



UNIVERSITI PUTRA MALAYSIA

MINIMIZATION OF ENTRANCE SURFACE DOSE AND CRITICAL ORGAN DOSE FOR MEDICAL RADIOGRAPHY USING **OPTIMIZATION PROCEDURES**

LOTF ALI MEHDIPOUR NASSAB RABOR FS 2010 2





MINIMIZATION OF ENTRANCE SURFACE DOSE AND CRITICAL ORGAN DOSE FOR MEDICAL RADIOGRAPHY USING OPTIMIZATION PROCEDURES

LOTF ALI MEHDIPOUR NASSAB RABOR

MASTER OF SCIENCE UNIVERSITI PUTRA MALAYSIA 2010





MINIMIZATION OF ENTRANCE SURFACE DOSE AND CRITICAL ORGAN DOSE FOR MEDICAL RADIOGRAPHY USING OPTIMIZATION PROCEDURES

By LOTF ALI MEHDIPOUR NASAB RABOR

Thesis Submitted to the School of Graduate Studies, Universiti Putra Malaysia, in Fulfillment of the Requirements for the Degree of Master of Science.

February 2010



This thesis dedicates to

My dear wife (NHHID),

My parents, my brothers, my sisters,

And

My dear niece (Sahar)



Abstract of thesis presented to the Senate of Universiti Putra Malaysia, in fulfillment of the Requirement for the degree of Master of Science

MINIMIZATION OF ENTRANCE SURFACE DOSE AND CRITICAL ORGAN DOSE FOR MEDICAL RADIOGRPHY USING OPTIMIZE PROCEDURES

By

LOTF ALI MEHDIPOUR NASSAB RABOR

February 2010

Chairman : Professor Dr. Elias Bin Saion, PhD

Faculty : Science

In hospitals, clinics, nursing homes, and medical laboratories, diagnostic radiography is extensively used to view internal structures of a patient and to aid radiologists and doctors diagnose and treat illness and injury. The most common medical radiography is by passing x-rays through the body and captures the image of the patient by means of a sensitized film. This radiographic procedure must feature the system of dose optimization and limitation known as the practice of ALARA (as low as reasonably achievable) recommended by the International Commission on Radiological Protection. The measurements of the entrance surface dose (ESD) and the critical organ dose (COD) in common medical radiography are very important to ensure the dose limit received by the patient in a single radiographic exposure must fulfill the ALARA principle. The most useful way to evaluate ESD is either by indirect measurement on a phantom using an ionization chamber or thermo luminescent dosimeter (TLD) or using calculation based on mathematical model.



In this work, the ESD values measured by the indirect method on RANDO phantom using ionization chamber and by direct method on volunteer patients using TLD. The ESD values of X-ray examinations on chest posterior-anterior (PA) and lateral (lat), skull PA and lat, cervical spine anterior-posterior (AP) and lat, thoracic spine AP and lat, lumbosacral spine AP and lat, abdomen AP, and pelvis AP were found to be 0.15, 0.75, 1.82, 1.16, 0.70, 0.73, 3.6, 5.40, 4.74, 11.7, 4.55, and 3.26 mGy respectively. The IAEA (1996) ESD values are 0.4, 1.5, 5, 3, -, -, 7, 20, 10, 30, 10, and 10 mGy respectively and the NRPB (2000) values are 0.2, 1, 3, 1.6, -, -, 3.5, 10, 6, 14, 6, and 4 mGy respectively. Patients weighting between 65 to 75 kg, from two hospitals in Iran were volunteered to be placed with TLD 100 (LiF) chips during Xray examinations on chest, skull, cervical, thoracic, lumbar, abdomen, and pelvis to measure the ESD values. For each radiographic procedure 10 patients were selected and in one sachet three TLD chips were used. The measured ESD values on RANDO phantom and patients were compared with the guidance levels provided by the International Atomic Energy Agency (IAEA) and the National Radiological Protection Board (NRPB).

For the indirect measurement of COD values, RANDO phantom and TLDs were used during ESD X-ray measurements. The COD values measured on chest PA for lens, thyroid, and testis were 0.11, 0.12, 0.09 mGy respectively, on chest lat for lens, thyroid and testis were 0.12, 0.14, 0.1 mGy respectively, on skull PA for lens, thyroid and testis were 0.20, 0.19, 0.13 mGy respectively, on skull lat for lens, thyroid and testis were 0.90, 0.20, 0.15 mGy respectively, on cervical spine AP for lens, thyroid and testis were 0.24, 0.67, 0.20 mGy respectively, on cervical spine lat for lens, thyroid and testis were 0.19, 0.62, 0.17 mGy respectively, on thoracic AP



for lens, thyroid and testis were 0.20, 0.68, 0.18 mGy respectively, on thoracic spine lat for lens thyroid and testis were 0.21, 0.25, 0.20 mGy respectively, on lumbosacral spine AP for lens thyroid and testis were 0.24, 0.27, 1.37 mGy respectively, on lumbosacral spine lat for lens thyroid and testis were 0.22, 0.24, 0.40 mGy respectively, on abdomen AP for lens thyroid and testis were 0.23, 0.24, 1.89 mGy respectively, and on pelvis AP for lens thyroid and testis were 0.24, 0.26, 1.23 mGy respectively. In this study the level of stochastic effect of X-rays in diagnostic radiology was lowered in comparison with the guidance levels of IAEA and NRPB. These results enable us to propose the COD values for common general radiography procedures.



Abstrak tesis yang dikemukakan kepada senat Universiti Putra Malaysia sebagai memenuhi keperluan untuk ijazah Master Sains

MENGURANGKAN DOS PERMUKAAN SINAR DATANG DAN DOS ORGAN KRITIKAL UNTUK KEGUNAAN RADIOGRAFI PERUBATAN MENGUNAKAN KAEDAH PENGOPTIMUMAN

Oleh

LOTF ALI MEHDIPOUR NASSAB RABOR

February 2010

Pengerusi : Profesor Dr. Elias Bin Saion, Ph.D

Fakulti : Sains

Di hospital, klinik, rumah pemulihan dan makmal perubatan, radiograf dianostik kerap digunakan untuk melihat struktur dalaman seorang pesakit dan bertujuan membantu pakar radiologi dan doktor melakukan diagnostik dan merawat penyakit dan kecederaan. Lazimnya radiografi penibutan adalah diperolehi dengan menyinarkan sinar-X menembusi jasad dan merekodkan imej pesakit dengan sekeping filem. Prosedur radiograf perlu menyatakan system pengoptimum dan penghadan dos dikenali sebagai ALARA (serendah mungkin yang boleh dicapai) yang disyorkan oleh Badan Antarabangsa mengenai Perlindungan Sinaran. Pengukuran dos permukaan sinar datang (ESD) dan dos organ kritikal (COD) dalam amalan biasa radiograf perubatan adalah amat penting untuk memastikan had dos yang diterima oleh pesakit dalam pendedahan radiograf tunggal perlu memenuhi prinsip ALARA.lazimny cara paling utama untuk menentukan ESD adalah samada melalui pengukaran terus keatas fentom menggunakan kebuk pengionan atau



dosimeter termopendarcahaya (TLD) atau dengan menggunakan pengiraan berdasarkan model matematik.

Dalam kajian ini, ESD diukur dengan kaedah tak terus menggunakan fentom Rando dan kebuk pengionan dan dengan kaedah terus menggunakan pesakit dan pengesan TLD. Nilai ESD bagi pemerikasaan bagi torkas posterior-anterior (PA) dan lateral (lat), tengkorak PA dan lat, spina servikal anterior-posterior (AP) dan lat, spina torkas AP and lat, spina lumbosakral AP and lat, abdomen AP, and pelvis AP mempunyai nilai masing-masing 0.15, 0.75, 1.82, 1.16, 0.70, 0.73, 3.6, 5.40, 4.74, 11.7, 4.55, dan 3.26 mGy. Nilai ESD bagi IAEA (1996) 0.4, 1.5, 5, 3, -, -, 7, 20, 10, 30, 10, dan. 10 mGy manakala nilai untuk NRPB (2000) ialah 0.2, 1, 3, 1.6, -, -, 3.5, 10, 6, 14, 6, dan 4 mGy. Bagi keadah terus, pesakit-pesakit yang beratnya diantara 65 dan 75 kg yang mendapat rawatan daripada dua hospital telah secara sukalera diletakkan cip TLD 100 (LiF) semasa pemeriksaan sinar-X dada, tengkorak, servikal, torkas, lumbar, abdomen, and pelvis to mengukur nilai ESD berkaitan. Untuk setiap kaedah radiograf sebanyak 10 pesakit telah dipilih dan tiga cip TLD diletakkan dalam setiap lokasi pengesan. Nilai-nilai ESD yang diukur dengan menggunakan fentom RANDO dan pesakit telah dibandingkan dengan paras dos yang dicadangkan oleh Agensi Tenaga Atom Antarabansa (IAEA) dan Badan Perlindungan Sinaran kebangsaan (NRPB).

Untuk mengukur nilai COD secara tak terus, fantom RANDO dan pengesan TLD telah digunakan. Nilai COD yang diukur semasa pemerikasan sinar-X dada PA untuk kanta, kelenjar tiroid, dan testis adalah masing-masing 0.11, 0.12, 0.09 mGy, penerikasaan dada lat untuk kanta, kelenjar tiroid, dan testis adalah masing-masing 0.12, 0.14, 0.1 mGy, pemeriksaan tengkorak PA untuk kanta, kelenjar tiroid and



testis adalah masing-masing 0.20, 0.19, 0.13 mGy, pemeriksaan tengkorak lat untuk kanta, kelenjar tiroid dan testis adalah masing-masing 0.90, 0.20, 0.15 mGy, pemeriksaan spina servikal AP untuk kanta, kelenjar tiroid dan testis adalah masingmasing 0.24, 0.67, 0.20 mGy, pemeriksaan spina servikal lat untuk kanta, kelenjar tiroid dan testis adalah masing-masing 0.19, 0.62, 0.17 mGy, pemeriksaan spina torkas AP untuk kanta, kelenjar tiroid dan testis adalah masing-masing 0.20, 0.68, 0.18 mGy, pemeriksaan spina torkas lat untuk kanta, kelenjar tiroid dan testis adalah masing-masing 0.21, 0.25, 0.20 mGy, pemeriksaan spina on lumbosacral spine x-ray AP for lens thyroid and testis adalah masing-masing 0.24, 0.27, 1.37 mGy, pemeriksaan spina lumbosakral lat untuk kanta, kelenjar tiroid dan testis adalah masing-masing 0.22, 0.24, 0.40 mGy, pemeriksaan abdomen AP untuk kanta, kelenjar tiroid dan testis adalah masing-masing 0.23, 0.24, 1.89 mGy, dan pemeriksaan pelvis AP untuk kanta, kelenjar tiroid dan testis adalah masing-masing 0.24, 0.26, 1.23 mGy. Dalam kajian ini paras kesan stokastik sinar-X dalam radiology adalah lebih rendah berbanding dengan paras panduan oleh IAEA dan NRPB. Keputusan kajian ini membolehkan kita mencadangkan nilai COD bagi prosedur radiografi am biasa.



ACKNOWLEDGEMENTS

"Open your heart eye, to see the ghost

You will see any invisible thing

If you split the heart of any particle,

You will see a sun within it,,

At the end of this step of my graduate period has allowed for a bit of reflection, and

the many people who have contributed to both my work, and my life during of this

period of time.

First, I would like to express my full thanks and sincere gratitude to my great dear

supervisor, Professor Dr Elias Saion for all of guidance, discussions, unlimited

assistance and consultations; also I would like to thank my committee members, Mr.

Abd. Aziz Mohd Ramli, and Dr Halimah Mohammed Kamari, for their invaluable

suggestions, beneficial advices and their endless helps.

I wish to acknowledge my gratitude to all lecturers and staffs in physics department

of faculty of science and medical physics group of Malaysian institute of nuclear

research technology.

I also wish to acknowledge my gratitude to my dear wife for her encouragements,

her emotional supports, and her fortitude. I am grateful to my friend Mohammad Ali

Shafahi for his helps; also I would like to express my full thanks and sincere

gratitude to my dear parents for their efforts in my life time.

Lotf Ali Mehdipour

2010

UPM BR

 \mathbf{X}

I certify that a Thesis Examination Committee has met on 11.2.2010 to conduct the final examination of Lotf Ali Mehdipour nassab rabor on his Master thesis entitled "Minimization of entrance surface dose and critical organ dose for medical radiography using optimization procedures"in accordance with the Universities and University Colleges Act 1971 and the Constitution of the Universiti Putra Malaysia [P.U. (A) 106] 15 March 1998. The Committee recommends that the student be awarded the Master of Science.

Members of the Thesis Examination Committee were as follows:

Zainal Abidin Talib, PhD

Associate Professor Faculty of Science Universiti Putra Malaysia (Chairman)

Abdul Halim Shaari, PhD

Professor Faculty of Science Universiti Putra Malaysia (Internal Examiner)

Azmi Zakaria, PhD

Professor Faculty of Science Universiti Putra Malaysia (Internal Examiner)

Ahmad Termizi Ramli, PhD

Professor Faculty of Science Universiti Technology Malaysia Malaysia (External Examiner)

BUJANG BIN KIM HUAT, PhD

Professor and Deputy Dean School of Graduate Studies Universiti Putra Malaysia

Date:



This thesis was submitted to the senate of Universiti Putra Malaysia and has been accepted as fulfillment of the requirement for the degree of Master of Science. The members of the Supervisory Committee were as follows:

Elias Saion, PhD

Professor Faculty of science University Putra Malaysia

Halimah Mohammed Kamari, PhD

Senior Lecturer Faculty of science University Putra Malaysia

Abd Aziz Mhd Ramli, PhD

Researcher Malaysian Nuclear Agency MINT Malaysia

HASSANAH MOHD. GHZALI, PhD

Professor and Dean School of Graduate Studies University Putra Malaysia

Date: 8 April 2010



DECLARATION

I hereby declare that the thesis is based on my original work except for quotations and citations, which have been duly acknowledged. I also declare that it has not been previously, and is not concurrently, submitted for any other degree at University Putra Malaysia or at any other institution.

(Signature)			
LOTF ALI N	MEHDIPOU	R NASSAB	RABOR

2010



TABLE OF CONTENTS

			Page
ABSTRAC	CT		i
ABSTRAE			v
ACKNOL		ENTS	viii
APPROVA		,	ix
DECLAR			xi
LIST OF			XV
LIST OF I LIST OF A		VIATIONS	xvi xvii
CHAPTEI	R		
1	INT	TRODUCTION	1
		General introduction	1
		Significance of study	2
		Problem statement	3
		Objective of the study	4
	1.5	Outline of the thesis	5
2	LIT	TERATURE REVIEW	
	2.1	Introduction	6
	2.2	ε	7
		2.2.1 Stochastic effects	8
	2.2	2.2.2 Deterministic effects	10
	2.3	6 6	12
		2.3.1 Diagnostic x-rays2.3.2 X-ray computed tomography	12 14
		2.3.3 Nuclear magnetic resonance imaging	14
		2.3.4 Diagnostic ultrasound	16
		2.3.5 Nuclear medicine	16
	2.4	Entrance surface dose	17
	2.5		19
	2.6	Anthropomorphic phantom	20
	2.7	Optimization in general radiography	21
	2.8	ALARA philosophy	22
3	TH	EORY	
	3.1	Medical radiography	24
	3.2		25
		3.2.1 Electromagnetic radiation	25
		3.2.2 Production of x-ray	27
		3.2.3 Bremsstrahlung or braking radiation3.2.4 Characteristic radiation	30
	3.3		30 31
	5.5	3.3.1 Photoelectric effect	32
		5.5.1 110000000000	<i>J</i> <u> </u>



			Rayleigh scattering	35
		3.3.3	ı e	35
	3-4		nce surface dose (ESD)	38
			Phantom	39
			Ionization chamber	40
	3-5		rs affecting radiation quality	41
		3.5.1		41
		3.5.2	1	41
			Filtration	42
			Inherent filtration	42
			Added filtration	42
			Collimation	43
	26	3.5.7		44
	3-6	3.6.1	rs affecting radiographic density Tube current	44 45
		3.6.2		45
		3.6.3		46
		3.6.4	C 1 \ \ 1 /	46
		3.6.5	Grid	48
			Filtration	48
			Patient factors	49
			Generator type	50
			Beam restriction	50
) Processing	51
	3-7		graphic contrast	51
		3.7.1	•	52
		3.7.2		53
		3.7.3	Patient factors	54
		3.7.4	Filtration	55
		3.7.5	Intensifying screen	56
			Image receptor (film)	56
	3.8	Critica	al organ dose (COD) and ALARA philosophy	58
		3.8.1	Shielding	58
			Time	59
		3.8.3	Distance	59
4	MAT	ERIAL	S AND METHOD	
	4.1	Mater	ials	61
		4.1.1	Phantom: Rando Alderson Phantom	63
		4.1.2	Radiography X-ray unit	62
		4.1.3	Ionization chamber	65
		4.1.4	Thermo luminescent dosimeter	66
	4.2	Instru	mentation	66
		4.2.1	Humidity meter	67
		4.2.2	Barometer and thermometer	67
		4.2.3	<i>C</i> ,	68
			Film-screen combination	68
		4.2.5	•	70
		4.2.6	Annealing system	70



	4.3	Methods	72
		4.3.1 Measurement of ESD on phantom	75
		4.3.2 Calibration of ionization chamber	74
		4.3.3 Geometry used for calculation of ESD	76
		4.3.4 Dose measurement in common Radiography	77
		4.3.5 Quality control of radiographs	82
		4.3.6 Measurement of critical organ dose by TLD	86
		4.3.7 Calibration method of TLD	87
		4.3.8 Geometry used for calculation of critical organ	dose 88
		4.3.9 Critical organ dose measurement	90
		4.3.10 Measurement of ESD on patient	90
5		RESUULTS AND DISCUSSION	
	5-1	Radiation quality measurement	92
		5.1.1 HVL measurement	92
		5.1.2 Measurement of effect of kVp on ESD	99
	5-2	Radiation quantity measurement	107
		5.2.1 Measurement of effect of mAs on ESD	107
		5.2.2 Measurement of effect of SID on ESD	111
	5-3	Measurement of Entrance surface dose (ESD)	117
		5.3.1 Comparative ESD measurement on patient	120
	5-4	Measurement of critical organ dose (COD)	123
		5.4.1 Critical organ dose (Lens)	127
		5.4.2 Critical organ dose (Thyroid)	128
		5.4.3 Critical organ dose (Testis)	129
6		CONCLUSION AND FUTURE WORK	
	6-1	Conclusion	131
	6-2	Future work and recommendations	132
		6.2.1 Speed of Film	133
		6.2.2 Critical Organ Dose (COD)	133
		REFERENCES	134
		BIODATA OF STUDENT	139



LIST OF TABLES

Table	F	age
4.1	calibration coefficient of ionization chamber in different kVp	76
4.2	evaluation criteria for some common medical radiography	83
5.1	suggested radiation factors for some common medical radiography	116
5.2	suggested entrance surface dose (ESD) values in mGy in present study on phantom and comparison with the recommended values of IAEA and NRPB.	119
5.3	comparison of ESD (mGy) measurements in patients, Rando phantom and values recommended from IAEA (1996) and NRPB (2000).	122
5.4	The critical organ (lens, thyroid and testis) doses (mGy) in general radiography measured by TLD on Rando phantom.	126



LIST OF FIGURES

Page	Fig	ure
3.1	Electromagnetic spectrum	26
3.2	Modern x-ray tube	29
3.3	Diagram of photoelectric effect	34
3.4	Photo electric effect	35
3.5	Schematic Diagram of Compton scattering	36
3.6	Schematic kinematic of Compton scattering	37
4.1	Rando phantom of man used in this work	62
4.2	Rando phantom is made up from thirty-five 2.5 cm thick transverse slices	62
4.3	Radiography X-ray machine	64
4.4	Control panel of x-ray machine	64
4.5	Ionization chamber (Radcal 9010) used in this work	65
4.6	Vacuum tweezers	66
4.7	Humidity meter	67
4.8	Barometer and thermometer	68
4.9	Image processor machine	69
4.10	Radiographic cassette	69
4.11	TLD readers Harshow 3500	71
4.12	Annealing system	71
4.13	Annealing process of TLD	72
4.14	Geometry used for measurement of ESD	76
4.12	Annealing system	68
4.13	Annealing process of TLDs	69



4.14	Geometry used for measurement of ESD	77
4.15	Geometry used for measurement of critical organ dose	89
4.16	Critical organ dose measurement by TLD	89
5.1	Out put with, Al – thickness, 55 kVp	93
5.2	Out put with, Al – thickness, 65 kVp	94
5.3	Out put with, Al – thickness, 70 kVp	94
5.4	Out put with, Al – thickness, 80 kVp	95
5.5	Out put with, Al – thickness, 90 kVp	95
5.6	Out put with, Al – thickness, 100 kVp	96
5.7	Out put with, Al – thickness, 110 kVp	96
5.8	X-ray Out put with, Al – thickness, for 55 kVp to 110 kVp	98
5.9	The linear Relation between HVL and applied anode voltage kVp	99
5.10	The entrance surface dose (ESD) (mGy) versus anode voltage (kV) in AP projection of abdomen X-rays.	100
5.11	Radiographic image taken at 46 mAs and 70 kV; SID 100 cm, field siz34×42 cm ² , film type green, film speed 400	102
5.12	Radiographic image taken at 6 mAs and 80 kV; SID 180 cm, field size 34×36 cm ² , film type green, film speed 400 (chest x-ray (PA	103
5.13	The entrance surface dose (ESD) (mGy) versus anode voltage (kV) in PA projection of chest X-rays.	104
5.14	The location of heart and lungs in chest region of human body	105
5.15	Comparative evaluations in ESD (mGy) versus voltage kVp between AP abdomen X-rays and PA chest X-rays	106
5.16	Relation between ESD (mGy) and mAs in abdomen (AP).	108
5.17	Relation between ESD (mGy) and mAs in Chest (PA).	109



5.18	Showing the radiation quality used.	110
5.19	Radiographic image of Skull (PA)	111
5.20	Relation between ESD (mGy) and SID (cm).	112
5.21	Relation between SID (Cm) and ESD (mGy).	114
5.22	Comparison between chest (PA) and skull (PA) examinations	115
5.23	Measured ESD values of various radiograph evaluations compared. With recommended values from IAEA (1996) and NRPB (2000).	117
5.24	Measured ESD values of various radiograph evaluations on patient compared with the ESD values that are measured on RANDO phantom in this study.	123
5.25	Measured lens COD (mGy) in 12 procedures.	127
5.26	Measured thyroid COD (mGy) in 12 procedures	129
5.27	Measured testis COD (mGy) in 12 procedures	130



LIST OF ABBREVIATIONS

ALARA As Low As Reasonably Achievable

AP Anterior - Posterior

BG Back ground radiation

CF Calibration Factor

COD Critical Organ Dose

Cm Centimeter

CPS Cycle per second

DNA Deoxyribonucleic Acid

DRL Diagnostic Reference Level

ESD Entrance Surface Dose

HVL Half Value Layer

HZ Hertz

IAEA International Atomic Energy Agency

ICRP International commission of Radiation Protection

KERMA Kinetic Energy Released in Material

Kev Kiloelectron volt

Kpa Kilopascal

kVp Kilovolt peak

Lateral Lateral

LiF Lithium Florid

mAs milliampere second

mbar millibar

MDD minimum Detectable Dose



mGy milligray

MINT Malaysian Institute of Nuclear research

Technology

MM millimeter

mR milliroentgen

NC nanocoulomb

PA Posterior - Anterior

Rad Radiation Absorbed Dose

RPM Round per minute

SID Source Image Distance

SSDL Secondary Standard Dose Laboratory

TLD Thermo Luminescent Dosimeter

UK United Kingdom

USA United State of America

μGy microgray

°C degree centigrade

oF degree fahrenheit



CHAPTER 1

INTRODUCTION

1.1 General introduction

X-ray was discovered in the 1895 by Wilhelm Conrad Roentgen by accident. He spent several weeks working in his laboratory to investigate the properties of X-rays and noticed that when he placed his hand between his energized tube and the barium platinocyanide-coated paper, he could see the bones of his hand glow on the paper with the fluoroscopic image moving as he moved his hand. He also produced a static radiograph of his wife's hand using this new radiation (Alexi A, 1995). This was the first radiograph of the world and has become an important step in physics and medicine. He proceeded to study them so thoroughly that within a very short period of time, he had identified the properties of X-rays that we recognized today.

In medical diagnostic radiology, X-ray creates images help diagnose the patient's medical conditions. The quality of the images produced depends partly on how much radiation is used, which is under the direct control of radiographers and radiologists. To produce a quality X-ray image, the amount of radiation transverse the patient depends on various factors such as type of examination, patient's physical characteristics, and condition of pathology to be imaged and several factors related to



instrumentation. One of the major goals of medical radiography is to minimize radiation dose to the patient without compromising the image quality needed to produce an accurate diagnosis (Seeram, and Patrick., 2006). This is the subject of the present study.

1.2 Significance of study

The basic principles of radiological protection as suggested by the International Commission of Radiological Protection (ICRP) are justification of the practice and optimization of protection. Justification is the first step in radiological protection, which has been accepted that, diagnostic exposure is justifiable only when there is a valid clinical indication, no matter how good the imaging performance may be, that every examination must result in a net benefit to the patient (IAEA, 2004). In the area of optimization in diagnostic radiology there is considerable scope for reducing dose without loss of diagnostic information, but the extent to which the measures available are used varies widely. The optimization of protection in diagnostic radiology does not necessarily mean the reduction of doses to the patient. It is paramount that the image obtained contains the diagnostic information as intended (IAEA, 2004).

The need to optimize the protection of patients results from the fact that medical exposures are by far the largest source of exposition of artificial origin. Diagnostic

