

1 **The use of near-infrared systems for investigations of haemodynamics in human *in vivo***
2 **bone tissue: A systematic review**

3 *Running Title:* NIR for haemodynamic bone measurements.

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1 **Abstract:**

2 A range of technologies using near infrared (NIR) light have shown promise at providing real
3 time measurements of haemodynamic markers in bone tissue *in vivo*, an exciting prospect
4 given existing difficulties in measuring haemodynamics in bone tissue. This systematic
5 review aimed to evaluate the evidence for this potential use of NIR systems, establishing their
6 potential as a research tool in this field. Major electronic databases including MEDLINE and
7 EMBASE were searched using pre-planned search strategies with broad scope for any *in vivo*
8 use of NIR technologies in human bone tissue. Following identification of studies by title and
9 abstract screening, full text inclusion was determined by double blind assessment using
10 predefined criteria. Full text studies for inclusion were data extracted using a predesigned
11 proforma and quality assessed. Narrative synthesis was appropriate given the wide
12 heterogeneity of included studies. Eighty eight full text studies fulfilled the inclusion criteria,
13 57 addressing laser Doppler flowmetry (56 intra-operatively), 21 near infrared spectroscopy
14 and 10 photoplethysmography. The heterogeneity of the methodologies included differing
15 haemodynamic markers, measurement protocols, anatomical locations and research
16 applications, making meaningful direct comparisons impossible. Further, studies were often
17 limited by small sample sizes with potential selection biases, detection biases, and wide
18 variability in results between participants. Despite promising potential in the use of NIR light
19 to interrogate bone circulation, the application of NIR systems in bone requires rigorous
20 assessment of the reproducibility of potential haemodynamic markers and further validation
21 of these markers against alternative physiologically relevant reference standards.

22

23 **Keywords:**

24 Bone; haemodynamics; near infrared; emerging technologies; optical systems.

1 **Introduction**

2 Bone is a dynamic and vascular tissue, dependent on this perfusion to meet its metabolic
3 demands. However, measuring the haemodynamics of the osseous vasculature is difficult
4 with existing imaging modalities due to the high density and mineral content of bone.

5 Imaging protocols typically involve nuclear medicine scans, positron emission tomography
6 (PET) or contrast enhanced magnetic resonance imaging (MRI) which are expensive, have
7 limited clinical access, involve injections and do not readily allow longitudinal evaluation. In
8 addition, these techniques do not allow evaluation of oxygen saturation within the tissue, as
9 these modalities can only measure markers of gross perfusion and blood volume based on
10 rates of radiopharmaceutical or gadolinium contrast uptake [1].

11 Near infrared (NIR) optical systems are a potential solution. They have the advantages of
12 being non-invasive, non-destructive, non-ionising, inexpensive and allowing repeat or
13 continuous measurements. NIR optical systems involve transmitting and receiving
14 designated optical wavelengths using probes at an anatomical site. These systems take
15 advantage of the difference in absorption characteristics of oxygenated and deoxygenated
16 haemoglobin to record markers of bone haemodynamics in real time including tissue
17 oxygenation, perfusion, blood flux and blood volume [2]. Although NIR light only penetrates
18 human tissue superficially, systems have been shown to be able to record data non-invasively
19 through *in vivo* tissue to depths of up to 4 cm [3].

20 NIR optical systems are already established research tools in muscle physiology and
21 transcranial cerebral circulation [4, 5]. The use of transcranial NIR optical systems,
22 demonstrates that NIR light can penetrate bone tissue, and raises the possibility of its use in
23 assessing bone haemodynamics. Development of NIR optical systems could benefit research
24 in a range of bone pathologies with suspected vascular components, such as the earlier

1 detection, prevention and monitoring of haematopoietic malignancies, osteoporosis, non-
2 osteoporotic fragility fractures, slow fracture healing and forms of arthritis. The primary aim
3 of this systematic review is to gauge the existing knowledge base on the ability of NIR
4 optical systems to measure haemodynamic markers of blood supply in bone tissue, and to
5 establish their potential as a research tool in this field.

6 **Methods**

7 An initial scoping review suggests no previous systematic review on this topic has been
8 performed, therefore a diverse but relatively small evidence base was expected. As such
9 broad search criterion were established for studies investigating *in vivo* bone tissue at any
10 anatomical bony site in human participants. Studies using NIR optical systems in either
11 healthy or diseased human populations (or both) were considered eligible. Any optical
12 system utilising NIR wavelengths (600-1050 nm) using a haemodynamic marker that could
13 give insight into the haemodynamic state of the bone tissue sampled was considered eligible.
14 This could include systems measuring haemodynamic markers of blood flux, oxygen
15 saturation, oxygenated or deoxygenated haemoglobin concentration changes or blood
16 volume. Any indication for utilising the NIR optical systems was eligible, including
17 validation for a particular application, diagnosis of disease states, prognostic assessment,
18 longitudinal monitoring or screening purposes.

19 Given the broad scope of the review, a wide range of reference standards were eligible, such
20 as bone biopsy for measuring oxygenation of bone tissue; MRI, nuclear medicine or
21 angiographic protocols for measuring bone perfusion; or, direct clinical observation of tissue
22 perfusion intra operatively. Again, allowing for broad search criterion, a comparator test or
23 external reference standard for results was desirable, but not essential for study eligibility.
24 There were no restrictions on the geographical location or year of publication for studies, but

1 only studies published in English were eligible. Case studies of individual participants were
2 excluded, as were opinion pieces, reviews and editorials.

3 Search Strategy

4 Pre-planned search strategies using medical subject headings and keywords were developed
5 around key inclusion criteria for searches using MEDLINE and EMBASE online databases.
6 Grey literature databases including conference abstracts, theses, and unpublished works were
7 searched, including Web of Science, Proquest, OpenSIGLE, OpenGrey, and the British
8 Library EThOS database. At this point the reference list and further citations of any eligible
9 studies were hand searched. Authors were contacted where clarification or full text access
10 was required. All searching was carried out by the primary author who then removed
11 duplicates and screened the returned results based on title and abstract. The remaining
12 studies were considered for inclusion based on a blinded full text assessment by two
13 independent reviewers (RM and FC). Upon agreement of eligible studies, the primary author
14 independently extracted relevant key data using a pre-piloted data extraction proforma
15 (extracted data is presented in Supplementary Materials 1). Searches were performed in
16 September 2015, with a repeated addendum search of MEDLINE and EMBASE performed
17 prior to publication.

18 Assessment of Risk of Bias

19 Identified studies were also scrutinised by the primary author across 6 domains of potential
20 intrinsic biases using the Cochrane based Risk of Bias Assessment Tool for Non-randomised
21 Studies (RoBANS) tool to form an overall judgement of reporting quality as either “good”,
22 “fair” or “poor” [6]. External applicability and generalisability of studies was also assessed
23 using these categorical criterion. Methodological patterns or trends for “unclear” or “high”
24 areas of risk of bias were identified and their potential effects are discussed in context within

1 the narrative synthesis of the review (extended assessment results are presented in
2 Supplementary Materials 2).

3 Data Synthesis

4 Due to the clinical and methodological heterogeneity of the identified studies, statistical
5 synthesis via meta-analysis was not appropriate. As such, narrative synthesis of identified
6 studies has been performed primarily synthesised around the NIR optical systems of interest
7 and grouped around the anatomical locations or target conditions investigated. Discussion is
8 also in context of the haemodynamic markers employed, types of participants, and
9 comparators. The review also includes discussion on the strength of the evidence
10 accumulated including consideration of the risk of bias of individual studies, patterns in
11 biases, the consistency of results across studies, the applicability of results across the general
12 population, as well as the strengths and limitations of the review process. Further detail on
13 the protocol for the review are registered on the PROSPERO database [7].

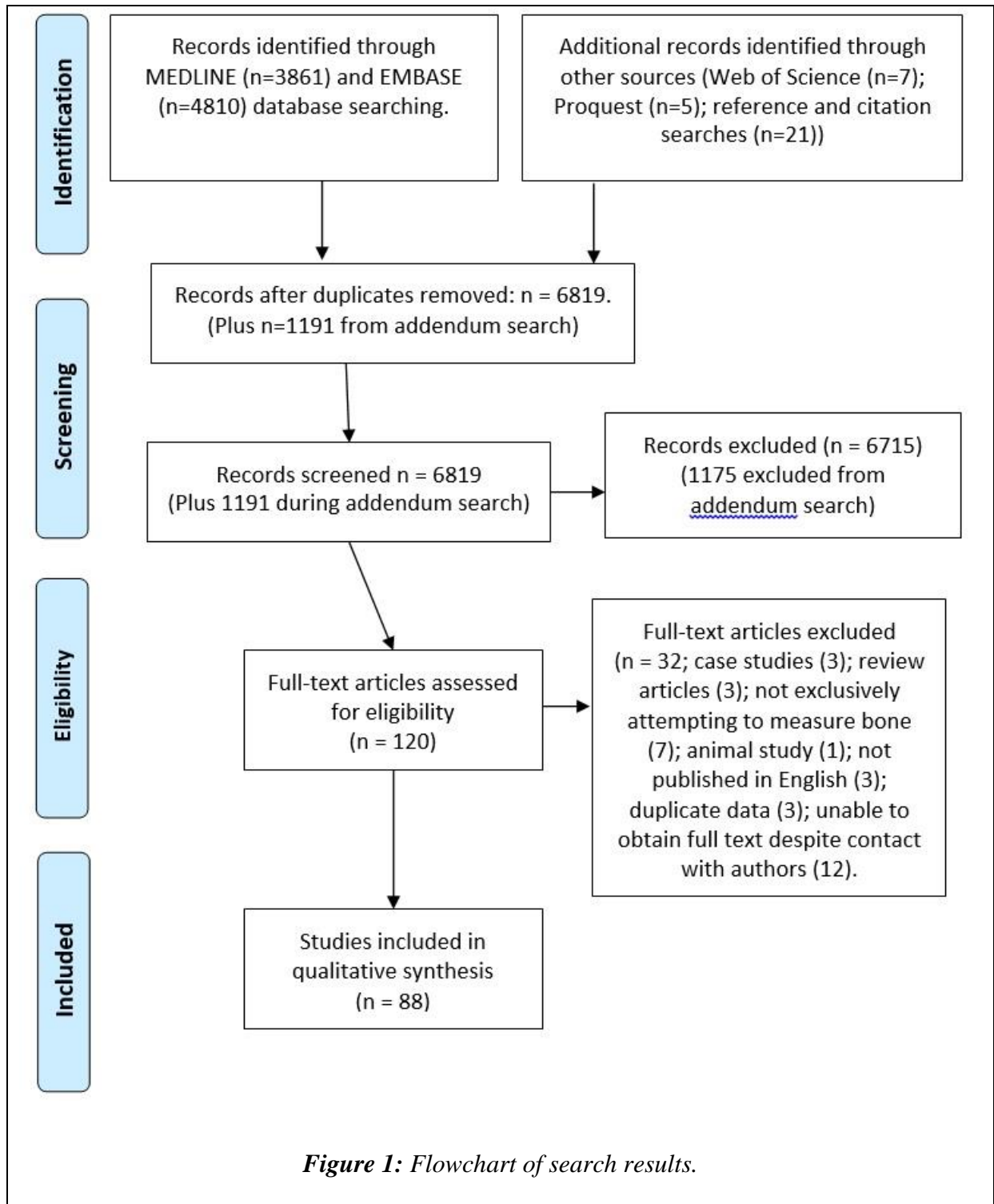
14 Results

15 Overview of Findings

16 A summary of search results and data extraction is presented in Figure 1 and Supplementary
17 Materials 1. Eighty eight studies were included for full text analysis. These were
18 predominately peer reviewed journal articles along with 5 conference proceedings [8-12] and
19 2 theses [13, 14]. Study publication dates ranged from 1987 to 2017 and there was wide
20 geographical variation with publications based in 13 different countries.

21 Twenty one studies were identified using near infrared spectroscopy (NIRS) [3, 8, 11, 13, 15-
22 30] and 10 studies were identified using photoplethysmography (PPG) non-invasively on *in*
23 *vivo* bone tissue [10, 24, 31-38]. Fifty seven studies were identified using laser Doppler
24 flowmetry (LDF) *in vivo* [9, 12, 14, 39-94] of which 56 were intra operative. Only one study

1 using LDF attempted to measure bone non-invasively [92]. Most studies were in adult
 2 populations with only 7 of the 56 LDF studies including paediatric populations [41, 46, 70-
 3 72, 78, 91].



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1 System Characteristics

2 Near Infrared Spectroscopy (NIRS)

3 Studies most commonly utilised “continuous wave” NIRS systems using spatially resolved or
4 modified Beer-Lambert law algorithms. These systems utilise at least 2 or 3 discrete
5 wavelengths of NIR light in the first NIR window (600 nm-1200 nm) to detect changes in
6 oxygenated and deoxygenated haemoglobin concentrations by taking advantage of their
7 different attenuation properties. This also allows these systems to measure oxygen saturation
8 and total haemoglobin concentration changes in the tissue sampled. The oxygen saturation is
9 the mean saturation across the arterioles, capillaries and venules. All were using reflectance
10 spectroscopy (light scattered back from tissue) apart from transmission spectroscopy (light
11 scattered through tissue) studies looking at the calcaneus [8, 22, 30] and mandible [21, 23].
12 For reflectance spectroscopy, probe spacing (affecting the depth of tissue measured) varied
13 from 10 mm [13, 19, 25], 20 mm [13], 25 mm [8, 20], 30 mm [15-18, 26], and 40 mm [3, 18].
14 Temporal resolution typically ranged from 1 second [17] to 12 seconds [20, 30].
15 Use of time resolved spectroscopy systems are reported in five studies [8, 20, 22, 29, 30].
16 These allow measurements of absorption and scattering coefficients for bone tissue and
17 therefore absolute concentrations of oxygenated and deoxygenated haemoglobin are
18 calculated with participants at rest (in μM) [8, 19, 20, 22, 23]. Farzam et al. 2013 also reports
19 on use of a frequency domain based NIRS system utilising 15 NIR laser sources (5 each at 3
20 different wavelengths) based around 2 photomultiplier detectors [19].
21 Six studies used NIRS systems utilising a broadband spectrum of NIR light enabling the
22 system to calculate absolute concentrations of haemoglobin and in some cases also water,
23 collagen, mineral and lipid content in the bone tissues sampled [8, 20, 22, 23, 28-30].

1 Additionally, four studies also measured markers of blood flow rates utilising emerging
2 diffuse correlation spectroscopy technology [8, 20, 27, 30].

3 Photoplethysmography (PPG)

4 We identified 10 PPG studies from two research groups investigating the patella and tibia
5 [10, 24, 31-38]. These studies utilised bespoke PPG systems making use of an isobestic 804
6 nm NIR wavelength to measure the amplitude of pulsatile flow in bone tissue based on
7 attenuation changes in reflected signal. When reported, inter-probe spacing ranged from 15-
8 25 mm. Some studies also measured overlying skin tissue, utilising a less penetrative
9 wavelength in the visible range (either 526 nm or 560 nm). All studies used “peak to peak”
10 amplitude during pulsatile flow as their primary outcome measure, typically measured and
11 averaged over a 30-60 second period to gain a mean value representing the strength of
12 pulsatile flow. Changes were then typically compared to baseline measurements during
13 and/or after an intervention in either relative (i.e. percentage change) or absolute terms (in
14 Volts).

15 Laser Doppler Flowmetry (LDF)

16 Most studies reported the use of a commercial LDF system utilising a monochromatic
17 wavelength typically at 632 nm, 780 nm, 785 nm, or 830 nm. LDF systems derive a measure
18 of flowmetry from the Doppler frequency shift induced by the moving red blood cells.
19 Changes in the frequency power spectrum of the reflected light provide a measure of the
20 concentration of moving red blood cells (blood flux or flowmetry) in arbitrary units
21 (described as perfusion units, flux units, or detector signal measured in milliVolts). A mean
22 amplitude of pulsatile flow is calculated over a set period (typically 60s or less). Comparison
23 of these values across participants should be done cautiously, and typically these values are

1 used to assess relative changes following a vascular challenge (either expressed as absolute
2 change or relative percentage change).

3 LDF systems only measure to a depth typically less than 4 mm [95], and therefore 56 of 57
4 studies involve intra operative use of LDF with probe placement directly on bone or intra-
5 osseous measurements. Two studies utilised laser speckle techniques involving laser light
6 interference from a tissue surface and mapping blood flux to produce a 2D flowgraphy “heat”
7 map. These were used intra-operatively to study the flux in the surface of the bone tissue up
8 to a depth of 2mm, namely the femoral head [50] and the cochlea promontory [73].

9 Study Characteristics

10 Studies looking to investigate bone tissue non-invasively used a wide range of superficial
11 anatomical bone sites including the tibia, calcaneus, radius, ulna, greater trochanter of the
12 femur, patella, mandible and manubrium/sternum. In addition, invasive LDF procedures also
13 investigated deeper bone tissue including the proximal femur, acetabulum, cochlea, maxilla,
14 metatarsal, humerus and lumbar vertebrae. Studies could broadly be split into two categories.
15 Firstly, studies investigating the feasibility of NIR technologies for measuring bone tissue in
16 healthy adults. Secondly, studies that used previous evidence to defend the validation of NIR
17 technologies, and applied these systems for a physiological research purpose.

18 Feasibility Studies

19 The most substantial work demonstrating NIRS and PPG could truly measure haemodynamic
20 parameters of bone tissue non-invasively was based around studies that demonstrated
21 significantly lower oxygen extraction rates and reperfusion rates in bone tissue compared to
22 adjacent muscle tissue. These two parameters were derived during and after extended arterial
23 occlusions of the leg respectively, reflecting bone’s lower metabolic rate compared to muscle
24 [11, 15, 16, 19, 26]. Three studies demonstrate a non-significant confounding contribution of

1 superficial tissue to PPG and NIRS measurements of the patella and tibia by selectively
2 altering superficial tissue haemodynamics either through the localised introduction of
3 vasodilating or vasoconstricting elements such as gentle compression [32], cold packs [13],
4 nitro-glycerine patches [32] and liniment [34]. However, Klasing et al. 2003 does report a
5 systematic influence from superficial tissue on NIRS measurements, although it is noted this
6 is a much earlier study [26].

7 Binzoni et al. 2013 was the only study focusing purely on non-invasive LDF measurements
8 in bone through the skin surface. Feasibility work was undertaken in healthy participants
9 with a source/detector spacing of 1.5 cm giving enough penetrative depth to measure
10 superficial bone *in vivo* at four anatomical sites [92]. Diffuse correlation spectroscopy
11 technology with NIRS also provides blood flux information non-invasively but at greater
12 tissue depths and may supersede LDF here given the added advantages of NIRS systems [30].

13 Other applications of NIRS and PPG systems applied to healthy populations included
14 haemodynamic measurements taken during positional changes such as leg extension, or head
15 up/down tilt to demonstrate oxygen saturation and blood volume changes [10, 13, 17, 24, 37,
16 38]. Four studies examined the effects of positive and negative external pressure changes
17 using lower body pressure chambers on the amplitude of PPG pulsatile flow and oxygen
18 saturation [24, 31, 33, 38]. In the case of Larsson et al. 2014, the use of hyperbaric chambers
19 and variable respired oxygen levels were also used to observe their effects on bone
20 haemodynamics at the patella [31]. These studies concluded that the use of pressure
21 alterations may have applications for therapy by mimicking weight-bearing physiology in a
22 microgravity environment, or for potential therapeutic applications involving vascular
23 mechanisms in bone. Three studies investigated the effects of exercise on tibia and patella
24 haemodynamics using exercise bikes [13], rowing machines [13, 28] or high intensity

1 quadriceps workloads [36]. For time resolved NIRS systems, absolute measurements could
2 be taken on healthy adult participants simply at rest [8, 20, 22, 29, 30].

3 Physiology Research Applications

4 Studies using NIR optical systems for physiological research in diseased populations were
5 predominately LDF studies, focusing on dynamic flux changes in response to fixed stimuli or
6 during various stages of a surgical intervention. Some studies used case-control designs to
7 correlate these results with other clinically relevant observations assessing the predictive role
8 of intra-operative LDF on outcomes.

9 The proximal femur and hip joint represented one of the biggest areas of interest for research
10 involving LDF in bone tissue, with 19 studies [9, 39, 41-44, 48-50, 54, 58, 65-67, 76, 77, 82,
11 84, 91] found investigating a range of clinical applications including osteonecrosis (either
12 idiopathic, steroid induced, or following neck of femur fracture) [50, 65, 82, 84], approaches
13 to hip resurfacing arthroplasty [9, 39, 42, 67, 77] or total hip replacement following arthritis
14 [44, 48, 49, 58, 66, 82], femur-acetabular impingement [43], hip joint debridement [76], and
15 congenital developmental problems [41, 54, 91]. Specifically most studies took
16 measurements from the femoral head and neck, but others also looked at intra-trochanteric
17 regions [65, 84], the greater trochanter [48, 58, 66], proximal femoral shaft [58], medial
18 calcar [58], or acetabulum [49, 54].

19 There were 6 studies identified that used LDF intraoperatively to investigate patellar blood
20 flux changes before and after positional changes or different surgical manoeuvres in adult
21 patients having total knee arthroplasty [52, 55, 57, 61, 74, 81]. Five studies used LDF
22 technology to measure blood flux in the manubrium [40] or sternum [51, 59, 60, 75] during
23 and following open cardiac surgery involving the internal mammary arteries. Seven studies
24 looked at the use of LDF to measure blood flux in the mandible [14, 62, 88], maxilla [90, 93,

1 94] or both [63, 89] for patients undergoing maxilla-facial or dental surgery including
2 wisdom tooth removal [14], dental implants [62, 88, 94], osteomyelitis [89] or corrective
3 maxillary surgery [63, 90, 93]. Eleven studies reported on the use of LDF to assess blood
4 flow in the bony wall of the cochlea [45, 46, 68-73, 79, 80, 87] to investigate a range of inner
5 ear pathologies including otosclerosis [73, 80], Meniere's disease [79], curative treatment for
6 uncontrolled drooling [68, 69] or idiopathic or congenital hearing loss and surgical
7 implantation of hearing aid devices [46, 70-72]. Four studies from the same group
8 investigated the use of LDF technology for assessing bone perfusion during the surgical
9 debridement of bone tissue in adult patients compromised by acute trauma (such as open
10 fracture) and/or osseous infections such as osteomyelitis [47, 83, 85, 86].

11 LDF has also been used to investigate successful post-operative monitoring of fibular bone
12 grafts [78]; intra-osseous haemodynamic measurements of thoracic and lumbar vertebral
13 bodies during mimicked unilateral and bilateral ligation [53]; for investigating the predictive
14 ability of humeral head fracture patterns for determining the risk of humeral ischemia [56];
15 and for investigating the blood flux in the first metatarsal head during corrective surgery [12,
16 64].

17 The clinical utility of NIRS has been explored in the mandible [18, 21, 23] and sternum [25].
18 In a case-control manner, mandibular conditions such as osteoradionecrosis post radiotherapy
19 [21, 23], and fibular grafting post tumour removal [18], as well as chest wall measurements
20 taken post cardiac surgery [25] were explored. Results showed potential for the use of NIRS
21 for post-operative monitoring using oxygen saturation measurements, however the small
22 sample sizes and shortage of adverse outcomes precluded the ability to identify a diagnostic
23 predictive threshold.

1 Naslund et al., 2007 used PPG to investigate haemodynamic differences between cases of
2 Patello-Femoral Pain Syndrome with age, gender and body mass index (BMI) matched
3 controls. This study demonstrated cases of Patello-Femoral Pain Syndrome had significantly
4 reduced PPG pulsatile amplitude when flexing their affected knee to 90 degrees for 5
5 minutes, supporting the hypothesised ischaemic element to pathogenesis [35].

6 Reliability of NIR systems

7 Broadly speaking, study results were predictive of the expected haemodynamic changes
8 during interventions. However, across most studies wide variability in results between
9 participants was evident, especially across applications of LDF. Crucially, no studies were
10 identified specifically addressing the reliability or reproducibility of NIR optical systems.
11 Studies that did attempt to assess reliability typically did this in a superficial or *ad hoc* way in
12 small samples without statistical analysis of agreement or reliability. Approaches included
13 comparing contralateral results, analysing repeat measurements for their variability (either in
14 the same or different sessions), or simple comparison of results with existing literature in
15 animal studies or involving different tissue types.

16 This wide variation in results may prohibit the development of useful diagnostic thresholds
17 for NIR optical systems [60, 76]. Wide biological variability in vascular measurements is a
18 known barrier to research in this field [96] and this is also reflected in suboptimal
19 reproducibility in alternative modalities for measuring bone tissue haemodynamic markers
20 such as MRI [97, 98].

21 Variability is likely to be affected by the heterogeneity of bone tissue and the small sampling
22 volume of NIR optical systems (particularly LDF) with sampling of small arterioles or less
23 vascular trabecular striate potentially altering readings. It is important to tease out what
24 variation in results is attributable to measurement error and what reflects normal

1 physiological ranges. Likewise, most studies typically used only one, or a small group, of
2 operators. Few studies took repeat measurements, or multiple readings at adjacent sites,
3 which is suggested due to this small penetration depth and sampling volume of NIR optical
4 systems.

5 Other potential factors affecting reliability specific to LDF studies include the comparison of
6 results in studies where the probe is placed non-invasively, directly on the bone surface, or
7 intra-osseously. The sensitivity of probes to movement also means stable probe placements
8 during surgical operations is important and some studies reported holding probes by hand or
9 using bespoke probe holders [40, 51]. Some study designs involved having to move probes
10 in between measurements to facilitate surgery, which can introduce measurement error given
11 the small sampling volume and potential for measuring a different vascular bed when probes
12 are repositioned [77, 81]. In addition, as these LDF studies were intra operative the effects of
13 anaesthesia, blood loss during surgery and direct impact of surgery cannot be discounted as
14 sources of error [41]. When placing probes intra-osseously, the effect of drilling on intra-
15 osseous blood flow is unknown and flushing of the probes is required to remove clotting
16 around the measurement site, which could otherwise prohibit flow and affect readings.

17 Quality Assessment

18 An overview of quality assessment ratings is presented in Supplementary Materials 2. A
19 general methodological issue with many studies was the poor description of inclusion and
20 exclusion criteria, recruitment strategies, and summary information of important participant
21 demographics. In the absence of specific details, this opens many studies to potential
22 criticism of selection biases. Similarly, most feasibility studies involved small cohorts of
23 healthy, young and predominately normal BMI participants, raising concerns around the
24 generalisability of non-invasive applications of NIR systems in wider demographics and

1 disease states. Many studies also included small sample sizes of participants without sample
2 size justification.

3 Attrition or incomplete results were rarely directly addressed. How incomplete results are
4 handled can lead to biases in the accuracy of results and so it is important these are reported
5 in context with study findings, especially at the early stages of the technological development
6 of NIR optical systems. Generally, most studies had a low risk of performance and reporting
7 bias as testing protocols were clearly pre-stated and all participants received the same testing.

8 In the case of studies investigating the potential feasibility of NIR optical systems on healthy
9 participants, detection bias was considered generally low, despite studies not always
10 reporting if testing and data analysis was strictly protocolled, or if acquisition and data
11 analysis was blinded to participant information/status. However, in studies investigating
12 different sub populations for physiological differences, this was deemed a more significant
13 potential bias risk, especially when LDF or oxygen saturation with NIRS was used as an
14 outcome measure, where probe placement can be easily adjusted for minor subjective
15 corrections in results, or the most suitable data could be selectively sampled for data analysis.

16 It is acknowledged that with intra operative LDF studies that in most cases LDF operators
17 were not blinded to their participant status as they were likely performing the surgical
18 procedures. As such, detection biases are hard to avoid.

19 Studies were all also deemed at risk of “other biases” as there are inherent unknowns around
20 the use of NIR optical systems for these applications in bone tissue, as relatively weak
21 validation exists. Along similar lines many studies involving NIRS and PPG systems reported
22 use of bespoke made systems, reducing the applicability of results as there is evidence for
23 systematic differences in haemodynamic measurements across commercial systems from
24 different manufacturers [99].

1 There was also an applicability issue evident when considering intra-operative LDF findings
2 to guide clinical practice or normal physiology. Often studies found reduced blood flux at
3 various stages during surgical interventions, but without the ability to take pre and post-
4 operative readings the clinical importance of these findings is hard to distinguish. Likewise,
5 obtaining healthy control data is also ethically difficult given the invasive approach taken.
6 Similarly, some studies only presented relative percentage changes in haemodynamic
7 markers with time. Whilst this demonstrates the responsiveness of NIR optical systems in
8 bone, the applicability of these results is limited without development of absolute
9 haemodynamic quantitative markers and threshold results for normal physiology that can
10 guide research into diseased states.

11 *Discussion*

12 A large number of studies have been identified utilising NIRS, PPG and LDF systems to
13 investigate bone tissue either non-invasively or intra-operatively. The wide heterogeneity in
14 anatomical sites and investigated applications demonstrates the demand for the types of
15 information NIR technology promises. The studies identified are predominately early stage
16 proof of concept type work which often illustrate the promise for future clinical and research
17 applications. However, there are a wide range of challenges that require addressing to
18 advance this field of research in bone health.

19 The need for further work on the reliability and reproducibility of NIR optical systems for
20 repeat measurements across different operators and participants has been identified.

21 Likewise, continued investigation around whether variability is biological or equipment
22 based (or both) is important, as this is still not clear from the literature. If physiological
23 variability is wide at an individual level, NIR optical systems may be unhelpful for
24 development of individual diagnostic thresholds, but NIR research could perhaps still

1 elucidate important haemodynamics differences between sub populations of interest given the
2 current lack of alternative research tools.

3 Few studies attempted to validate NIR optical system results against an external comparator
4 or reference standard, such as microangiography, MRI protocols, nuclear medicine and PET
5 protocols. However, those that did presented promising results [50, 56, 82]. External
6 validation remains crucial to give credence to future NIR optical systems. Alternatively,
7 confidence could be gained through correlation of other relevant indicators of bone health,
8 such as bone density, blood markers of bone metabolism, or longitudinal patient follow up
9 when used to guide operative cases.

10 Establishing the generalisability of results is also crucial to the development of these
11 technologies. This includes gauging the expected normal physiological variability expected
12 between different ethnicities, ages, genders and body habitus as well as during the operative
13 state. It appears the influence of overlying tissue on non-invasive measurements requires
14 careful consideration but may be overcome with continued technological advances. As
15 always, patient tolerability of protocols should also be considered, as well as ruling out any
16 potential negative impact of intra-operative use of LDF, which was not addressed by the
17 studies identified.

18 Technological advances in NIR optical systems holds the key to the future of this application.
19 The development of time-resolved NIRS systems promises the ability to measure absolute
20 concentrations of oxygenated and deoxygenated haemoglobin non-invasively with the patient
21 at rest. This facilitates easier measurement protocols and more appropriate data comparison
22 between participants. It may also help to address some of the variability in measurements
23 between different tissue types resulting from the significant variability in light scattering.
24 Likewise, the possible development of commercially available broadband NIRS systems can

1 allow the potential measurement of other relevant components of bone tissue such as mineral,
2 lipid, collagen and water concentration [8, 22, 29, 30]. With improved probe design the
3 ability to measure deeper tissues may also be feasible in the future.

4 Further work is required before NIR optical systems can be considered a valid and reliable
5 research tool of vascular bone health. However, the wide and varied literature base identified
6 in this review ultimately highlights the strong promise of this application of NIR optical
7 systems, which potentially offers real time, safe and inexpensive measurements of bone tissue
8 haemodynamics.

9

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