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Stokes-correlometry of polarization-inhomogeneous objects

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ABSTRACT

The paper consists of two parts. The first part presents short theoretical basics of the method of Stokes-correlometry description of optical anisotropy of biological tissues. It was provided experimentally measured coordinate distributions of modulus (MSV) and phase (PhSV) of complex Stokes vector of skeletal muscle tissue. It was defined the values and ranges of changes of statistic moments of the 1st-4th orders, which characterize the distributions of values of MSV and PhSV. The second part presents the data of statistic analysis of the distributions of modulus MSV and PhSV. It was defined the objective criteria of differentiation of samples with urinary incontinence.

Keywords: Stokes vector, correlometry, anisotropy, diagnostic.

1. THEORETICAL BASICS AND EXPERIMENTAL REALIZATION OF THE METHOD OF STOKES-CORRELOMETRY OF BIOLOGICAL LAYERS

1.1. Brief theory.

In the series of research works the possibility of polarimetry diagnostic[1-19] of optically anisotropic biological layers is demonstrated. Separate place in such investigations occupy laser polarimetry of optically thin (non-depolarizing) layers of biological tissues[20-22] and fluids[23-34]. At that high sensitivity of laser polarimetry techniques is achieved [9,11,13,16,17]. It is determined by the significant range of differences in average (within the test groups of biological layers and those under study) values of statistical points that characterize the distribution of polarization parameters (polarization azimuth and ellipticity) of the series of microscopice images [5,8-11,15,16,22,24,28]. To describe the correlation structure of the stationary distributions of the fields of complex amplitudes of laser light converted by optically anisotropic biological layers, one can use the following mutual spectral density matrix [35]

$$W_{i,j}(r_1,r_2)=E_i^*(r_1)\cdot E_j(r_2), i,j=x,y \tag{1}$$

Here r_1 and r_2 - the coordinates of the neighboring points in the field of laser radiation.

In this work we have to analyze the 4th (the degree of crystalization) Stokes vector parameter.

Using this matrix operator one can introduce the following expression for the "two-point" Stokes vector parameters

$$S_4=i\left[W_{yx}(r_1,r_2)+W_{xy}(r_1,r_2)\right]=i\left[E_x^*(r_1)E_y(r_2)+E_y^*(r_1)E_x(r_2)\right]. \tag{2}$$

Using relations (2),(3) the following algorithms to calculate the "two-point" Stokes vector parameters (hereinafter "Stokes-correlometry parameters" - SCP) can be obtained

$$S_4=\left[E_{y1}E_{x2}\sin\delta_1+E_{y2}E_{x1}\sin\delta_2\right]+i(E_{x2}E_{y1}\cos\delta_1+E_{x1}E_{y2}\cos\delta_2). \tag{3}$$

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In order to simplify the physical analysis of manifestations of optical anisotropy (distributions of optical axes directions $\rho(r) = arctg\dfrac{E_y(r)}{E_x(r)}$ and phase shifts $\delta(r)$ between the orthogonal components ($E_x(r), E_y(r)$) of laser wave amplitude) of biological layers

$$\begin{cases} S_4 = \mathrm{Re}\, S_4 + \mathrm{Im}\, S_4 = \left(\sin\delta_1 + ctg\rho_2 tg\rho_1 \sin\delta_2\right) + i\left(\cos\delta_1 + ctg\rho_2 tg\rho_1 \cos\delta_2\right); \\ |S_4| = \sqrt{\left[1 + ctg^2\rho_2 tg^2\rho_1 + 2ctg\rho_2 tg\rho_1 \cos(\delta_2 - \delta_1)\right]}; \\ ArgS_4 = arctg\left(\dfrac{\cos\delta_1 + ctg\rho_2 tg\rho_1 \cos\delta_2}{\sin\delta_1 + ctg\rho_2 tg\rho_1 \sin\delta_2}\right). \end{cases} \quad (4)$$

In the approximation of weak phase fluctuation relation (5) has the form of

$$\begin{cases} |S_4| = 1 + ctg\rho_2 tg\rho_1; \\ ArgS_4 = arctg\left(\dfrac{1 + ctg\rho_2 tg\rho_1}{\delta_1 + \delta_2 ctg\rho_2 tg\rho_1}\right). \end{cases} \quad (5)$$

1.2. Experimental results of the method of Stokes-correlometry

Measurement of the coordinate distributions values is carried out in the experimental arrangement of Stokes-polarimeter[16,31-34].

The modulus $\left|\left(S_{i=4}(\Delta x, \Delta y)\right)\right|$ of the were calculated by the following ratios

$$\left\{|S_4| = \sqrt{\left[\sqrt{I_0(r_2)I_{90}(r_1)}\sin\delta_1 + \sqrt{I_0(r_1)I_{90}(r_2)}\sin\delta_2\right]^2 + \left[\sqrt{I_0(r_2)I_{90}(r_1)}\cos\delta_2 + \sqrt{I_0(r_1)I_{90}(r_2)}\cos\delta_1\right]^2}\right. . \quad (6)$$

$Arg\left(S_{i=4}(\Delta x; \Delta y)\right)$ were calculated by the following ratios

$$\left\{ ArgS_4 = arctg\left(\frac{\left[\sqrt{I_0(r_2)I_{90}(r_1)}\cos\delta_2 + \sqrt{I_0(r_1)I_{90}(r_2)}\cos\delta_1\right]}{\left[\sqrt{I_0(r_2)I_{90}(r_1)}\sin\delta_1 + \sqrt{I_0(r_1)I_{90}(r_2)}\sin\delta_2\right]}\right). \quad (7)$$

Here I_0 and I_{90} - the intensities at the orientation of transmission plane of polarizer 0^0 and 90^0; δ_i - phase shifts between the orthogonal components of the amplitude of the laser radiation in the points with coordinates r_1 and r_2 .The results of experimental approbation of the Stokes-correlometry method of optically-thin layer of muscular tissue are illustrated by a series of dependencies (maps and histograms of m_{ik} distributions), which are shown in Fig. 1.

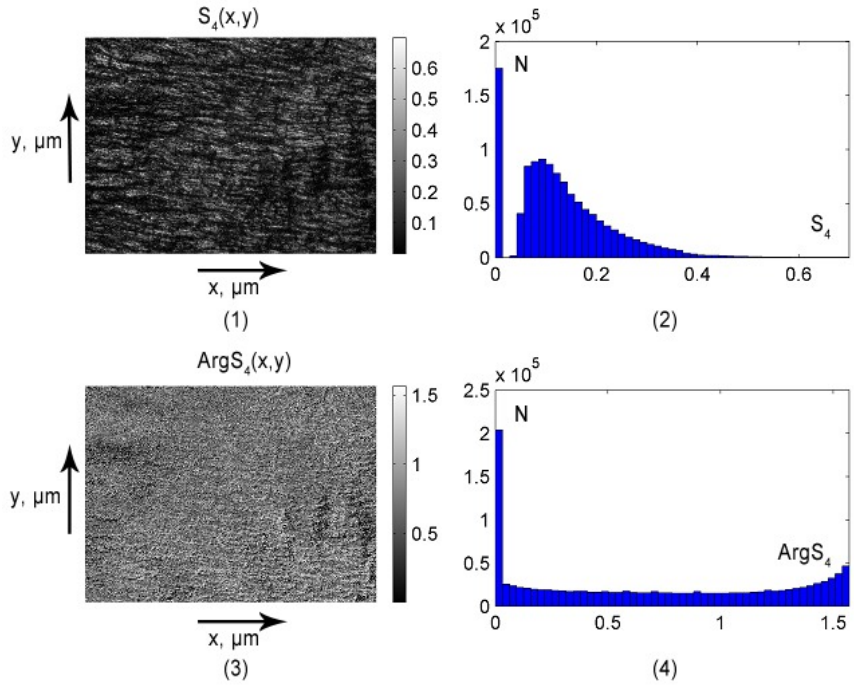

Fig. 1. Maps (fragments (1),(3)) and histograms (fragments (2, 4) of the distributions of the values of MSV and PhSV of the histological section of skeletal muscle.

Table 1 presents the results of statistic analysis (statistical moments of the 1st-4th orders $Z_{i=1;2;3;4}$) of coordinate distributions of $|j_{ik}|$ of coordinate distributions of MSV and PhSV of images of skeletal muscle.

Table 1. Statistical moments $Z_{i=1;2;3;4}$ of the distributions of the values of MSV and PhSV of skeletal muscle

$Z_{i=1;2;3;4}$	$\lvert S_4 \rvert$	$ArgS_4$
$Z_{i=1}$	0.27	0.89
$Z_{i=2}$	0.34	1.21
$Z_{i=3}$	0.15	0.47
$Z_{i=4}$	0.26	0.82

It was defined the individual sensitivity of the value of $Z_{i=1;2;3;4}$ to the peculiarities of coordinate distributions of MSV $|S_4|$ и PhSV $ArgS_4$. Such a fact was chosen as the basic for applied biomedical usage of statistic analysis of coordinate distributions of MSV $|S_4|$ и PhSV $ArgS_4$.

2. CLINICAL APPLICATION OF STOKES-CORRELOMETRY OF UTERUS WALL TISSUE IN DIFFERENTIAL DIAGNOSTICS OF PROLAPSE

2.1. Objects of investigation

It was investigated two groups of samples of biopsy of uterus wall tissue:

- healthy donors – control group 1 (30 samples);
- affected by prolapse - group 2 (30 samples).

Histological sections were produced due to the standard technique on the freezing microtome.

2.2. Experimental results

The set of Figs. 2, 3 presents the results of Stokes-correlometry mapping of the histological sections of the uterus wall of healthy donors (Fig.2) and affected by prolapse (Fig. 3).

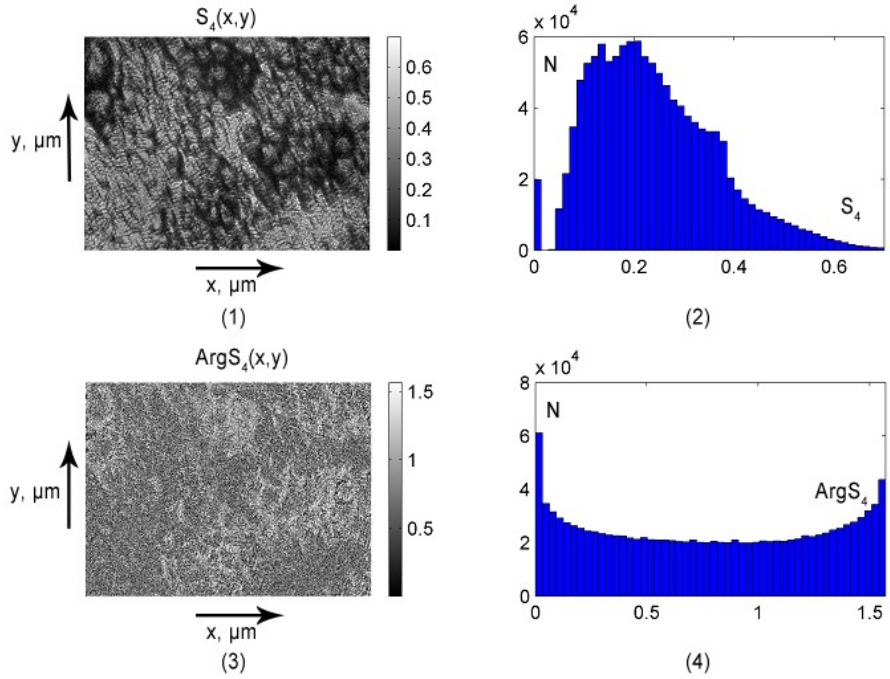

Fig. 2. Maps (fragments (1),(3)) and histograms (fragments (2, 4)) of the distributions of MSV for healthy donors (fragments (1),(2)) and with prolapse (fragments (3),(4)).

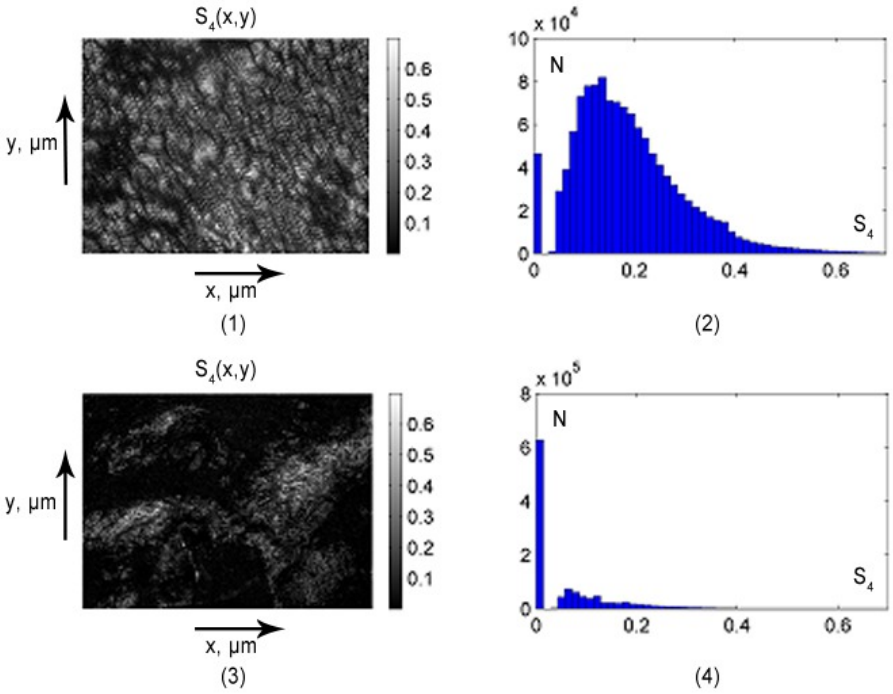

Fig. 3. Maps (fragments (1),(3)) and histograms (fragments (2, 4)) of the distributions of PhSV for healthy donors (fragments (1),(2)) and with prolapse (fragments (3),(4)).

For the possible clinical application of the Mueller matrix mapping method for each group of samples the operating characteristics, typical for evidence-based medicine[36-38] that determine the diagnostic power of the method are determined, namely – sensitivity ($Se = \frac{a}{a+b}100\%$), specificity ($Sp = \frac{c}{c+d}100\%$) and balanced accuracy ($Ac = \frac{Se+Sp}{2}$), where a and b – the number of correct and incorrect diagnoses within group 2; c and d – the same within group 1 – Table 2.

Table 2. Balanced accuracy of Stokes-correlometry

Ac,%	$\lvert S_4 \rvert$	$ArgS_4$
$Z_{i=1}$	91%	77%
$Z_{i=2}$	93%	79%
$Z_{i=3}$	96%	82%
$Z_{i=4}$	93%	85%

It was reached a good ($Ac(ArgS_4) = 82\% - 85\%$) and excellent ($Ac(\lvert S_4 \rvert) = 93\% - 96\%$) level of balanced accuracy of the method of differential diagnostics of healthy donors and with prolapse.

CONCLUSIONS

Short theoretical basics of the method of polarization-interference Stokes-correlometry mapping of polycrystalline structure of biological layers were provided.
It was demonstrated the results of experimental approbation of such method and defined the distributions of Jones-matrix elements of polycrystalline film of urine.
The differentiation of such samples was realized with good and excellent levels of balanced accuracy of differentiation between normal uterus wall tissue and with prolapse.

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