Murdoch, Craig S. and Kusch, Jonas and Flockhart, Gordon M.H. and Graham, Duncan and Faulds, Karen and Uttamchandani, Deepak (2017) Effect of nanoparticle morphologies on signal strength in photoacoustic sensing. In: IEEE SENSORS 2017 - Conference Proceedings. IEEE, Piscataway, N.J.. ISBN 978-1-5090-1013-4 , http://dx.doi.org/10.1109/ICSENS.2017.8234390

This version is available at https://strathprints.strath.ac.uk/64502/

Effect of Nanoparticle Morphologies on Signal Strength in Photoacoustic Sensing

Craig S. Murdoch*, Jonas Kusch*, Gordon M. H. Flockhart*, Duncan Graham**, Karen Faulds**, Deepak Uttamchandani*

*Centre for Microsystems and Photonics,
**Centre for Molecular Nanometrology,
University of Strathclyde,
Glasgow, UK.

Abstract—**Spherical gold nanoparticles with a plasmonic extinction peak at 532 nm and two sizes of star shaped gold nanoparticles with plasmonic extinction peaks at 532 nm and 600 nm were synthesised and introduced into tissue phantoms as exogenous absorbers. The photoacoustic signals generated from the three different nanoparticle morphologies embedded in tissue the phantoms is compared. The effect of nanoparticle concentration on the generated photoacoustic signal strength was also investigated for the spherical nanoparticles. At an excitation laser wavelength of 532 nm, the spherical gold nanoparticles were shown to produce the greatest photoacoustic response.**

Keywords—*photoacoustic; gold nano-stars; gold nano-spheres; nanoparticles;*

I. INTRODUCTION

Photoacoustic sensing and imaging are increasingly taking advantage of plasmonic nanoparticles as exogenous contrast agents. An important factor fuelling this trend is the relative ease with which plasmonic resonances of metallic nanoparticles, e.g. gold nanoparticles, can be engineered to align with commonly used visible and near infra-red laser wavelengths, thereby increasing the overall optical-to-acoustic conversion efficiency using affordable laser systems [1]. Building upon the optimization of this photoacoustic efficiency, the next evolutionary step is to use functionalized metallic nanoparticles so that very specific nanobiological and molecular interactions occurring on the surface of the nanoparticle can be photoacoustically probed [2].

Compared to alternative all-optical based probing techniques used for sensing changes in biological tissue, such as fluorescence or Raman microscopy which require bi-directional propagation of light, the photoacoustic based technique has the advantage of requiring uni-directional light propagation, and therefore the adverse impact of light scattering in tissue on the detected signal is significantly reduced [3]. Consequently, photoacoustic sensing, mediated by functionalized nanoparticles, has the potential to probe nanobiological and molecular interactions from, generally greater depth - up to a few centimeters in biological tissue - compared to the microscopies mentioned above [4], and this has recently generated considerable interest in this technique. This paper reports work on in-house synthesis of (non-functionalized) gold nanoparticles of different geometrical shapes and optical extinction profiles, and subsequently compares their photoacoustic signal response at a fixed wavelength using a laser-excited and piezo-transducer based photoacoustic sensing system.

II. SYNTHESIS AND OPTICAL CHARACTERISATION OF NANOPARTICLES

A. Synthesis Steps

Colloidal gold nanoparticles were prepared in both spherical and star shapes . Star shaped gold nanoparticles have a lower molar extinction coefficient than spheres but their absorption peak can be tuned to longer wavelengths thereby enabling photoacoustic sensing systems to employ lower cost infra-red laser diode sources [5]. The star shaped nanoparticles were synthesised in two different sizes. Gold stars were synthesised using a facile, "one-pot" process combining a growth solution, gold nanoparticle seeds and a reducing agent. The growth solution is a combination of sodium tetrachloroaurate and silver nitrate. A solution of ascorbic acid was used as the reducing agent and 12 nm gold nanoparticles where used as star seeds. The spikes of the star grow on top of the seed and the final star size, and peak extinction wavelength, is dictated by the ratio of growth solution to seed. A higher growth solution to seed ratio will produce longer spikes and a longer peak absorption wavelength. Spherical gold nanoparticles were prepared using a simple sodium citrate reduced synthesis method [6].

B. Optical Characterisation

The optical properties of each shape and size of nanoparticle was investigated using ultraviolet-visible spectroscopy. Fig. 1 shows the extinction spectra of the two different sizes of stars. One size of star nanoparticle has a peak extinction wavelength at 532 nm and a FWHM of 100 nm. The second star size has a peak extinction at 600 nm and a FWHM of 350 nm. This indicates a star diameter of approximately 15 nm with spike lengths of ~3 nm and ~6 nm respectively [5]. The dashed line plots in Fig. 1 show the extinction spectra of nanoparticle doped gelatin. The decreased extinction is due to a decrease in concentration because of the addition of gelatin. This indicates that the addition of nanoparticles to gelatin does not alter their optical properties. Fig. 2. shows the extinction spectra of the spherical gold nanoparticles. These nanoparticles

have a peak extinction wavelength at 532 nm and a FWHM of 150 nm. The diameter of the spherical nanoparticles has been confirmed to be around 45 nm by SEM which agrees with the peak absorption [1], [7].
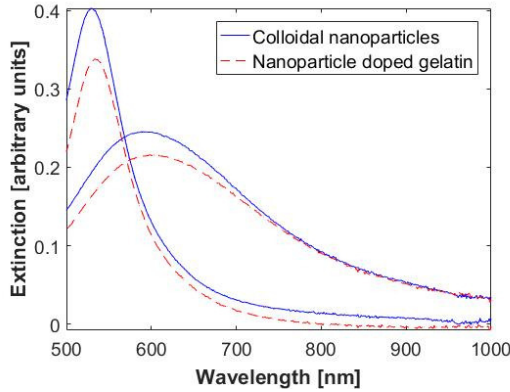

Fig. 1. Extinction spectra of two different sizes of star shaped gold nanoparticles in colloid (solid line) and in gelatin (dashed line).
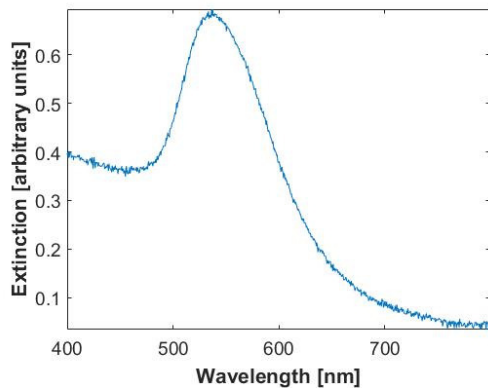

Fig. 2. Extinction spectrum of spherical gold nanoparticles.

III. EXPERIMENTAL APPROACH

A. Fabrication of Phantoms

Tissue phantoms made of gelatin were used to evaluate and compare the photoacoustic response of each type of nanoparticle. The phantoms are composed of 10% porcine gelatin so that they mimic the mechanical properties of real tissue. They are doped with nanoparticles to enhance their optical absorption properties and in turn enhancing their optical-to-acoustic conversion. Phantoms were prepared by dissolving porcine gelatin powder into the nanoparticle colloid which was heated using a water bath. This mixture was then poured into a mould and refrigerated to set. Visual inspection of the cured phantoms indicates uniform distribution of nanoparticles. Cube shaped phantoms of dimension 1 cm^3 and 4 cm^3 have been made using custom moulds. Three 4 cm^3 phantoms were made and each was doped with 9 μgml^{-1} of the spherical nanoparticles or one of the two sizes of star shaped nanoparticles. As shown in Fig. 3, six 1 cm^3 phantoms were also produced and doped with

different concentrations of spherical nanoparticles from 30 μgml^{-1} to 5 μgml^{-1}. Each phantom was removed from refrigeration and allowed to heat up to room temperature before any measurements were taken.

Fig. 3. 1 cm^3 tissue phantoms with concentrations 30 μgml^{-1}, 25 μgml^{-1}, 20 μgml^{-1}, 15 μgml^{-1}, 10 μgml^{-1} and 5 μgml^{-1}, from left to right, of the spherical nanoparticles.

B. Optical Characterisation

The photoacoustic sensing arrangement consists of three parts; a pulsed excitation laser for generation of photoacoustic ultrasound, an ultrasonic transducer for detection of the ultrasonic signals and an oscilloscope which doubled as a fast analogue-to-digital converter for acquisition and digitization of the ultrasonic signals. A frequency doubled, pulsed Nd:YAG laser with a wavelength of 532 nm producing pulses of 10 ns duration was used as the excitation laser. A piezoelectric transducer with a central frequency of 10 MHz and a bandwidth of 10 MHz has been used to detect ultrasound from inside the tissue phantoms. An Agilent Infiniium oscilloscope has been used for acquisition of photoacoustic signals using a high speed photodiode to produce a trigger signal from the laser pulse. To compare the photoacoustic signal strength of the three different nanoparticle morphologies, the laser pulse energy used was 23 mJ with a shot to shot standard deviation of 3.5 mJ. For measurements of the photoacoustic signal strength using different spherical nanoparticle concentrations the laser pulse energy used was lower at 14.2 mJ with a standard deviation of 0.186 mJ.

IV. RESULTS AND DISCUSSION

A 70 mm focal length lens was used to focus the 532 nm Nd:YAG laser inside the gelatin based phantom generating a photoacoustic signal. The 10 MHz transducer was acoustically coupled to a perpendicular face of the phantom with ultrasound gel. For each phantom, 16 ultrasound waveforms, Fig. 4, were acquired and their average calculated. The digitised signals are then transferred to a computer for processing. The photoacoustic response of each type of nanoparticle has been quantified by taking the absolute value of the Hilbert transform of each ultrasound waveform to calculate a waveform envelope. Each point on this envelope was then summed to give a single value which represents the photoacoustic signal strength. For identical illumination conditions, Table 1 shows that the spherical gold nanoparticles produced an average photoacoustic signal strength of 6.4 a.u. The star shaped gold nanoparticles with extinction peaks at 532 nm and 600 nm produced photoacoustic signal strengths of 4.7 a.u. and 3.9 a.u. respectively. Fig. 5 shows the change in photoacoustic signal strength as the concentration of

the gold spherical nanoparticles is changed from 0 to 30 μgml⁻¹. As can be seen the signal strength sharply increases from 5 a.u. to 10 a.u. from the un-doped reference gelatin phantom (0 μgml⁻¹) to the doped sample with 5 μgml⁻¹. From 5 μgml⁻¹ to 30 μgml⁻¹ the photoacoustic signal strength increases more slowly from 10 a.u. to 13 a.u.
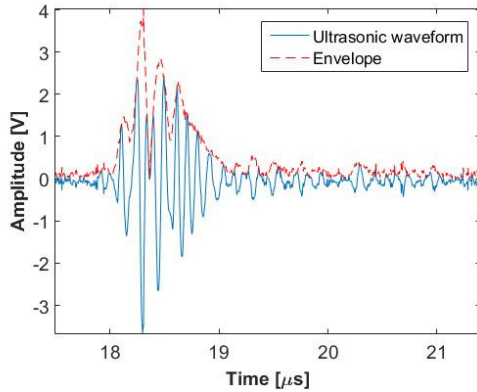

Fig. 4. Example of an ultrasound waveform (solid line) acquired using the photoacouistic sensing system and the waveform envelope (dashed line) calculated by taking the absolute value of the Hilbert transform.

Table 1. Signal strength of the photoacoustic response of spherical gold nanoparticles with a peak extinction at 532 nm and two sizes of star shaped gold nanoparticles with peak extinctions at 532 nm and 600 nm.

Shape	Sphere	Star	Star
Peak Extinction [nm]	532	532	600
Signal Strength [arb. units]	6.4	4.7	3.9
Standard Deviation	0.7	0.4	0.3

The star shaped gold nanoparticles that have an extinction peak at 532 nm are resonant with the emission wavelength of the excitation laser. This is the reason they generated a greater photoacoustic signal strength compared to the star shaped nanoparticles with an extinction peak at 600 nm. The 532 nm spherical nanoparticles produced the greatest photoacoustic signal strength as they have a molar extinction coefficient two orders of magnitude greater than the stars and so absorb light more effectively. Although the spherical nanoparticles generated a higher photoacoustic response at a laser wavelength of 532 nm this may not translate to higher wavelengths. Unlike star shaped nanoparticles, spherical nanoparticles are limited to a maximum extinction peak of 600 nm.

The first data point in Fig. 5 corresponds to a control phantom where the concentration of spherical gold nanoparticles is zero. It can be seen that the inherent absorption properties of the gelatin produced a small photoacoustic signal strength of 5 a.u. To establish a clear trend more measurements need to be obtained between the concentrations of 0 and 5 μgml⁻¹. From 5 μgml⁻¹ to 30 μgml⁻¹ the photoacoustic response increases linearly.
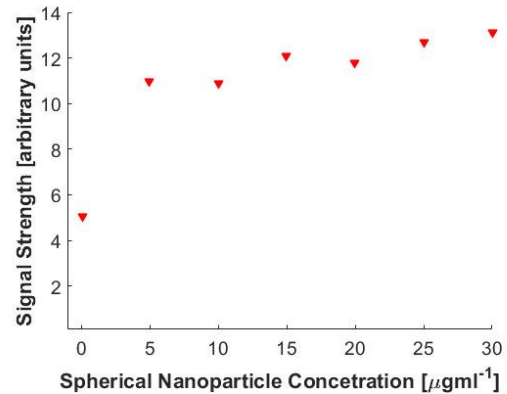

Fig. 5. Signal strength of photoacoustic response of spherical gold nanoparticles for concentrations from 0 to 30 μgml⁻¹.

V.   CONCLUSION

An in-house photoacoustic sensing setup has been used to compare the photoacoustic response of three different nanoparticle morphologies. One size of spherical gold nanoparticles and two sizes of star shaped gold nanoparticles have been synthesised and characterised when embedded in a tissue phantom. It was found that at a laser wavelength of 532 nm the spherical nanoparticles generated the strongest photoacoustic signal strength. It has also been shown that the photoacoustic signal approximately doubles when comparing an un-doped phantom to a 5 μgml⁻¹ doped phantom. As the nanoparticle concentration increases from 5 μgml⁻¹ to 30 μgml⁻¹ the photoacoustic signal strength generated continues to increase linearly but at a slower rate.

REFERENCES

[1]   A. Feis, C. Gellini, P. R. Salvi, and M. Becucci, "Photoacoustic excitation profiles of gold nanoparticles," *Photoacoustics*, vol. 2, no. 1, pp. 47–53, 2014.

[2]   J. Weber, P. C. Beard, and S. E. Bohndiek, "Contrast agents for molecular photoacoustic imaging," *Nat. Publ. Gr.*, vol. 13, no. 8, pp. 639–650, 2016.

[3]   S. L. Chen, L. J. Guo, and X. Wang, "All-optical photoacoustic microscopy," *Photoacoustics*, vol. 3, no. 4, pp. 143–150, 2015.

[4]   L. V Wang *et al.*, "Photoacoustic tomography: in vivo imaging from organelles to organs.," *Science*, vol. 335, no. 6075, pp. 1458–62, 2012.

[5]   H. de Puig, J. O. Tam, C.-W. Yen, L. Gehrke, and K. Hamad-Schifferli, "Extinction Coefficient of Gold Nanostars," *J. Phys. Chem. C*, vol. 119, no. 30, pp. 17408–17415, 2015.

[6]   P. C. Stevenson, "A STUDY OF THE NUCLEATION AND GROWTH PROCESSES I N THE SYNTHESIS OF," vol. 55, no. c, 1951.

[7]   P. K. Jain, K. S. Lee, I. H. El-Sayed, and M. A. El-Sayed, "Calculated absorption and scattering properties of gold nanoparticles of different size, shape, and composition: Applications in biological imaging and biomedicine," *J. Phys. Chem. B*, vol. 110, pp. 7238–7248, 2006.