

Comparing different filtering and enhancement methods to evaluate the impact on the geometry reconstruction for medical images A.J. João, A.M. Gambaruto & A. Sequeira	179
Fast identification of individuals based on iris characteristics for biometric systems J.G. Rogeri, M.A. Pontes, A.S. Pereira, N. Marranghello, A.F. Araujo & J.M.R.S. Tavares	183
Monitoring feet temperature using thermography D. Bento, F.C. Monteiro & A.I. Pereira	189
Identification of foliar diseases in cotton crop A.A. Bernardes, J.G. Rogeri, N. Marranghello, A.S. Pereira, A.F. Araujo & J.M.R.S. Tavares	193
A local invariant features approach for classifying acrosome integrity in boar spermatozoa L.F. Robles, V. González-Castro, O. García-Olalla, M.T. García-Ordás & E. Alegre	199
Analysis of mixing of a clothoid based passive micromixer: A numerical study F. Pennella, S. Ripandelli, L. Ridolfi, F. Mastrangelo, M.A. Deriu, F.M. Montevecchi, U. Morbiducci, M. Rasponi, M. Rossi & C.J. Kähler	205
Flow visualization of trace particles and Red Blood Cells in a microchannel with a diverging and converging bifurcation  V. Leble, C. Fernandes, R. Dias, R. Lima, T. Ishikawa, Y. Imai & T. Yamaguchi	209
Does fluid shear stress represent the degree of a Red Blood Cell deformation?  M. Nakamura & S. Wada	213
Flow of Red Blood Cells through a microfluidic extensional device: An image analysis assessment T. Yaginuma, A.I. Pereira, P.J. Rodrigues, R. Lima, M.S.N. Oliveira, T. Ishikawa & T. Yamaguchi	217
An automatic method to track Red Blood Cells in microchannels D. Pinho, F. Gayubo, A. Isabel & R. Lima	221
Speech articulation assessment using dynamic Magnetic Resonance Imaging techniques S.R. Ventura, M.J.M. Vasconcelos, D.R. Freitas, I.M. Ramos & J.M.R.S. Tavares	225
The breast lesions characterization by b values variation in the DW-Magnetic Resonance Imaging A.A. Fernandes, M.B. Ribeiro, J.C. Janardo, S.D. Jaguegivane & M.E. Pereira	233
Efficient lesion segmentation using Support Vector Machines  JB. Fiot, L.D. Cohen, P. Raniga & J. Fripp	239
Multimodality imaging population analysis using manifold learning  JB. Fiot, L.D. Cohen, P. Bourgeat, P. Raniga, O. Acosta, V. Villemagne,  O. Salvado & J. Fripp	245
2D MRI brain segmentation by using feasibility constraints V. Pedoia, E. Binaghi, S. Balbi, A. De Benedictis, E. Monti & R. Minotto	251
Stochastic bone remodeling process: From isotropy to anisotropy N. Mellouli & A. Ricordeau	257
Carotid artery atherosclerosis plaque analysis using CT and histology F. Santos, A. Joutsen, J. Salenius & H. Eskola	261
Level set framework for detecting arterial lumen in ultrasound images A.R. Abdel-Dayem	267
Micromovement measurements of endosseous dental implants with 3D Digital Image Correlation (DIC) method A.T. Rodrigues, B.A. Neto & C.P. Nicolau	273
Monte Carlo simulation of PET images for injection dose optimization J. Boldyš, J. Dvořák, O. Bělohlávek & M. Skopalová	279
The use of medical thermal imaging in obstetrics R. Simões & C. Nogueira-Silva	285

# Monitoring feet temperature using thermography

# D. Bento & F.C. Monteiro

Polytechnic Institute of Bragança, ESTiGIPB, C. Sta. Apolonia, Bragança, Portugal

## A.I. Pereira

Polytechnic Institute of Bragança, ESTiG/IPB, C. Sta. Apolonia, Bragança, Portugal ALGORITMI, Minho University, Campus de Azurém, Guimarães, Portugal

ABSTRACT: Studies show that regular monitoring of feet temperature may limit the incidence of disabling conditions such as foot ulcers and lower-limb amputations. Infrared thermometry and liquid crystal thermography were identified as the leading technologies in use today. In this study, we analysed the maximum temperature and tested some mathematical models for the foot temperature distribution.

#### 1 INTRODUCTION

Diabetic foot (DF) ulcers are one of the major complications in diabetics, seriously affecting the quality of their lives. The possibility to measure the different aspects of DF and its ulcerative pathology gives to clinicians the chance to both evaluate and weigh up the different components contributing to the genesis and evolution of the cases and to monitor their clinical course as a consequence of the therapeutic interventions. Therefore, it is necessary to establish methods of prevention or early diagnosis for diabetic foot complications (Nishide et al., 2009).

The DF lesions are a combination of several risk factors acting simultaneously and can be triggered by peripheral diabetic neuropathy, peripheral vascular diseases and biomechanical changes. The decrease in sensory function in the foot and limitation of joint mobility are some early signs for the appearance of foot ulcers, meaning high risk of developing inflammations or other complications. These changes can be assessed using various techniques, thus preventing the appearance of ulcers and reducing the risk of foot amputation.

The use of thermal techniques to evaluate diabetic foot has largely remained a research topic (Lavery et al., 2004, Sun et al., 2006, Armstrong et al., 2007, Nagase et al., 2011). The authors believe that thermal techniques can be significantly useful in diabetic foot assessment, with the intent of determining risk of foot ulceration.

Recent advances of physiological imaging techniques have prompted us to use thermography for screening skin temperature, deep tissue edema or fluid collection due to inflammation (Nishide et al., 2009). Infrared thermography is one of the

leading technologies in use today. This technology is feasible for temperature monitoring of the foot and can be used as a complement to current practices for foot examinations in diabetes.

In this study, we used thermal plantar images in patients without diabetes to support a mathematical model for foot normal temperature distribution.

# 2 MATERIALS AND METHODS

#### 2.1 Subjects

This study includes healthy volunteers, recruited from Polytechnic Institute of Bragança, representing a feet healthy population who were between 21 to 43 years old. This preliminary study includes a set of fifteen thermographic images.

#### 2.2 Protocol

The subjects were guided to keep resting supine position without shoes or socks for 10 minutes, before measurement, to stabilize the feet temperature.

The images were collected by a thermal camera (FLIR 365) positioned at a fixed distance of 1 metre of subject's feet. A plate of rigid foam was placed over the ankles to isolate the temperature of feet from the rest of the body. The total duration of data acquisition process did not exceed 15 minutes.

#### 2.3 Image processing

Infrared thermography is a real-time temperature measurement technique used to produce a coloured visualization of thermal energy emitted by skin.

However, temperature discrimination threshold, on the foot, could be a difficult process due to the large temperature variation between the feet and the background.

As we can see from Figure 1, the large temperature variation in the image produces small colour variations of skin temperature.

Through the application of image processing techniques it is possible to obtain images with a better contrast of the structures in question. In order to isolate the feet from the background, we apply image segmentation, based on region growing, followed by a histogram expansion using only the temperature values of the feet, obtaining discriminative images, as showed in Figure 2.

### 2.4 Characterize foot regions

Interpretation of the colour patterns according to the anatomic temperature distribution is thought to aid in evaluating and diagnosing foot complications.



Figure 1. Thermal infrared image.



Figure 2. Improving the temperature discrimination.

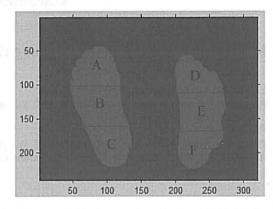


Figure 3. Foot regions.

With the numerical data, obtained through image processing, we defined main areas by measuring each foot (length and width) and divided it in three regions. Considering the left foot, Region A is the upper region; Region B is the central region and the lower region was defined as Region C.

In a similar way, Regions D, E and F were defined for the right foot, as represented in Figure 3.

# 3 NUMERICAL RESULTS AND DISCUSSION

In this study, we used fifteen feet images. Nine of them follow the same pattern for the maximum temperature while the other six do not have a defined pattern.

Figure 4 shows the maximum temperature value, for each region, from the set of nine images which follow a pattern.

We can observe that the maximum temperature value was obtained at Region A and D (the upper regions of the feet) which agrees with other results presented in the literature.

In this preliminary study, we tested three nonlinear mathematical models for the temperature distribution. The parameters i, j represent the pixels positions.

$$f_1(x,i,j) = x_1 i j + x_2 i^2 + x_3 j^2 + x_4 i + x_5 j + x_6$$
 (1)

$$f_2(x,i,j) = x_1 \sin(x_2 i + x_3) + x_4 \sin(x_5 j + x_6) + x_7$$
 (2)

$$f_3(x,i,j) = x_1 \sin^2(x_2 i + x_3) + x_4 \sin^2(x_5 j + x_6) + x_7$$
 (3)

It was observed that the best mathematical function that approximates the temperature distribution was the function  $f_2$ . The evaluation was done using the nonlinear least method combined with  $l_1$  penalty method.

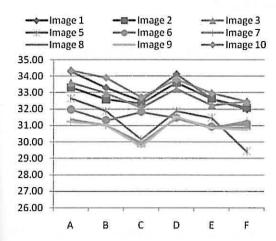


Figure 4. Absolute temperature maximum values.

#### 4 CONCLUSIONS AND FUTURE WORK

High temperature gradients between foot regions may predict the onset of neuropathic ulceration, which makes temperature monitoring a way to reduce the risk of ulceration.

In this study, we observed that the temperature maximum value, in general, is obtained in the upper regions of the foot.

A preliminary study indicates that the best mathematical model to approximate the temperature distribution is a sine sum function. Future prospective observation is needed to confirm our mathematical model or some variation of it.

#### REFERENCES

Armstrong, D., Holtz-Neiderer, K., Wendel, C. et al., 2007. Skin temperature monitoring reduces the risk for diabetic foot ulceration in high-risk patients, *The American Journal of Medicine* 120: 1042–1046

American Journal of Medicine 120: 1042–1046.

Lavery, L., Higgins, K., Lactot, D., Constantinitides, G., Zamorano, R., Armstrong, D., et al., 2004. Home monitoring of foot skin temperatures to prevent ulceration, Diabetes Care 27(11): 2642–2647.

Nagase, T., Sanada, H., Takehara, K., Oe, M., Iizaka, S., Ohashi, Y., Oba, M., Kadowaki, T. & Nakagami, G. 2011. Variations of plantar thermographic patterns in normal controls and non-ulcer diabetic patients: novel classification using angiosome concept, *Journal* of Plastic, Reconstructive & Aesthetic Surgery 64(7): 860–866.

Nishide, K., Nagase, T., Oba, M., Oe, M., Ohashi, Y., Iizaka, S., Nakagami, G., Kadowaki, T. & Sanada, H. 2009. Ultrasonographic and thermographic screening for latent imflammation in diabetic foot callus. *Diabetes Research and Clinical Practice* 85(3): 304–309.

Sun, P.C., Lin, H.D., Jao, SH., Ku, Y.C., Chan, R.C. & Cheng, C.K. 2006. Relationship of skin temperature to sympathetic dysfunction in diabetic at-risk feet. *Diabetes Research and Clinical Practice* 73(1): 41–46.