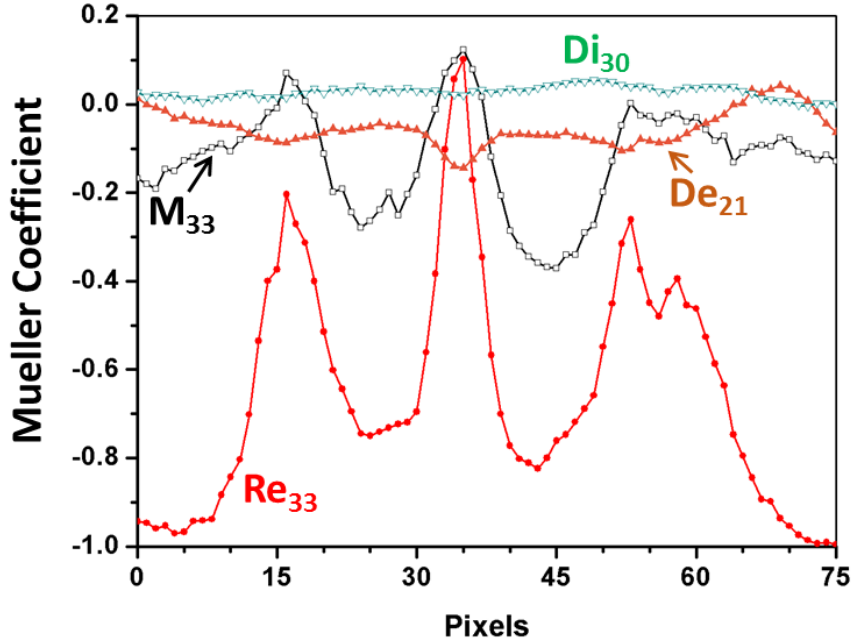


Fig. 10 Cross-sections (related to the line shown in Fig. 9(a)) corresponding to the coefficients providing the best visibility for the Mueller matrix (black empty squares), the Retarder (red circles), the Depolarizer (brown triangles) and the Diattenuator (green empty triangles).

In agreement with the qualitative discussion provided above, the best contrast for the chicken nerve (see red line in Fig. 9(a)) is obtained with the Retarder matrix, where the separation between different nerve structures is highlighted by the different picks (see red circles in Fig. 10). Note that this sample detail is almost hidden in the Diattenuation and the Depolarization channels (green empty triangles and brown triangles respectively in Fig. 10).

At this point, we have shown how PG techniques based on MM measurements lead to a generalization of the standard PG methods (Sec. 2.2 and 4.1). In this sub-section we also highlighted the interest of using MM measurements for biological tissue inspection as they bring a whole new battery of analytical techniques. Last but not least, we want to discuss the interest of combining PG methods with MM analytical tools.

To this aim, we used the Sample B (chicken neck, see ROI in Fig. 3(b)) described in Sec. 3.2. In particular, the function f_{MM} (Eq. (16) in Sec. 2.2; PG based relation) was calculated from the

MM coefficients of the Sample B (data pictured in Fig. 8(a)). In addition, to exploit the Mueller matrix capabilities, the f_{MM} was calculated again but this time from the decomposed Mueller matrices, which were calculated according to the Lu-Chipman decomposition [22]. Therefore, the f_{MM} function was obtained for the diattenuator (Di), the retarder (Ret), and the depolarizer (De) Mueller matrices. As f_{MM} is an analytical expression, in all the cases it was calculated for different ellipticity values, from -45 to +45 degrees with steps of 1 degree. Thus, results are provided in video format. In particular, [Video 2](#) provides the f_{MM} function calculated from the MM as a function of the ellipticity value selected. Moreover, the same function but calculated from the Di, De and Ret matrices is given in [Video 3](#), [Video 4](#) and [Video 5](#) respectively.

On the one hand, when analyzing the data obtained from the MM coefficients ([Video 2](#)), we observe certain contrast between the biological tissues present in the sample, mainly nerves and muscle tissues. Moreover, the biological structures visualization strongly depends on the ellipticity of the PG channel selected. For instance, in [Video 2](#) we see as the nervous tissue placed at the image bottom is better visualized by using larger ellipticities ($\varepsilon \sim \pm 45$ degrees) showing more clearly its ramified structure. On the contrary, surface muscle is better contrasted by using linear polarizations ($\varepsilon \sim 0$ degrees).

On the other hand, better sample interpretation can be achieved by using the f_{MM} function derived from decomposed Mueller matrices. First, [Video 3](#) provides the f_{MM} function calculated from the Diattenuator matrix coefficients. As can be observed, we obtain a very poor image contrast between tissues, this indicating that the analyzed structures do not present significant dichroism values (at least at the superficial layers), and polarimetric features of the Sample B are mainly related to birefringence and depolarizing processes. Next, the f_{MM} function calculated from the Depolarizer matrix coefficients provides a noticeable image contrast between nerves

and muscles ([Video 4](#)), this indicating that each particular tissue scatters light in a different way. In addition, image contrast varies with the selected elliptical channel, ellipticities close to $\varepsilon \sim -45$ degrees being those providing the best contrast between nerves and muscle. By contrast, fibrillary nature of muscle tissue is better resolved by using linear channels ($\varepsilon < \pm 10$ degrees). Finally, the function f_{MM} calculated from the retarder matrix Ret also provides different polarimetric information ([Video 5](#)). By using this polarimetric information, muscle-nerve contrast is reduced when compared with data in [Video 4](#). In addition, muscle tissue seems to be quite uniform through the whole muscle surface, leading to a uniform black image (the best muscle contrast is obtained for linear channels). Nevertheless, nerve contrast itself is significant. In fact, f_{MM} function based on the retarder data reveals a ramified structure for the nerve (in the lower part of the images), where different nerve details are discovered by using different ellipticity channels.

We want to emphasize that this particular example could be further investigated by using other analytical expressions deducted from MM coefficients, as those provided in Ref. [45], or others relevant processing techniques.

5 Conclusions

We presented an experimental method based on the calculation of the Mueller matrix of samples suitable for the calculation of standard Polarization Gating (PG) techniques. We proved that this method is not only equivalent to standard PG measurements, but also, it can be used to build general analytical expressions from which a set of PG configurations can be simultaneously obtained.

We also proved that when conducting PG measurements to inspect biological tissues, it is not only important to optimize the ellipticity of the input and analyzing states of polarization, as

previously highlighted by some authors, but also to optimize the helicity of the elliptical state of polarization. This situation occurs because when polarized light interacts with complex structures, right-handed and left-handed polarizations are modified in a different way due to different media polarimetric characteristics, for instance, the retardance introduced by the media, the orientation of the extraordinary axis of the anisotropic media, etc.

Finally, we have also highlighted the interest of not only performing PG based on Mueller matrix (MM) measurements, but also to take benefit of all those analytical tools related to the Mueller formalism. By doing this, extra polarimetric channels and analysis techniques are available. In addition, they can be combined with standard PG methods to obtain further information.

The experimental method here proposed was tested on different samples, as different phantom experiments and ex-vivo biological tissues, this providing the suitability of the method to be applied for the polarimetric analysis of samples.

Disclosures

No conflicts of interest, financial or otherwise, are declared by the authors.

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First Author received the M.Sc. degree in physics and the Ph.D. degree in physics at the Autonomous University of Barcelona, Barcelona, Spain, in 2006 and 2011, respectively. His research interests include liquid crystal displays and their application to diffractive optics, as well as the implementation of polarimeters and their use in biological applications. He has been a postdoctoral scientist in the Laboratoire de Physique des Interfaces et des Couches Minces (LPICM) of the École Polytechnique (France), in 2011–12 and in 2013–2014, where he has worked in the optimization and implementation of a polarimeter able to operate in the infrared spectrum, and in the analysis of polarimetric information for its application to materials characterization. He is an Associated Professor at the Autonomous University of Barcelona since 2016. He is a Member of the SPIE and of SEDOPTICA.

Caption List

Fig. 1 Optical scheme of the used Mueller polarimeter.

Fig. 2 (a) Picture of the experimental system; (b) Image of a ruler placed on a slice of pork, for image resolution calculation.

Fig. 3 (a) Tank filled with Intralipid diluted in water and the metallic ruler (Sample A). The sample is located in a sample-holder to be measured with the polarimeter. The scattering effect is clearly observed; (b) Chicken neck for the ex-vivo experiment. The red square shows the measured ROI.

Fig. 4 Comparison between different PG configurations obtained from: MM coefficients (a, c, e, g, i and k); and from standard PG procedures (b, d, f, h, j and l).

Fig. 5 Intensity absolute differences for the PG configurations: (a) C1, (b) C3, (c) C4; (d) and C3-C4.

Fig. 6 (a) Cross-sections selected for the 4 number (blue line) and a ruler millimeter tick mark (red line); (b) Visibility (V) as a function of the ellipticity angle.

Fig. 7 (a) Ruler with stuck scotch types (Sample C); (b) Cross-section values of the red line in Fig. 7(c) (black empty squares) and Fig. 7(d) (red circles) ;(c) C3-C4 PG image for right-handed circular light; and (d) C3-C4 PG image for left-handed circular light.

Fig. 8 Experimental Mueller matrix of the Sample C measured at 625 nm.

Fig. 9 (a) Experimental Mueller matrix of the Sample B measured at 470 nm; (b) 3x3 Mueller sub-matrix of the equivalent linear retarder for the Sample B.

Fig. 10 Cross-sections (related to the line shown in Fig. 9(a)) corresponding to the coefficients providing the best visibility for the Mueller matrix (black empty squares), the Retarder (red circles), the Depolarizer (brown triangles) and the Diattenuator (green empty triangles).

Video 1 PG based function f_{MM} calculated from the Mueller matrix of the Sample A. Different frames are related to different ellipticity values.

Video 2 PG based function f_{MM} calculated from the Mueller matrix of the Sample B.

Video 3 PG based function f_{MM} calculated from the equivalent Diattenuator matrix (D_i) for the Sample B.

Video 4 PG based function f_{MM} calculated from the equivalent Depolarizer matrix (D_e) for the Sample B.

Video 5 PG based function f_{MM} calculated from the equivalent Retarder matrix (Ret) for the Sample B.

Table 1 Mean absolute difference and standard deviation σ for different PG channels.