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1 **Effects of noise exposure on young adults with normal audiograms II: Behavioral measures**

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3

4 Garreth Prendergast<sup>a,\*</sup>, Rebecca E. Millman<sup>a,b</sup>, Hannah Guest<sup>a</sup>, Kevin J. Munro<sup>a,b</sup>, Karolina Kluk<sup>a,b</sup>,

5 Rebecca S. Dewey<sup>c,d,e</sup>, Deborah A. Hall<sup>d,e</sup>, Michael G. Heinz<sup>f</sup>, Christopher J. Plack<sup>a,b,g</sup>.

6

7 a, Manchester Centre for Audiology and Deafness, University of Manchester, Manchester Academic  
8 Health Science Centre, M13 9PL, UK.

9 b, NIHR Manchester Biomedical Research Centre, Central Manchester University Hospitals NHS  
10 Foundation Trust, Manchester Academic Health Science Centre, Manchester, M13 9WL, UK.

11 c, Sir Peter Mansfield Imaging Centre, School of Physics and Astronomy, University of Nottingham  
12 Nottingham, NG7 2RD, UK.

13 d, National Institute for Health Research (NIHR) Nottingham Biomedical Research Centre,  
14 Nottingham, NG1 5DU, UK.

15 e, Otology and Hearing Group, Division of Clinical Neuroscience, School of Medicine, University  
16 of Nottingham, Nottingham, NG7 2UH, UK.

17 f, Department of Speech, Language, & Hearing Sciences and Biomedical Engineering, Purdue  
18 University, West Lafayette, IN 47907, USA.

19 g, Department of Psychology, Lancaster University, Lancaster, LA1 4YF, UK.

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28 Abstract

29 An estimate of lifetime noise exposure was used as the primary predictor of performance on a range  
30 of behavioral tasks: frequency and intensity difference limens, amplitude modulation detection,  
31 interaural phase discrimination, the digit triplet speech test, the co-ordinate response speech  
32 measure, an auditory localization task, a musical consonance task and a subjective report of hearing  
33 ability. One hundred and thirty-eight participants (81 females) aged 18-36 years were tested, with a  
34 wide range of self-reported noise exposure. All had normal pure-tone audiograms up to 8 kHz. It  
35 was predicted that increased lifetime noise exposure, which we assume to be concordant with noise-  
36 induced cochlear synaptopathy, would elevate behavioral thresholds, in particular for stimuli with  
37 high levels in a high spectral region. However, the results showed little effect of noise exposure on  
38 performance. There were a number of weak relations with noise exposure across the test battery,  
39 although many of these were in the opposite direction to the predictions, and none were statistically  
40 significant after correction for multiple comparisons. There were also no strong correlations  
41 between electrophysiological measures of synaptopathy published previously and the behavioral  
42 measures reported here. Consistent with our previous electrophysiological results, the present  
43 results provide no evidence that noise exposure is related to significant perceptual deficits in young  
44 listeners with normal audiometric hearing. It is possible that the effects of noise-induced cochlear  
45 synaptopathy are only measurable in humans with extreme noise exposures, and that these effects  
46 always co-occur with a loss of audiometric sensitivity.

47

48 Keywords

49 Cochlear synaptopathy

50 Hidden hearing loss

51 Noise-induced hearing loss

52 Speech-in-noise

53 Psychophysics

54

55

56 1. Introduction

57 Cochlear synaptopathy due to noise exposure (often referred to as “hidden hearing loss”) was  
58 demonstrated in a mouse model by Kujawa and Liberman (2009). In the base of the cochlea, 50%  
59 of synapses were lost between inner hair cells (IHCs) and auditory nerve (AN) fibers after a 2-hour  
60 exposure to 100 dB SPL noise (8-16 kHz). Post-exposure, measures of absolute auditory sensitivity  
61 were unaffected but a permanent decrease in the amplitude of wave I of the auditory brainstem  
62 response (ABR), reflecting decreased auditory nerve activity, was seen in response to moderate- and  
63 high-intensity stimuli. The synaptic loss was subsequently found to preferentially affect the high-  
64 threshold, low spontaneous-rate (SR) AN fibers (Furman et al., 2013).

65

66 A loss of cochlear synapses due to noise exposure, in the presence of almost unaffected threshold  
67 sensitivity, has also been demonstrated in a range of other rodents (e.g. guinea pig, Lin et al., 2011;  
68 chinchilla, Hickox et al., 2015; 2017; rat, Möhrle et al., 2016). However, pure synaptopathy may be  
69 more difficult to produce in primates. In the macaque model, high noise exposures (108 dB SPL or  
70 greater) may be required for around 4 hours to produce supra-threshold reductions in the amplitude  
71 of wave I of the ABR (Valero et al., 2017). A number of review articles give a thorough account of  
72 the progression from the initial seminal work in the mouse, to the current understanding in the field  
73 (Kobel et al., 2017; Liberman and Kujawa, 2017; Plack et al., 2014; 2016). However, the initial  
74 account of cochlear synaptopathy as described in the mouse model may not be translated into an  
75 analogous human pathology in a straightforward way (Hickox et al., 2017).

76

77 The evidence for noise-induced cochlear synaptopathy in human listeners is somewhat sparse and

78 inconsistent. Stamper and Johnson (2015a) first provided evidence for reductions in ABR wave I  
79 amplitude with greater noise exposure in audiometrically normal human listeners. However,  
80 audiograms were only measured up to 8 kHz, and it is possible that high-frequency hair cell loss  
81 affected wave I amplitudes in the more exposed listeners (Don and Eggermont, 1978). Furthermore,  
82 there was a confound of sex in that the most noise exposed listeners in the cohort were male, and  
83 males also tend to show smaller ABR amplitudes due to factors such as skull thickness and head  
84 size (Picton et al., 1981; Jerger and Hall, 1980). In a subsequent letter, Stamper and Johnson  
85 (2015b) analyzed their data for the highest click level (90 dB nHL) for the two sexes independently.  
86 The relation between wave I amplitude and a 12-month noise exposure estimate persisted for  
87 females, but not males.

88

89 Recently, Bramhall et al. (2017) reported that non-veteran firearm users and veterans with high  
90 levels of noise exposure have reduced wave I amplitudes relative to lower noise exposed veterans  
91 and non-veterans without a history of firearm use. All groups had similar otoacoustic emissions and  
92 normal audiograms up to 8 kHz, although noise-exposed veterans showed an average elevation of  
93 audiometric threshold (averaged across 2000, 3000 and 4000 Hz) of 7.3 dB HL compared to non-  
94 veterans. High-frequency audiometric testing (> 8 kHz) was only performed on 59% of participants,  
95 and so the contribution of high-frequency hearing loss is uncertain.

96

97 In contrast to these findings of lower wave I amplitudes with greater noise exposure, we conducted  
98 a large-scale study (N=126) of young, normal-hearing adults and found no significant relation  
99 between lifetime noise exposure and ABR wave I amplitude for either males or females  
100 (Prendergast et al., 2017). These findings were replicated in a subsequent study from the same  
101 laboratory (Guest et al., 2017). Such negative findings are concordant with Liberman et al. (2016),  
102 who reported no significant difference in wave I amplitude between their high- and low-exposure

103 groups. However, they did find a difference in the ratio of the summing potential (SP) relative to  
104 the action potential (AP; effectively wave I). A larger SP/AP ratio was found for the high-noise  
105 group, due mainly to a higher SP for that group. Since the SP is thought to be generated by the hair  
106 cells (Kiang and Peake, 1960), a high SP/AP ratio is consistent with synaptopathy. However, it  
107 remains unclear how a loss of cochlear synapses would lead to enhancement of the SP, or how the  
108 SP would be affected by the substantial high-frequency audiometric deficit observed in the high-  
109 noise group.

110

111 Although the electrophysiological results in humans are mixed, with a number of studies showing  
112 discordant findings, it is possible that ABR measures are relatively insensitive to cochlear  
113 synaptopathy (Bourien et al. 2014; Prendergast et al., 2017) and that behavioral measures of  
114 auditory coding are more sensitive. Furthermore, important questions remain regarding the  
115 behavioral consequences of cochlear synaptopathy, and, more generally, regarding whether or not  
116 noise exposure is related to behavioral deficits in humans in the presence of normal audiometric  
117 thresholds.

118

119 There is existing evidence that noise exposure leads to impaired performance on a range of  
120 behavioral auditory tasks for listeners with normal audiograms, although some of these studies are  
121 confounded by age and audiometric differences between the groups. Alvord et al. (1983) measured  
122 identification scores for words in background noise presented at 60 dB HL. Noise-exposed listeners  
123 performed on average 10% more poorly than non-noise-exposed listeners but the groups were not  
124 sex-, age- or audiogram-matched. Kujala et al. (2004) used a task of deviant syllable detection and  
125 for age- and audiogram-matched groups, found a decrease in performance for noise-exposed  
126 listeners. Kumar et al. (2012) compared noise-exposed train drivers with age-matched controls and  
127 found that the noise-exposed group had deficits in amplitude modulation detection and speech  
128 recognition in background babble using stimuli presented at 80 dB SPL. However, it is not clear

129 from the paper if the groups were audiometrically matched and thus the observed differences may  
130 be explained by a more standard, and measurable, loss of audiometric sensitivity. Hope et al. (2013)  
131 compared noise-exposed Air Force pilots with non-exposed Air Force administrators and found a  
132 deficit in speech-in-noise (vowel-consonant-vowel stimuli) perception thresholds for the noise-  
133 exposed group. There was no difference between the groups on other auditory tasks including  
134 simultaneous masking, backward masking and frequency discrimination. Though the groups were  
135 audiometrically matched to within 2.2 dB, this only included frequencies up to and including 4000  
136 Hz.

137

138 Stone et al. (2008) used a task in which normal-hearing listeners were required to discriminate  
139 envelopes with different noise statistics at low sensation levels. Noise-exposed listeners showed a  
140 deficit in performance compared to non-noise-exposed controls, though these differences were  
141 observed at low sensation levels and therefore would not be dependent primarily on low-SR fibers.  
142 This evidence is therefore difficult to reconcile with the animal model of noise-induced  
143 synaptopathy. Liberman et al. (2016) demonstrated performance deficits on a speech-in-noise task  
144 for noise-exposed listeners relative to less exposed controls. However, stimuli were presented at 35  
145 dB HL, again suggesting minimal contributions of low-SR fibers to performance as at this sound  
146 intensity the high-SR fibers are unlikely to be saturated and thus efficient coding is not primarily  
147 dependent on low-SR fibers. Le Prell and Lobarinas (2016) examined measures of recreational  
148 noise exposure for groups of audiometrically normal young people, divided based on performance  
149 on a measure of word recognition in noise. The groups did not differ significantly in preferred  
150 listening level, nor in number of sources of high-level noise they were exposed to. Additionally, no  
151 reliable relation was observed between perceptual performance and the reported incidence of  
152 temporary threshold shift. Finally, Yeend et al. (2017) report results from a cohort of 30-60 year-old  
153 listeners. The primary aim was to characterize the perceptual deficits associated with increased  
154 noise exposure. The authors reported no link between lifetime noise exposure and performance on

155 any of the psychophysical or speech tasks. High-frequency hearing thresholds were predictive of  
156 speech-in-noise performance.

157

158 In this article we describe a series of behavioral measures that we collected concurrent with the  
159 electrophysiological data presented in Prendergast et al. (2017). We consider whether an estimate of  
160 lifetime noise exposure is able to predict performance on a range of behavioral tasks for young  
161 listeners with normal audiograms. By doing so we hoped to determine which, if any, behavioral  
162 tasks may be affected by synaptopathy, based on the assumption that greater lifetime noise exposure  
163 is a proxy for increased cochlear synaptopathy. As well as psychophysical tasks used to examine the  
164 coding fidelity of a listener's auditory system, we included tasks more representative of real-world  
165 listening ability, including speech-in-noise tasks, an auditory localization task, and a musical  
166 consonance task. Finally, we included the Speech, Spatial and Qualities of Hearing Scale (SSQ;  
167 Gatehouse and Noble, 2004) questionnaire to measure self-reported listening ability. Listeners with  
168 normal audiograms often report that they have listening difficulties (e.g. Davies, 1989), and it may  
169 be important to capture aspects of more general listening ability, beyond specific laboratory tasks.

170

171 The rationales for the tasks and stimuli chosen are based in part on what is known about noise-  
172 induced synaptopathy in the animal model. A compelling overview of how this may express itself in  
173 humans is provided by Bharadwaj et al. (2014), in which the authors predict that a loss of low-SR  
174 fibers will lead to a reduction in temporal coding, with poorer representations of acoustic signals in  
175 the auditory nerve. This would then lead to a reduction in the ability to discriminate subtle timing  
176 differences, for example in a frequency discrimination or inter-aural phase discrimination task.  
177 Bharadwaj et al. (2015) demonstrated that subcortical EEG measures, the ability of a listener to  
178 detect differences in the phase of a stimulus between ears, and amplitude modulation detection  
179 performance all co-vary seemingly due to individual differences in temporal coding. Although the  
180 study contained a crude measure of noise exposure history, which suggested that noise-exposed



181 participants have weaker evoked responses and elevated behavioral thresholds, the authors were  
182 cautious in concluding that noise-induced synaptopathy was the primary factor. In this study we  
183 included comparable tasks to ascertain if temporal coding varies as a function of lifetime noise  
184 exposure.

185

186 The effects of noise exposure were predicted to be most readily observed in response to high-level  
187 stimuli, as these would lead to saturation of high-SR fibers and therefore any differences in residual  
188 coding would be carried by the population of low-SR fibers. This approach is based on the low-SR  
189 hypothesis, supported by data from Furman et al. (2013), and assumes that this fiber group is  
190 critically important to the encoding of high-intensity sounds. Hence, for most tasks we used both  
191 low- and high-level conditions in order to provide a differential measure of the effects of  
192 synaptopathy. Note that this approach is insensitive to synaptopathy if medium- and high-SR fibers  
193 are able to encode high-level sounds by modulating their firing patterns (Young and Sachs, 1979).  
194 In addition, noise-induced audiometric hearing loss, caused mainly by damage to the outer hair cells  
195 (OHCs), typically manifests in the 3000-6000 Hz region (Toynbee, 1860; McBride and Williams,  
196 2001). Therefore, for a number of tasks, stimuli with frequency components in two spectral regions  
197 were used, with the assumption that synaptopathy is most likely to occur in the same frequency  
198 range as noise-induced outer hair cell dysfunction. Hence, for the psychophysical tasks, we  
199 measured performance at 255 Hz and 4000 Hz to provide another differential measure. Differential  
200 measures may help to control for the effects of variability between individuals due to factors  
201 unrelated to synaptopathy (Plack et al., 2016).

202

203 Finally, musical training is related to enhanced performance on some auditory tasks (Parbery-Clark  
204 et al., 2009; Zendel and Alain, 2009). Yeend et al. (2017) reported that sensitivity to temporal fine  
205 structure and amplitude modulation was enhanced in musically trained listeners. In order to control  
206 for the effects of musical experience in our cohort, we included an estimate of the number of years

207 during which a musical instrument was played regularly.

208

## 209 **2. Methods**

### 210 **2.1. Participants**

211 One hundred and thirty-eight participants (82 females), with a wide range of noise exposures, were  
212 tested, 123 of whom were also tested as part of an electrophysiological study of noise-induced  
213 synaptopathy (Prendergast et al., 2017). Participants were recruited mainly via a publicly available  
214 University of Manchester website listing active research projects. Advertisements were also placed  
215 in a number of bars and music venues in Manchester city center. All participants exhibited clinically  
216 normal audiometric thresholds (see section 2.3). Males had a mean age of 23.3 years (range, 18-36)  
217 and females had a mean age of 23.1 years (range, 18-36). The procedures were approved by the  
218 University of Manchester Research Ethics Committee and all participants gave informed consent  
219 (project number 14163).

220

### 221 **2.2. Noise exposure**

222 Lifetime noise exposure was estimated using a structured interview developed to assess the  
223 effectiveness of the UK noise at work regulations (Lutman et al., 2008). The specific  
224 implementation used is described fully by Prendergast et al. (2017). In summary, participants are  
225 asked to consider any high-noise (above ~ 85 dBA) environments/activities to which they have  
226 exposed themselves with a degree of repeatability over the course of their lifetime. The duration,  
227 frequency and level of exposure is estimated from discussion with the participant (including any  
228 attenuation from hearing protection used) and entered into the following formula:

229

$$230 \quad U = 10^{(L-A-90)/10} \times Y \times W \times D \times H / 2080,$$

231

232 where  $U$  is cumulative noise exposure,  $L$  is estimated noise exposure level in dBA,  $A$  is attenuation

233 provided by hearing protection in dB,  $Y$  is years of exposure,  $W$  is weeks of exposure per year,  $D$  is  
234 days of exposure per week,  $H$  is hours of exposure per day, and 2080 corresponds to the number of  
235 hours in a working year. One noise exposure unit is equivalent to exposure for 1 year to a working  
236 daily level of 90 dBA. For our purposes, we used the raw noise immission units and these were log  
237 transformed to produce a normal distribution. Each such logarithmic unit is a factor of 10 in terms  
238 of lifetime exposure energy.

239

240

### 241 **2.3. Pure tone audiometry**

242 Pure tone audiometry was performed for each ear separately at octave frequencies between 250 and  
243 8000 Hz in accordance with the British Society of Audiology (2011) recommended procedure.

244 Thresholds were measured using VIASYS GSI-Arrow audiometers coupled to TDH-39P supra-  
245 aural headphones, with MX41 cushions. The audiometric criterion for inclusion in the study was  
246 audiometric thresholds < 25 dB HL in both ears at all test frequencies.

247

248 High-frequency audiometry was also performed at 16 kHz using a Creative E-MU 0202 USB  
249 soundcard. Sounds were played over Sennheiser HDA 200 circum-aural headphones designed for  
250 high-frequency audiometry. The sound stimulus was a quarter-octave wide band of noise centered at  
251 16 kHz and converted from digital to analog at a sample rate of 48 kHz using a 24-bit depth. Stimuli  
252 were 220 ms in duration (including 10-ms raised-cosine ramps) ramps and there was an inter-  
253 stimulus interval of 500 ms. A three-alternative forced-choice procedure was used, with a two-  
254 down, one-up staircase adaptively setting the stimulus level. Stimulus level was varied  
255 arithmetically using a step size of 4 dB for the first four reversals and 2 dB for the following 10  
256 reversals. Thresholds were calculated by averaging the levels of the final 10 reversals from a single  
257 run.

258

259 Participants were asked if they suffered from tinnitus. If a positive response was given, participants  
260 were asked further questions to determine if this constituted prolonged tinnitus and when it was last  
261 perceived. If participants reported this percept regularly (at least every month), they were recorded  
262 as having tinnitus.

263

#### 264 **2.4. Behavioral tasks**

265 All sounds were presented using a Creative E-MU 0202 USB soundcard and Sennheiser HD650  
266 circum-aural headphones. All stimuli were presented diotically, except for the interaural phase  
267 difference (IPD) task and the localization task. Many of the behavioral tasks were performed in both  
268 a low- and high-frequency region (255 Hz and 4000 Hz respectively, denoted “L” and “H”) and also  
269 at a low and high sound intensity (40 and 80 dB SPL, denoted “40” and “80”). This was done to test  
270 the specific hypothesis that high-threshold, high-frequency fibers are preferentially affected by  
271 lifetime noise exposure. Unless specified, a two-down, one-up adaptive track was used, and the first  
272 four reversals were made using one step size and the final 10 using a smaller step size. Thresholds  
273 were calculated from the average of the tested parameter values at the final 10 reversals. Each of the  
274 four conditions was completed once in a random order in each block of trials. Three blocks were  
275 presented for each task. The mean threshold across the three blocks was taken as the final mean for  
276 each condition. Where geometric tracking was used, a geometric average of the means was  
277 calculated. 10-ms ramps were used to gate the onset and offset of all stimuli, unless otherwise  
278 specified, and these are included in all stimulus durations reported.

279

280 For three of the psychophysical discrimination tasks a two-alternative forced-choice paradigm was  
281 used in which the listener was asked to detect which of two observation intervals, each consisting of  
282 four stimuli (AAAA vs ABAB), contained non-identical stimuli (Hopkins and Moore, 2010). This  
283 paradigm has been shown to minimize practice effects (e.g. King et al., 2013). For these tasks, there

284 was a 50-ms silent period between stimuli within one of the two observation intervals, and a 500-ms  
285 silent period between observation intervals. Minimal training was given, with the experimenter  
286 confirming that the participant understood the task via a brief discussion after hearing the stimuli  
287 and by observing two correct responses on a brief practice run. The numbered intervals were  
288 visually cued with white lights on the screen for the duration of each stimulus and feedback was  
289 given in the form of a red or green light for incorrect and correct responses, respectively.  
290 Participants made their responses using numeric buttons on the keyboard. The participant could take  
291 a break between adaptive tracks and did not commence another test sequence until they indicated  
292 they were ready. Specific details for each of the tasks performed are given in the following sections.

293

#### 294 **2.4.1. Frequency difference limens (FDLs)**

295 The AAAA vs. ABAB paradigm was used. Tones were 200 ms in duration. Stimulus levels of 40  
296 and 80 dB SPL were used for each frequency. The low-frequency standard stimulus (A) was a 255-  
297 Hz pure tone. For the high-frequency condition, the stimulus was a transposed tone, consisting of a  
298 4000-Hz carrier modulated by a half-wave rectified, and low-pass filtered, pure tone (using a  
299 fourth-order Butterworth filter with a cutoff frequency of 2040 Hz). Transposed tones were used as  
300 they are designed to produce equivalent neural temporal firing patterns in high-frequency spectral  
301 regions of the cochlea as occur in low-frequency spectral regions in response to a pure tone  
302 (Bernstein and Trahiotis, 2002). For the standard stimulus (A) the frequency of the pure tone  
303 modulator was 255 Hz. Note that for the high-frequency condition, the task was modulation  
304 frequency discrimination. In both cases, the frequency of the pure tone for the comparison stimulus  
305 (B) was higher than that of the standard, and was varied adaptively. The starting difference in  
306 frequency was 10% and the frequency of the comparison stimulus was varied geometrically with an  
307 initial step size of a factor of 2 and a subsequent step size of  $\sqrt{2}$ . For the high-frequency conditions,  
308 low-pass pink noise was added in order to mask combination tones. The cut-off frequency of the  
309 noise band was 2500 Hz and the spectrum level at 1000 Hz was 40 dB below the signal level. Based

310 on estimates of distortion product level by Oxenham et al. (2009), the noise should have masked  
311 any combination tones below 2500 Hz.

312

#### 313 **2.4.2. Intensity difference limens (IDLs)**

314 The AAAA vs. ABAB paradigm was used. Tones were 200 ms in duration. Stimuli were pure tones  
315 presented at 255 or 4000 Hz, and at two levels (40 and 80 dB SPL for the standard, A, stimuli). The  
316 comparison stimulus (B) was higher in level than the standard. The starting Weber fraction was 10  
317 dB and was varied arithmetically with an initial step size of 4 dB and a second step size of 2 dB.

318

#### 319 **2.4.3. Interaural phase difference discrimination (IPD)**

320 The AAAA vs. ABAB paradigm was used. Tones were 300 ms in duration (including 50 ms ramps).  
321 The low-frequency stimulus was a 255-Hz pure tone, the starting phase of which was varied  
322 adaptively for the target tones. For the high-frequency condition, the stimulus was a transposed  
323 tone, consisting of a 4000-Hz tonal carrier modulated by a half-wave rectified, and low-pass  
324 filtered, 255-Hz pure tone. Stimulus levels of 40 and 80 dB SPL were used for each frequency. For  
325 the comparison stimulus (B) the phase of the pure tone or pure-tone modulator was varied  
326 adaptively. The starting difference was a positive shift of 30 degrees for stimulus B (stimulus A  
327 always had a starting phase of 0) and the phase was varied geometrically using an initial step size of  
328 a factor of 1.56 and a second step size of 1.25. The maximum difference between the phase of the  
329 reference and target was restricted to 90 degrees. If the maximum difference was reached, the  
330 difference remained fixed until two correct responses were given consecutively. For the high-  
331 frequency conditions, low-pass pink noise was added in order to mask combination tones. The cut-  
332 off frequency of the noise band was 2500 Hz and the spectrum level at 1000 Hz was 40 dB below  
333 the signal level.

334

335 **2.4.4. Amplitude modulation detection (AMD)**

336 A three-alternative forced-choice paradigm was used. Stimuli were 200 ms in duration. Carriers  
337 were 255-Hz and 4000-Hz pure tones for the low- and high-frequency stimuli respectively, and the  
338 target stimulus was a carrier sinusoidally amplitude modulated at 25 Hz. Carrier levels of 40 and 80  
339 dB SPL were used for each frequency. The RMS energy was equated across intervals. The starting  
340 modulation depth was 50% and this was then geometrically varied according to a two-down one-up  
341 track with an initial step size factor of 1.56 and a final step size factor of 1.25. There was a 500-ms  
342 inter-stimulus interval between each of the three tones.

343

344 **2.4.5. Digit triplet test (DTT)**

345 In the DTT, the participant is required to identify three spoken digits presented sequentially in a  
346 background noise (Smits et al., 2004). The digits were in the range 1-9 and the correct identification  
347 of all three was required for a correct response. The digits were voiced recordings from a single  
348 speaker taken from McShefferty et al. (2013). The noise was speech-shaped and fixed at each of  
349 two levels (40 and 80 dB SPL) while the sound level of the spoken digits was varied. A method of  
350 constant stimuli was used, with six repetitions at each of eight signal-to-noise ratios (SNRs). Each  
351 SNR / level combination was presented once, in a random order, in each block of trials. Three  
352 blocks were presented, and the overall percent correct responses calculated for each condition. The  
353 SNRs used were -24 to -3 in steps of 3 dB. The stimulus began with 200 ms of noise before the first  
354 digit was presented. There was a 50-ms interval between each of the spoken digits and the noise  
355 was continuous. Participants made their response by selecting three tick-boxes covering the range 1-  
356 9 using a computer mouse and then confirming their selection. Visual feedback was given in the  
357 form of a green (correct) or red (incorrect) light. For each individual, a cumulative Gaussian was  
358 fitted to the data to model the distribution and to allow the SNR to be estimated for a range of  
359 response rates. The results section uses 25%, 50% and 75% correct points to give an overview of

360 the psychometric function.

361

#### 362 **2.4.6. Co-ordinate response measure (CRM)**

363 In the CRM speech task (Bolia, 2000), the participant is presented with a number of speech  
364 utterances of the structure “*Ready <call sign> go to <color> <number> now*”, in which there are  
365 eight unique callsigns, four different colors (Blue, Red, White, Green) and the number is in the  
366 range 1-4. The participant’s callsign was always “Baron” and they were instructed to listen for the  
367 speaker who says “*Ready Baron*” and identify the color and number spoken by that speaker. The  
368 gender and identity of the target was changed on each trial and there were four male and four  
369 female speakers. Two maskers were presented simultaneously, which were always different  
370 speakers and different callsigns, although the color and number could match that of the target. All  
371 stimuli were spoken by native British-English speakers (Kitterick et al., 2010).

372

373 The CRM was performed at two sound levels (40 and 80 dB SPL) which defined the level of the  
374 combined masker stimuli, and in two different masker configurations; one where the maskers were  
375 presented centrally (CRM<sub>c</sub>) and one in which they were offset by 60 degrees azimuth on either side  
376 of the mid-line (CRM<sub>o</sub>). This was achieved by multiplying the acoustic stimuli by head-related  
377 impulse responses from the CIPIC database (Algazi et al., 2001). In each trial the target sentence  
378 was presented centrally at a sound level which varied trial-by-trial and the maskers were presented  
379 at a fixed sound level. A method of constant stimuli was used, with six repetitions at each of eight  
380 SNRs. Each offset / level / SNR combination was presented once, in a random order, in each block  
381 of trials. Three blocks were presented, and the overall percent correct responses calculated for each  
382 condition. The SNRs used were -6 dB to +8 dB in steps of 2 dB for the central condition and -14 dB  
383 to 0 dB in steps of 2 dB for the offset condition. Participants indicated their response by clicking on  
384 one of 16 buttons on the computer display, arranged in four color-coded columns with each row  
385 identified as a separate number. Visual feedback was given in the form of a green (correct) or red



386 (incorrect) light. For each individual, a cumulative Gaussian was fitted to the data to model the  
387 distribution and to allow the SNR to be interpolated for a range of response rates. The results  
388 section uses 25%, 50% and 75% correct points to give an overview of the psychometric function.

389

390

#### 391 **2.4.7. Localization task (LOC)**

392 The auditory localization task was performed for levels of 40 and 80 dB SPL. A single spoken word  
393 (“Tiger” taken from the CRM corpus) was heard in quiet presented over headphones after being  
394 multiplied by one of 17 head-related impulse responses (Algazi et al., 2001), intended to make the  
395 percept originate from one of the following virtual azimuths: +/- 80, 65, 55, 45, 35, 25, 15, 5 and 0  
396 degrees. Each speech token was presented with zero degrees elevation. Participants indicated their  
397 response by clicking one of 17 boxes on the computer display laid out schematically in a semi-  
398 circle, as if looking down on the participant perceiving the sound source. Each location was  
399 presented six times in a single run, and three runs were completed for each sound level. Both the  
400 order of the runs and of the stimuli within a run were randomized. No feedback was provided.

401

#### 402 **2.4.8. Musical consonance task (CON)**

403 There is evidence that ratings of the perceived pleasantness of chords are related to the strength of  
404 neural temporal coding (Bones et al., 2014), and temporal coding has been linked to synaptopathy  
405 (Bharadwaj et al., 2014). Hence a consonance preference task may be effective at identifying  
406 temporal coding deficits due to synaptopathy. The stimuli and methodology were based on Bones  
407 and Plack (2015). Two-note chords (dyads) were created by combining each of eight complex tones  
408 (fundamental frequencies, F0s, of 293.66, 311.12, 329.62, 349.22, 370, 392, 415.3, 440 Hz) with  
409 each of 11 higher-F0 tones. Each complex tone contained 20 equal-amplitude harmonics. Each dyad  
410 is named after the musical interval between the F0s of the high and low notes (ratios of 1.06, 1.12,  
411 1.19, 1.26, 1.33, 1.41, 1.50, 1.59, 1.68, 1.78, 1.89). Dyads were 2 s in duration, including 10 ms

412 raised-cosine onset and offset ramps. Each dyad was preceded by Gaussian noise with the same  
413 duration and filtering (low-pass filtered at 6000 Hz). A 500-ms silence separated the noise and the  
414 dyad. The purpose of the noise was to prevent trials being influenced by the preceding stimulus and  
415 thus biasing the pleasantness judgement of the current trial (McDermott et al., 2010). Listeners were  
416 asked to rate how pleasant or unpleasant they found the chord using a seven-point Likert scale (-3 to  
417 +3). The harmonics of each note had the same amplitude, and the overall level of each dyad was 80  
418 dB SPL.

419

#### 420 **2.4.9. Self-report assessment of hearing ability**

421 The SSQ was used to allow listeners to report their hearing ability in several domains, which are  
422 split into three scales; speech, spatial and qualities of hearing. The questionnaire consists of 49  
423 questions which describe a listening situation and ask people to rate their listening ability in that  
424 situation from 0-10, with a higher number indicating better performance and an improved sense of  
425 hearing ability. The SSQ is designed to provide a comprehensive assessment of an individual's  
426 perceived ability to hear in the real world. The Speech scale (consisting of 14 items) covers an  
427 extensive range of realistic speech contexts that vary in their assumed difficulty. The items cover  
428 conditions of competing sound, the number of speakers, and selective attention (attending to one  
429 speech stream in a background of many), in an attempt to identify specific listening environments in  
430 which the ability to hear speech may be affected. The Spatial hearing scale (consisting of 17 items)  
431 addresses direction, distance, and movement discrimination abilities. The Qualities scale (consisting  
432 of 18 items) addresses issues related to the ability to segregate sounds, the clarity of sounds, and the  
433 demand of listening effort. For each individual, the mean score across all of the items on a scale was  
434 taken, which allows all three scales to be plotted on the same axis. This average score for each scale  
435 is used as a summary metric for each listener and can be compared to that listeners' noise exposure  
436 score to ascertain if there is a relation between the two. A negative relation is predicted, with  
437 increasing noise exposure expected to be associated with a decreasing score, which would indicate a

438 decrease in the listener's perceived hearing ability.

439

#### 440 **2.4.10 Musical experience**

441 To estimate the degree of musical experience, we asked those participants who reported having  
442 learnt an instrument: "Between what ages did you regularly play?" The total number of years of  
443 playing a musical instrument was taken as the metric of musical experience. A subset of participants  
444 worked in the music industry as sound engineers/technicians and these participants scored highly on  
445 this metric.

446

### 447 **3. Results**

448

449 Many of the behavioral thresholds were found to be non-normally distributed and so in these cases  
450 Spearman's rho was used in order to evaluate the extent to which lifetime noise exposure predicted  
451 performance. Due to attrition, the number of participants varies slightly for each task and so the  
452 number of participants included is noted for each task. Note that the primary focus here is on the  
453 relation of behavioral performance to noise exposure, not on the relations between behavioral  
454 measures. Due to the exploratory nature of this study, a large number of comparisons are performed.  
455 This approach comes with a multiple comparisons penalty, to the extent that potentially genuine,  
456 albeit weak, relations may be discarded. Therefore, no correction for multiple comparisons has been  
457 performed and discussion of the results considers any relation which reaches an alpha of 0.05, albeit  
458 with appropriate caveats.

459

#### 460 **3.1. Noise exposures**

461 Estimated lifetime noise exposure scores varied with respect to  $\log(\text{energy})$  from 0 (a listener with  
462 effectively no exposure to sounds with levels estimated to be above 85 dBA) to 2.54. In terms of  
463 energy, there was a difference of a factor of 300 between the lowest and the highest noise exposed

464 participants. There was no significant difference between noise exposure scores for males  
465 (mean=1.37, s.d.=0.54) and females (mean=1.22, s.d.=0.51):  $t(136)=1.63$ ,  $p=0.10$ . Therefore, the  
466 remaining results for male and female listeners were pooled. Noise exposure is used as the primary  
467 predictor variable in the analyses. Fig. 1 shows the distribution of noise exposures for the cohort as  
468 a function of age.

469

470 In addition to considering the entire cohort in correlational analyses, it is instructive to examine  
471 groups with extreme low and high noise exposure. This division into sub-groups may increase the  
472 likelihood of observing the effects of synaptopathy, and provides a concise and clear visual  
473 indication of the sensitivity of each measure to noise exposure. Hence, in the figures that follow,  
474 we present data for the 25% of the cohort (34 individuals in each group) with the lowest (green  
475 open squares) and highest (black filled squares) noise exposure scores. These groups had mean  
476 exposures (expressed on a logarithmic scale) of 0.63 (range; 0-0.95) and 1.95 (range; 1.60-2.54),  
477 respectively. Across the different tasks, the number of individuals included sometimes changed  
478 slightly due to attrition, though the mean exposures were always close to those presented here.

479

### 480 **3.2. Audiometric data and tinnitus**

481 Fig. 2 shows audiometric data (averaged across the ears) for all listeners, and for the low- and high-  
482 exposure groups. There was very little effect of noise exposure on audiometric threshold for  
483 frequencies up to 8 kHz, although there was a substantial difference between groups at 16 kHz, with  
484 the high-exposure group having poorer hearing thresholds on average. The Pearson correlation  
485 between 16-kHz audiometric thresholds and lifetime noise exposure was statistically significant  
486 ( $r=0.29$ ;  $p<0.001$ ), as also reported by Prendergast et al. (2017) using a near-identical dataset.  
487 Pearson correlation coefficients revealed no significant relation between audiometric threshold and  
488 noise exposure at 2000 Hz ( $r=0.09$ ;  $p=0.27$ ), 4000 Hz ( $r=0.10$ ;  $p=0.24$ ), and 8000 Hz ( $r=0.02$ ;  
489  $p=0.82$ ). Musical experience showed no statistically significant relation with any of the audiometric

490 thresholds tested.

491

492 Ten participants reported experiencing prolonged tinnitus. Three of these participants were in the  
493 lowest 25% of noise exposures and five in the highest 25%.

494

### 495 **3.3. Psychophysics (FDL, IDL, IPD, AMD)**

496

497 Fig. 3 shows the results for the four psychophysical experiments: FDL, IDL, IPD and AMD. In each  
498 panel, results for all four conditions are shown for each of the two levels and frequencies (L40, L80,  
499 H40, and H80, where “L” and “H” refer to low and high frequency, and the number refers to the  
500 level in dB SPL). There were no marked differences between the two groups, and small confidence  
501 intervals, which suggest that any effects of exposure were small.

502

503 Table 1 shows Spearman correlations for the whole group (with the N for each task indicated)  
504 between the noise exposure scores and the thresholds for each of the conditions. Table 1 also shows  
505 the correlation of noise exposure with two differential measures; one which contrasts different  
506 sound levels in the same spectral region (4000 Hz) and one which contrasts different spectral  
507 regions at the same sound level (80 dB SPL). It was predicted that cochlear synaptopathy would be  
508 associated with a positive correlation (increasing threshold with increasing noise exposure) in each  
509 case, based on the assumption that a positive correlation in the differential measure is caused by an  
510 elevation of threshold for high-noise exposed listeners in the H80 condition and equivalence of  
511 thresholds across exposure for the lower frequency/level condition. This assumption is premised on  
512 the low-SR fibers being primarily affected by noise exposure. There were only weak correlations,  
513 and these must be considered with caution as no correction for multiple comparisons was applied,  
514 and none of the significant correlations would survive Bonferroni correction.

515

516 The strongest relations across all tasks were in the opposite direction to those predicted. For the  
517 FDL task, increasing noise exposure was related to an improvement in performance. This appears to  
518 be driven by high-noise participants outperforming low-noise participants in the high-frequency,  
519 high-level (H80), condition but performing more poorly in the high-frequency, low-level (H40)  
520 condition. For the IPD task there was a weak relation with noise exposure in the predicted direction  
521 with the differential measure, computed using H80-L80. This relation was partly driven by higher  
522 thresholds for the more exposed listeners in the H80 condition, as predicted, but it was driven more  
523 strongly by the noise-exposed listeners outperforming the less exposed in the L80 condition. There  
524 was also a weak effect for the IDL task, again for the differential measure computed using the two  
525 high-level conditions. This negative relation with noise exposure was driven by the fact that high-  
526 and low-noise exposed participants performed comparably in the H80 condition, but there was a  
527 decrease in performance with increasing noise exposure for the L80 condition.

528

529 The strongest relation of interest in the tasks presented is that between lifetime noise exposure and  
530 AMD, though it was in the opposite direction to that predicted. There was a negative relation  
531 between lifetime noise exposure and AMD threshold in the H80 condition; i.e. performance  
532 improved as noise exposure increased. The use of the differential frequency measure strengthened  
533 the relation, as in the L80 condition there was a slight decrease in performance with increasing  
534 noise exposure. The relations need to be validated in different cohorts to establish if they are in fact  
535 genuine, weak effects related to lifetime noise exposure.

536

537 Audiometric thresholds at 4000 Hz were found to correlate significantly with performance on the  
538 AMD high-frequency conditions, with high thresholds associated with better performance (H40,  $\rho$   
539 = -0.25; H80,  $\rho$  = -0.31; H80-H40,  $\rho$  = -0.37; all  $p < 0.01$ ). However, the correlations with noise  
540 exposure for these conditions showed a similar strength to the original correlations once

541 audiometric sensitivity was controlled for (H40,  $\rho = -0.25$ ; H80,  $\rho = -0.31$ ; H80-H40,  $\rho =$   
542  $-0.37$ ; all  $p < 0.01$ ). No other behavioral measure (including those reported in sections 3.4., 3.5. and  
543 3.6) varied significantly as a function of 4000 Hz audiometric threshold.

544

#### 545 **3.4. Speech measures (DTT, CRM)**

546 Fig. 4 shows a summary of performance for each of the three speech tasks used; the DTT, the co-  
547 ordinate response measure with central maskers (CRM<sub>c</sub>), and the co-ordinate response measure  
548 with maskers spatially offset (CRM<sub>o</sub>). The SNRs at which 25%, 50% and 75% correct performance  
549 was estimated to occur are plotted for the low- and high-noise exposed groups. In each case, the  
550 differences between the groups are small.

551

552 Table 2 summarizes the relations between noise exposure and performance across the full group of  
553 participants (with N specified for each task). The relations were weak: None of the significant  
554 effects would survive correction for multiple comparisons and therefore must be interpreted with  
555 caution. The DTT showed a relation between performance and lifetime noise exposure for the  
556 differential measures taken at 25% and 50% correct on the psychometric function in the opposite  
557 direction to that predicted, i.e. with improving performance (a decrease in SNR) as a function of  
558 lifetime noise exposure. The effect was strongest at 25% correct, which was driven by highly noise-  
559 exposed listeners performing more poorly than lower noise-exposed listeners at 40 dB SPL and  
560 outperforming them at 80 dB SPL (a moderate but insignificant relation). A similar pattern was seen  
561 for 50% correct on the psychometric function, although it was weaker and only reached significance  
562 for the differential measure.

563

564 The CRM<sub>c</sub> task, in which the maskers were presented from the same spatial location as the target,  
565 revealed some weak trends. All three points on the psychometric function showed a qualitatively

566 similar trend, with high noise-exposed listeners outperforming the less noise exposed in the 40 dB  
567 SPL condition and the groups being largely comparable for the 80 dB SPL condition.  
568 There were no significant relations between noise exposure and performance on the CRMo task, in  
569 which the maskers were spatially offset. The 25% and 50% values for the CRMo task were  
570 extrapolated downwards from the range of SNRs tested (0 to -14 dB) and this extrapolation likely  
571 contributed in part to the increased confidence intervals for these values.

572

### 573 **3.5. Localization task (LOC)**

574 Fig. 5 shows the average localization error in both conditions for the 25% of listeners with the  
575 lowest and highest levels of noise exposure (total N = 126; 31 participants in each of the two  
576 exposure groups). The results were averaged across the midline, such that each point is the average  
577 absolute error for both positive and negative azimuths. A summary error score was calculated for  
578 each participant by summing the mean absolute errors for each of the azimuths in order to correlate  
579 performance with noise exposure. Spearman's rho indicated no significant relation between noise  
580 exposure and localization error for either the 40 dB SPL ( $\rho=0.11$ ,  $p>0.05$ ) or 80 dB SPL  
581 ( $\rho=0.04$ ,  $p>0.05$ ) condition, nor was there a relation for the differential measure: the ratio between  
582 average errors at 80 and 40 dB SPL ( $\rho=-0.02$ ,  $p>0.05$ ).

583

### 584 **3.6. Musical consonance (CON)**

585 Fig. 6 shows the average rating for each of the 11 two-note chords for the 25% of highest and  
586 lowest noise-exposed participants (total N=125, 31 participants in each of the exposure groups).  
587 Using a technique described by Bones and Plack (2015), a consonance preference score was  
588 calculated by taking the average z-score for the five most consonant chords and subtracting the  
589 average z-score for the five most dissonant chords for each participant. Spearman's rho indicated  
590 that this consonance preference score did not vary significantly with noise exposure ( $\rho=0.11$ ,  $p$



591 >0.05). The predicted direction was a reduction in consonance preference as a function of  
592 increasing lifetime noise exposure, due to a loss of temporal coding precision, which would mimic  
593 that observed in older listeners (Bones and Plack, 2015).

594

### 595 **3.7. Speech, Spatial, and Qualities of Hearing Scale (SSQ)**

596 Fig. 7 shows the average subjective rating on the three scales of the SSQ for the 25% of lowest and  
597 highest noise-exposed participants (total N=135). A high SSQ score indicates good self-perceived  
598 hearing abilities. Contrary to the prediction, self-report hearing ability increased slightly with  
599 lifetime noise exposure for the Spatial (Spearman's  $\rho=0.17$ ;  $p<0.05$ ) and Qualities scales  
600 ( $\rho=0.23$ ;  $p<0.01$ ). No such relation was observed for the Speech scale of the questionnaire. The  
601 relation between lifetime noise exposure and SSQ score was statistically significant for two of the  
602 three scales. However, this was achieved by virtue of a large sample size and low variability across  
603 ratings. The mean difference between the groups was  $<1$ , which is the unit of granularity in the  
604 measure. Therefore, although these relations may indicate an underlying difference in perceived  
605 hearing ability that is of interest and potentially important to characterize, these differences are not  
606 of clinical relevance.

607

### 608 **3.8. Relation of behavioral measures to musical experience**

609 Musical experience correlated positively with noise exposure ( $\rho=0.38$ ;  $p<0.001$ ). Hence musical  
610 experience could have been a confound, with the deleterious effects of noise exposure compensated  
611 by the performance benefits associated with musical experience (Parbery-Clark et al., 2009; Zendel  
612 and Alain, 2009; Yeend et al, 2017). Table 1 reports two further correlational analyses for the  
613 psychophysical measures: one in which partial correlations were performed between performance  
614 and lifetime noise exposure, with musical experience controlled. The second analysis is for the  
615 correlation of performance and musical experience.

616

617 Of the six correlations with noise exposure, all but one remained of a similar strength after  
618 controlling for musical experience. The relation between AMD H80 and noise exposure was  
619 markedly reduced, but four of the remaining five AMD conditions remained significant at the 0.05  
620 level. The correlations indicate that AMD and FDL performance improved significantly with  
621 increased musical training. However, none of the differential measures were significantly correlated  
622 with musical experience.

623  
624 A similar pattern was seen for the speech tasks (Table 2), with the differential measures for the DTT  
625 and CRMc tasks having the strongest correlations with noise exposure once musical experience was  
626 controlled. The correlation with musical experience reached significance for the 40 dB SPL  
627 condition of the CRMc task (at 25% and 50% correct) but the differential measures did not. The  
628 differential measure for 50% correct on the DTT showed a significant correlation with musical  
629 experience.

630  
631 Scores for the localization and musical consonance tasks showed no significant correlations either  
632 with musical experience controlled, or with musical experience on its own. For the SSQ, scores for  
633 the three scales were not significantly correlated with musical experience. However, the partial  
634 correlations between noise exposure and SSQ score, controlling for musical experience, were 0.12,  
635 0.19 (both  $p < 0.05$ ) and 0.23 ( $p < 0.01$ ) for the Speech, Spatial and Qualities components,  
636 respectively. This suggests that the relation initially shown between subjective report of hearing  
637 ability and noise exposure is not related to the degree of musical experience reported by the listener.

638

### 639 **3.9. Relation of behavioral measures to electrophysiological measures of synaptopathy**

640 One core assumption of this study was that increased lifetime noise exposure is a proxy for  
641 increased levels of synaptopathy. Prendergast et al. (2017) used a largely identical dataset and found  
642 no relation between lifetime noise exposure and objective physiological measures of synaptopathy.

643 One reason for this, which was discussed in that paper, is that supra-threshold ABR measures may  
644 not be sensitive enough to detect subtle changes in auditory processing. However, it could be argued  
645 that better estimates of synaptopathy can be obtained by using the electrophysiological measures,  
646 with the assumption that a weaker evoked response is indicative of greater underlying synaptopathy.  
647 To address this issue, we looked at how our battery of measures related to two core differential  
648 measures of synaptopathy, the wave I/V amplitude ratio and the FFR responses reported in  
649 Prendergast et al. (2017). The FFR (expressed in dB SNR) generated in response to a 255-Hz pure  
650 tone was used to assess the relation with low-frequency psychophysical conditions. The envelope  
651 FFR (expressed in dB SNR), generated in response to the modulated waveform (255 Hz  
652 modulation) of a 4000 Hz carrier was used to assess the relation with the high-frequency  
653 psychophysical conditions. The differential FFR measure was obtained by subtracting the SNR for  
654 the low-frequency FFR from the SNR for the envelope FFR, and this was used to assess any  
655 relation with differential behavioral measures. The differential FFR was also used to investigate  
656 whether there was any association with performance on the speech, musical consonance,  
657 localization, and SSQ measures.

658  
659 The wave I/V ratio at 100 dB peSPL showed no significant relation with scores for any of the  
660 psychophysical, speech, musical consonance, or localization tasks, or the SSQ measures ( $p > 0.05$  for  
661 all tests). The correlations of the FFR measures with behavioral performance are reported in Table  
662 3. There were no significant relations between the differential FFR measure and the speech, musical  
663 consonance or localization tasks, nor the SSQ measure. The correlations with the psychophysical  
664 thresholds were generally weak. For all four psychophysical tasks, performance on the L40  
665 condition showed a negative correlation with the FFR SNR in response to a 255-Hz pure tone. This  
666 association was strongest, and reached significance, for the AMD task. This AMD condition  
667 previously showed no relation with noise exposure and the effects of cochlear synaptopathy were

668 expected to be observed in the high-frequency envelope FFR, rather than the low-frequency FFR.  
669 None of the differential behavioral measures showed a significant relation with the differential FFR  
670 measure.

671

### 672 **3.10. Relation of behavioral measures to 16-kHz audiometric thresholds**

673 Liberman et al. (2016) suggested that high-frequency audiometry may be a marker for cochlear  
674 synaptopathy at lower frequencies. To test this prediction, Spearman's rho correlations were  
675 computed between 16-kHz audiometric thresholds and scores for each of the behavioral tasks.

676

677 For the psychophysical tasks all the individual and differential measures were used. The 80 dB SPL  
678 condition was used for the speech, localization, and musical consonance tasks. The only task whose  
679 scores showed a significant relation with 16 kHz thresholds was AMD. In the H80 condition,  
680 performance improved with increasing 16-kHz thresholds ( $\rho = -0.25$ ;  $p < 0.01$ ), although this  
681 relation was markedly reduced when a partial correlation was performed which controlled for the  
682 audiometric pure tone average at 2000, 4000 and 8000 Hz ( $\rho = -0.15$ ;  $p > 0.05$ ). For the H80 – L80  
683 differential measure, the relation was similar, performance improving with reduced 16-kHz  
684 audiometric sensitivity ( $\rho = -0.26$ ;  $p < 0.01$ ) and for this condition the relation persisted after  
685 controlling for low-frequency audiometric thresholds ( $\rho = -0.18$ ;  $p < 0.05$ ). These relations were in  
686 the opposite direction to that predicted on the basis of synaptopathy, as the expected effect of  
687 greater noise exposure (and therefore potentially greater synaptopathy) would be to reduce the  
688 fidelity of temporal coding and elevate behavioral thresholds. However, it is known that  
689 sensorineural hearing loss is often associated with improved AMD thresholds (e.g. Füllgrabe et al.,  
690 2003). From this perspective, relating to OHC dysfunction in participants with a high-frequency  
691 audiometric loss, the correlations were in the predicted direction. The H80 – H40 differential  
692 measure showed a comparable trend, with performance improving with increasing 16-kHz threshold

693 ( $\rho = -0.27$ ;  $p < 0.01$ ) and this trend persisted after correcting for low-frequency audiometric  
694 thresholds ( $\rho = -0.23$ ;  $p < 0.01$ ). The H80, and both differential conditions, were the only conditions  
695 in which performance on the AMD task varied with high-frequency thresholds. The speech,  
696 localization, and musical consonance tasks, in addition to IPD, FDL, IDL, and SSQ, did not show  
697 any significant relation with 16-kHz thresholds ( $p > 0.05$ ). The pure tone average of the 2000, 4000  
698 and 8000 Hz audiometric thresholds was positively related to audiometric sensitivity at 16 kHz  
699 ( $r = 0.31$ ;  $p < 0.01$ ).

700

#### 701 **4. Discussion**

702 The main aim of this study was to establish whether performance on a range of behavioral tasks  
703 varies as a function of lifetime noise exposure for young listeners with normal audiograms. Overall,  
704 there was no strong evidence that performance is affected by noise exposure. There were some  
705 weak trends which may be of interest for further study, but these did not survive correction for  
706 multiple comparisons. This study provides further evidence that any effects of cochlear  
707 synaptopathy are difficult to observe in young human listeners with normal audiograms.

708

#### 709 **4.1. Psychophysical results**

710

711 The IDL, FDL and AMD thresholds are consistent with those in the literature for normal-hearing  
712 listeners (e.g. Viemeister and Bacon, 1988; He et al., 1979; Füllgrabe et al., 2003; Moore and Ernst,  
713 2012). Whilst the IPD thresholds for the transposed stimuli are larger than those reported by  
714 Bernstein and Trahiotis (2002), they are comparable with IPD thresholds reported by Bharadwaj et  
715 al. (2015).

716

717 The basic psychophysical results indicate some weak relations of potential interest, although these  
718 are difficult to explain, as performance improved as a function of noise exposure for some

719 conditions and declined for others. These contradictions were found both across conditions of the  
720 same task and across the different tasks. The strongest effects occurred for the differential measures,  
721 which attempt to account for some of the inherent variability across different listeners. Therefore,  
722 future investigations of sub-clinical hearing deficits, which are not readily identified from  
723 audiometric testing, may benefit from differential measures in order to reduce the impact of  
724 individual differences on performance (Plack et al., 2016). It must be noted however, that the  
725 differential measure based on level assumes that synaptopathy affects one condition (H80, in the  
726 context of the current study) and does not affect the lower-level condition (H40), which can then act  
727 as a within-subject control. Such an assumption is based on the evidence that low-SR fibers are  
728 primarily affected by noise exposure (Furman et al., 2013). If a specific fiber group is not targeted  
729 in this way in humans, then the results obtained with a differential measure based on level become  
730 more difficult to interpret.

731

732 The condition with the strongest relation with noise exposure was AMD for the high carrier  
733 frequency and high carrier level. However, this relation was counter to the predicted direction, as  
734 performance improved with increasing noise exposure. Similar effects have been reported in the  
735 literature when quantifying the modulation detection sensitivity of hearing-impaired listeners with a  
736 sensorineural hearing loss. Moore et al. (1996) reported that listeners with unilateral sensorineural  
737 hearing loss perceived enhanced envelope fluctuations in the impaired ear relative to the near-  
738 normal ear, possibly due to the loss of cochlear compression associated with OHC dysfunction.  
739 Also, Kale and Heinz (2010) reported enhanced envelope coding in auditory-nerve-fiber responses  
740 from noise-exposed chinchillas with permanent sensorineural hearing loss. Therefore, the relation  
741 between AMD performance and noise exposure may actually be driven by subtle differences in  
742 OHC function, an interpretation supported by the fact that 16-kHz thresholds were also related to  
743 AMD performance. Elevated thresholds at 16 kHz may be an early marker for sub-clinical OHC

744 dysfunction in the standard audiometric range which is not detectable using pure-tone audiometry,  
745 although there was no effect of exposure on transient-evoked otoacoustic emission amplitudes,  
746 measured up to 4000 Hz, in the present cohort (Prendergast et al., 2017). Such an explanation would  
747 highlight the need to reconsider how we define “normal” hearing for the purposes of research  
748 studies and may have interesting implications for future investigations of sub-clinical processing  
749 deficits, but would contribute little to our understanding of noise-induced cochlear synaptopathy.

750

#### 751 **4.2. Speech measures and self-report**

752 The DTT and the CRMc results both revealed weak relations with noise exposure that were again  
753 non-significant after correction. However, for the CRMc task, the relation with noise exposure was  
754 primarily observed for the 40 dB SPL condition, showing an improvement in performance with  
755 increasing noise exposure. This is opposite to the effect reported by Liberman et al. (2016) for their  
756 low-level speech task. The DTT showed different effects across the two sound levels, with  
757 increasing noise exposure relating to decreasing performance at 40 dB SPL and increasing  
758 performance at 80 dB SPL. The effects for the DTT occurred at 25% and 50% correct on the  
759 psychometric function. It is possible that the effects of synaptopathy are more apparent in difficult  
760 listening conditions, which would be concordant with Liberman et al. (2016), who used both time  
761 compression and reverberation to increase the difficulty of the task and exacerbate the differences  
762 between low and high noise exposed individuals. This notion is also supported by recent behavioral  
763 data collected in rats. Lobarinas et al. (2017) found a reduction in the ability to detect a narrowband  
764 of noise presented in an ongoing background noise after exposure to intense (109 dB SPL) noise.  
765 This was associated with a supra-threshold decrease in wave I amplitude, consistent with a loss of  
766 cochlear synapses. However, the behavioral reduction in sensitivity was only observed for the most  
767 challenging condition tested (20 dB SNR).

768

#### 769 **4.3. Effects of musical experience**

770 FDL and AMD thresholds were found to vary strongly with musical experience. However, this was  
771 only seen when looking at individual conditions, and none of the differential measures showed such  
772 a relation. The partial correlations, which controlled for musical experience, resulted in a weaker  
773 relation between noise exposure and performance for a number of the individual psychophysical  
774 tasks. However, the differential measures resulted in more robust correlations, as the partial  
775 correlations controlling for musical experience were comparable in magnitude to the initial  
776 correlation with noise exposure.

777

778 Performance on the speech tasks was not clearly related to musical experience, with only the 40 dB  
779 SPL CRM task with central maskers showing a clear relation between years of musical training and  
780 performance. In a pattern similar to that seen for the psychophysical tasks, when controlling for  
781 musical experience in a partial correlation, the coefficients decreased in magnitude but the  
782 differential measures remained largely unaltered, and still showed a weak, but significant  
783 correlation. For the SSQ estimate of hearing ability, the correlations with noise exposure were  
784 unchanged or increased after musical experience was controlled.

785

786 To summarize, the data presented here are consistent with recent work by Yeend et al. (2017) in that  
787 a participant's degree of musical training is predictive of their performance on a number of  
788 psychophysical and speech-in-noise tasks. This adds further complexity to a series of parameters  
789 which are already difficult to delineate; those with high-degrees of noise exposure tend to be older,  
790 possibly have poorer high-frequency hearing, and are also more likely to have musical training  
791 which leads to enhanced performance on a number of auditory tasks. The data presented in the  
792 current manuscript highlight the value of using a differential measure of performance, as it is these  
793 measures which are largely unchanged after controlling for musical experience. Using a differential  
794 estimate of performance in an individual may control for musical experience and allow a more  
795 direct measure of the effects of noise exposure.



#### 797 **4.4 Relation of behavioral measures to electrophysiological measures**

798 Prendergast et al. (2017) reported, in a dataset largely overlapping with the current cohort, no clear  
799 changes in ABR or FFR as a function of lifetime noise exposure. The estimate of lifetime noise  
800 exposure is sub-optimal, but does appear to accurately differentiate those with high levels of noise  
801 exposure from those with much lower exposure. We approached the current study with the  
802 hypothesis that noise-induced synaptopathy may be too subtle to detect using auditory evoked  
803 potentials, and that behavioral changes may be more readily observed. Therefore, we maintained the  
804 assumption that greater lifetime noise exposure is a legitimate proxy for an underlying loss of  
805 cochlear synapses. A counter-argument would be that electrophysiological measures of auditory  
806 function are a better proxy for underlying cochlear synaptopathy. Such an approach would posit that  
807 those with weaker ABRs and FFRs have sustained a loss of cochlear synapses which accounts for  
808 this altered response and thus they should also exhibit poorer behavioral performance. However, the  
809 wave I/V ratio was found not to be predictive of performance on any of the tasks used in this study.  
810 The strength of these correlations was generally weaker than those for performance versus noise  
811 exposure. The FFR was found to be weakly predictive of performance when single conditions were  
812 considered separately and this was for the low-frequency FFR and not the envelope FFR for the  
813 high frequency region. The differential FFR was not predictive for the differential behavioral  
814 conditions. Hence, using the electrophysiological metrics as a marker for synaptopathy did not  
815 provide any further insight into the relation of synaptopathy to behavioral measures.

816

817 It has been reported previously that the strength of auditory evoked potentials in an individual is  
818 predictive of performance on psychophysical tasks for normal-hearing listeners (e.g., Bones et al.,  
819 2014; Bharadwaj et al., 2015). Such a relation, with stronger evoked responses being concordant  
820 with better behavioral performance, is consistent with temporal coding precision being crucial for  
821 accurate auditory perception. However, these results were not replicated in the present study.

822 Furthermore, if such measures are to be used to better understand noise-induced cochlear  
823 synaptopathy, they must in some way be linked to the noise exposure history of the individual. The  
824 present approach assumes a simple relation between noise exposure and behavioral thresholds. The  
825 interpretation is complicated if different listeners have different degrees of susceptibility to  
826 suffering physiological damage from acoustic trauma. It may also be the case that an acoustic event  
827 is more damaging depending on when in the lifetime it occurs. It is currently unknown whether  
828 such factors affect the manifestation of cochlear synaptopathy in humans.

829

#### 830 **4.5. Can noise-induced synaptopathy in humans with normal audiograms be disregarded?**

831 The lack of an effect of noise exposure on behavioral performance is consistent with Prendergast et  
832 al. (2017) and Guest et al. (2017), who found no systematic changes in the ABR or the frequency-  
833 following response as a function of noise exposure. The current study, using a wide range of  
834 behavioral measures, further supports the idea that the amount of cumulative lifetime exposure to  
835 high intensity sounds is not related to meaningful changes in auditory perception in young,  
836 audiometrically normal adults. However, it is possible that behavioral performance is relatively  
837 insensitive to synaptopathy. Oxenham (2016) applied a theoretical model based on signal detection  
838 theory to demonstrate that a 50% loss of synapses would lead to a decrease in d-prime on a typical  
839 psychophysical task by a factor of  $\sqrt{2}$ , which is close to the limits of test sensitivity, and well within  
840 the range of expected variability across audiometrically normal young adults. This analysis suggests  
841 that, even if substantial synaptopathy occurs, it may be difficult to measure its effects on perception.  
842 There are also some potential limitations in our methodology that should be considered. One  
843 possible limitation is that the stimuli for the four psychophysical tasks were narrowband, and hence  
844 for the high-level conditions, off-frequency listening (particularly on the high-frequency side of the  
845 excitation pattern) may have contributed to performance. This may have reduced the impact of low-  
846 SR fiber loss by recruiting unsaturated high-SR fibers. Another possibility, discussed by Prendergast

847 et al. (2017), is that our retrospective self-report measure of noise exposure is too unreliable to  
848 distinguish individuals in terms of potential synaptopathy. However, as we argued previously, the  
849 differences in estimated exposure between the lowest and highest exposed were so great that it is  
850 unlikely that meaningful effects were washed out by imprecision in the estimates. In addition,  
851 essentially the same noise measure was significantly predictive of tinnitus in a recent study (Guest  
852 et al., 2017), even though the range of exposures and number of participants were smaller than in  
853 the present study. This suggests that the measure is sufficiently sensitive to distinguish between  
854 participants in terms of exposure.

855

856 Despite these caveats, our findings across the three studies from our laboratory to date are  
857 consistent with the hypothesis that noise-induced cochlear synaptopathy is insignificant in young  
858 humans with normal audiograms. In animal models, it is possible to titrate the noise exposure so as  
859 to deliver the maximum intensity possible without permanent threshold shift. The exposures  
860 encountered by humans are not so precise, and it may be that exposures sufficient to significantly  
861 reduce the number of cochlear synapses are also likely to lead to a loss of OHC function and an  
862 elevation of audiometric thresholds, particularly at high frequencies. Dobie and Humes (2017)  
863 discussed the difficulties involved in extrapolating the exposure levels used in the animal work to  
864 the human listener. They used historical evidence from human studies, in which very intense  
865 laboratory exposures were used, and the degree of temporary threshold shift as a proxy for damage  
866 to the auditory system. They argued that human listeners require much higher exposures than  
867 rodents to produce equivalent damage. The studies that have reported a decrease in wave-I ABR  
868 amplitude with noise exposure (Bramhall et al., 2017) and an increase in SP/AP ratio (Liberman et  
869 al., 2016) also reported audiometric differences between the groups. As discussed previously, there  
870 are differences in sensitivity in the 3000-6000 Hz range in the Bramhall et al. (2017) study.  
871 Liberman et al. (2016) reported significant differences in audiometric sensitivity between low and

872 high exposure groups at 10 kHz and above, and a non-significant difference between the two groups  
873 at 8 kHz.

874

875 There are two competing hypotheses regarding the relation of audiometric loss to the differences in  
876 ABR waveforms between the exposure groups observed in some studies. The first is that high-  
877 frequency threshold elevations, and perhaps mild low-frequency (<8 kHz) threshold elevations, are  
878 markers for synaptopathy, and that the electrophysiological effects are a direct result of noise-  
879 induced synaptopathy. A second hypothesis is that the electrophysiological effects and the high-  
880 frequency audiometric deficits share the same cause: basal hair cell dysfunction, as opposed to  
881 cochlear synaptopathy at lower frequencies. As Liberman et al. (2016) suggest, the use of high-  
882 frequency masking noise to remove the contribution from basal regions when making ABR  
883 recordings may help to differentiate between these hypotheses.

884

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891

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1116

1117 **Figure Captions:**

1118 Fig. 1. Noise exposure scores as a function of age for 137 participants. The regression line is plotted  
1119 with the Pearson correlation coefficient shown in the text (\* = 0.05, \*\* =  $p < 0.01$ ).

1120

1121 Fig. 2. Pure tone audiometric thresholds (averaged across ears and listeners) are shown, with 95%  
1122 confidence intervals, for the whole group and for the 25% of participants with the highest and  
1123 lowest noise exposures.

1124

1125 Fig. 3. The four panels show the results of the four psychophysical tasks: Frequency difference  
1126 limens (FDL), intensity difference limens (IDL), interaural phase difference discrimination (IPD),

1127 and amplitude modulation detection (AMD). Mean thresholds and 95% confidence intervals are  
1128 plotted for the 25% of participants with the lowest and highest lifetime noise exposures for the four  
1129 conditions of each task.

1130

1131 Fig. 4. Mean thresholds (and 95% confidence intervals) are shown for the DTT, CRMc and CRMo  
1132 speech tasks. The SNRs required for 25%, 50% and 75% correct on the psychometric function are  
1133 plotted for the 25% of participants with the highest and lowest noise exposures in black (closed) and  
1134 green (open) symbols, respectively.

1135

1136 Fig. 5. Mean localization error (and 95% confidence intervals) for the 25% of participants with the  
1137 lowest and highest noise exposures (green and black lines, respectively).

1138

1139 Fig. 6. Mean pleasantness ratings are shown (along with 95% confidence intervals) for the 11 dyads  
1140 in the consonance task. Results for the 25% of listeners with the lowest and highest lifetime noise  
1141 exposures are plotted in green and black, respectively.

1142

1143 Fig. 7. Mean ratings (and 95% confidence intervals) for the Speech, Spatial, and Qualities scales of  
1144 the SSQ. Results for the 25% of listeners with the lowest and highest lifetime noise exposures are  
1145 shown by green open squares and black solid squares, respectively.

1146

1147

1148

1149

1150 **Tables**

1151 **Table 1. Spearman's rho coefficients are shown for the relation between thresholds for each of**  
 1152 **the four psychophysical tasks (and the two differential measures) and lifetime noise exposure,**  
 1153 **lifetime noise exposure controlling for musical experience, and musical experience. Conditions**  
 1154 **are labelled with the letter denoting frequency [(L)ow or (H)igh] and the numeric value**  
 1155 **indicating sound level (40 or 80, respectively). Positive correlations indicate results in the**  
 1156 **predicted direction (worse performance with increasing noise exposure) for the correlation**  
 1157 **and partial correlation with noise exposure. For musical experience, negative correlations**  
 1158 **indicate results in the predicted direction (better performance with increasing musical**  
 1159 **training). \* =  $p < 0.05$ ; \*\* =  $p < 0.01$  (uncorrected).**

1160

Task (N)	Condition					
	L40	L80	H40	H80	H80 – L80	H80 – H40
Correlation with noise exposure						
FDL (138)	-0.11	-0.09	0.14	-0.13	0.03	-0.23 **
IPD (138)	-0.05	-0.16	0.03	0.08	0.19 *	0.04
IDL (134)	-0.02	0.11	0.02	-0.06	-0.17 *	-0.09
AMD (133)	0.02	0.08	-0.03	-0.20 *	-0.24 **	-0.21 *
Correlation with noise exposure, controlling for musical experience						
FDL (138)	-0.01	0.15	0.06	-0.04	-0.03	-0.19*
IPD (138)	-0.04	0.07	-0.10	0.10	0.17*	0.04
IDL (134)	0.01	0.09	0.16	-0.03	-0.16	-0.09
AMD (133)	-0.11	0.04	0.16	-0.11	-0.21*	-0.18*
Correlation with musical experience						
FDL (138)	-0.26**	-0.36**	0.00	-0.22**	0.16	-0.16
IPD (138)	-0.05	-0.16	-0.08	-0.03	0.10	-0.00
IDL (134)	-0.08	-0.10	-0.19*	-0.23**	-0.07	-0.01
AMD (133)	-0.23**	-0.19*	-0.19*	-0.26**	-0.13	-0.12

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1163 **Table 2. Spearman's rho coefficients are shown for the relation between threshold on the speech tasks (and the differential measure) and**  
 1164 **lifetime noise exposure, lifetime noise exposure controlling for musical experience, and musical experience. Otherwise as Table 1.**

Task (N)	Correlation with noise exposure			Correlation with noise exposure, controlling for musical experience			Correlation with musical experience		
	40 dB SPL	80 dB SPL	80 – 40 dB SPL	40 dB SPL	80 dB SPL	80 – 40 dB SPL	40 dB SPL	80 dB SPL	80 – 40 dB SPL
<b>DTT (139)</b>									
75%	0.12	-0.08	-0.11	0.10	-0.05	-0.08	0.08	-0.09	-0.10
50%	0.16	-0.12	-0.21 *	0.12	-0.09	-0.16	0.11	-0.09	-0.17 *
25%	0.17 *	-0.13	-0.24 **	0.14	-0.05	-0.20 *	0.10	-0.07	-0.14
<b>CRMc (136)</b>									
75%	-0.19 *	-0.01	0.09	-0.14	0.03	0.07	-0.15	0.10	0.04
50%	-0.18 *	0.02	0.21 *	-0.11	0.03	0.19 *	-0.20 *	-0.03	0.10
25%	-0.15	-0.06	0.21 *	-0.08	0.09	0.19 *	-0.19 *	-0.04	0.10
<b>CRMo (136)</b>									
75%	-0.06	-0.11	-0.09	-0.02	-0.08	-0.10	-0.10	-0.07	-0.01
50%	-0.11	-0.09	-0.12	-0.05	-0.09	0.15	-0.16	-0.02	0.05
25%	-0.11	-0.10	-0.09	-0.05	0.11	0.11	-0.15	0.03	0.03

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1170 **Table 3. Spearman's rho coefficients are shown for the relation between the FFR measures and threshold for each of the behavioral tasks.**  
1171 **Conditions are labelled with the letter denoting frequency [(L)ow or (H)igh] and the numeric value indicating sound level (40 or 80 dB SPL,**  
1172 **respectively). For the L40 and L80 conditions, correlations were with the 255-Hz pure-tone FFR. For the H40 and H80 conditions, correlations**  
1173 **were with the envelope FFR for a 4000-Hz carrier amplitude modulated at 255 Hz. For the differential measures (H80-L80, and H80-H40),**  
1174 **correlations were with the differential FFR measure (envelope FFR minus pure-tone FFR). In each case, the predicted relation between the**  
1175 **FFR measure and performance is a negative one. Those with noise-induced synaptopathy are expected to have lower FFR scores and poorer**  
1176 **(higher) psychophysical thresholds. \* =  $p < 0.05$ ; \*\* =  $p < 0.01$  (uncorrected).**

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	<b>Condition</b>					
<b>Task (N)</b>	<b>L40</b>	<b>L80</b>	<b>H40</b>	<b>H80</b>	<b>H80 – L80</b>	<b>H80 – H40</b>
FDL (123)	-0.08	0.00	-0.06	0.08	-0.03	0.09
IPD (123)	-0.12	0.05	0.04	-0.06	-0.15	-0.13
IDL (119)	-0.08	-0.15	-0.09	0.04	-0.01	0.00
AMD (119)	-0.19 *	-0.06	0.04	0.15	0.12	0.11

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1184 Figure 1

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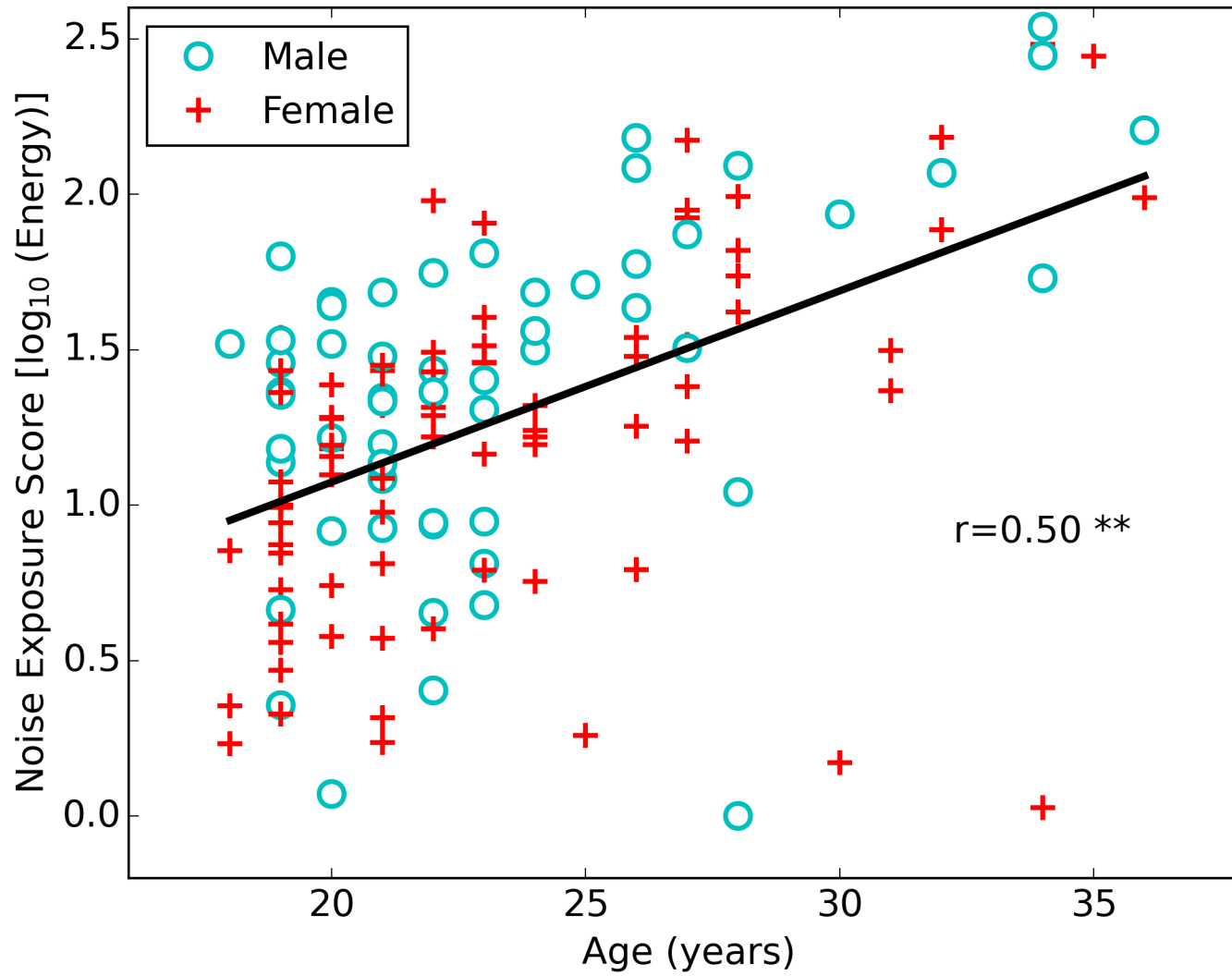
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1205 Figure 2

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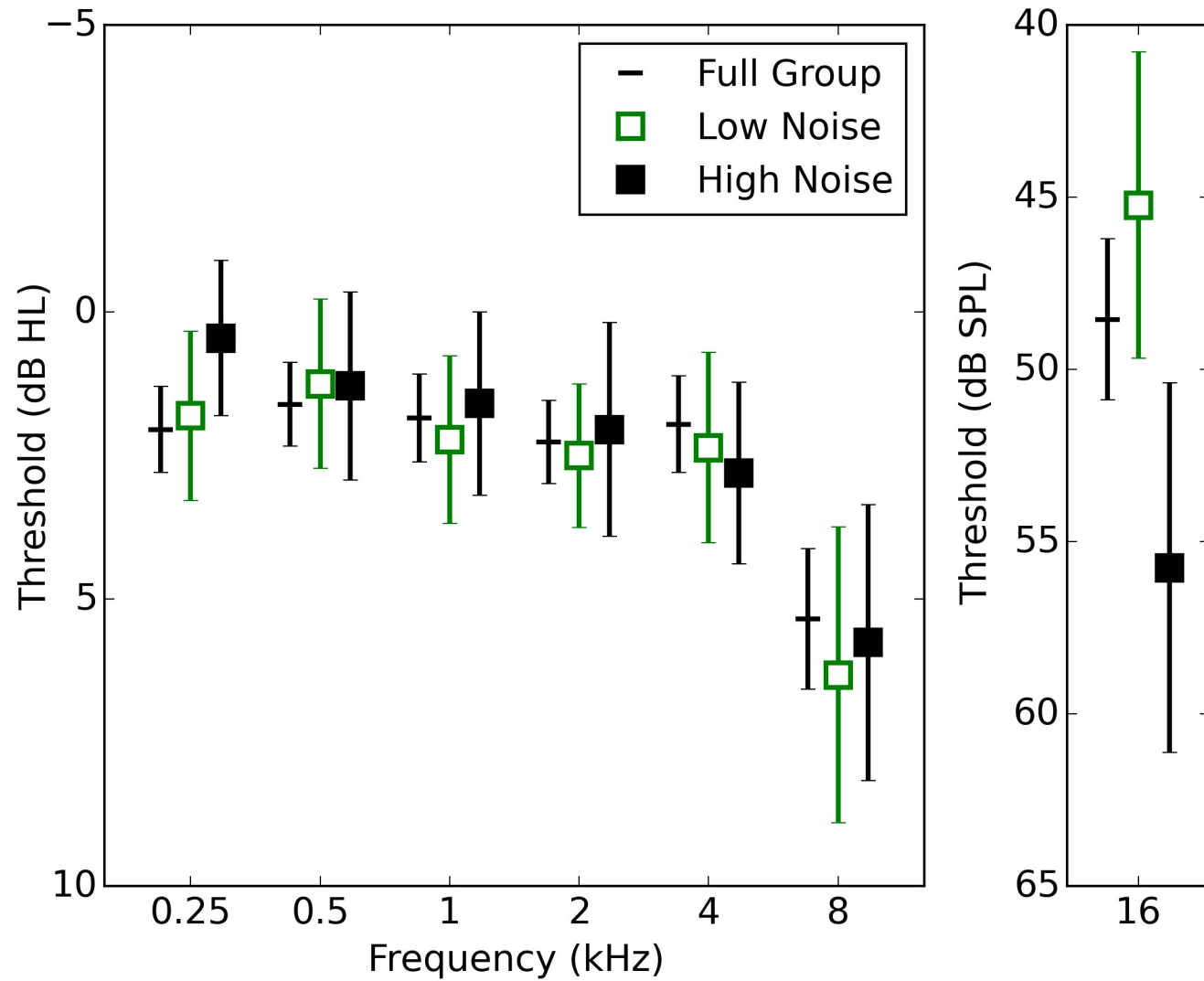
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1226 Figure 3

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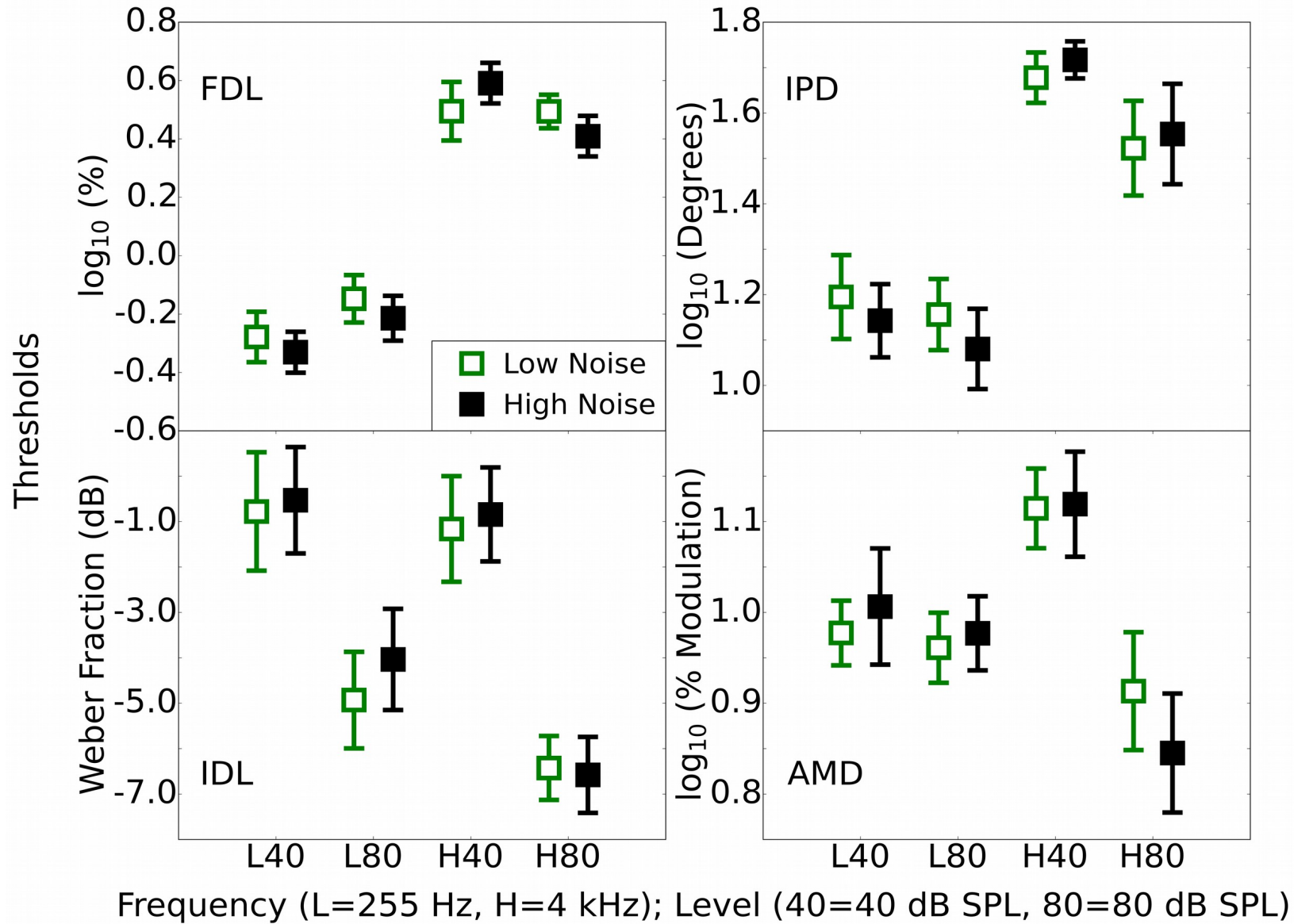
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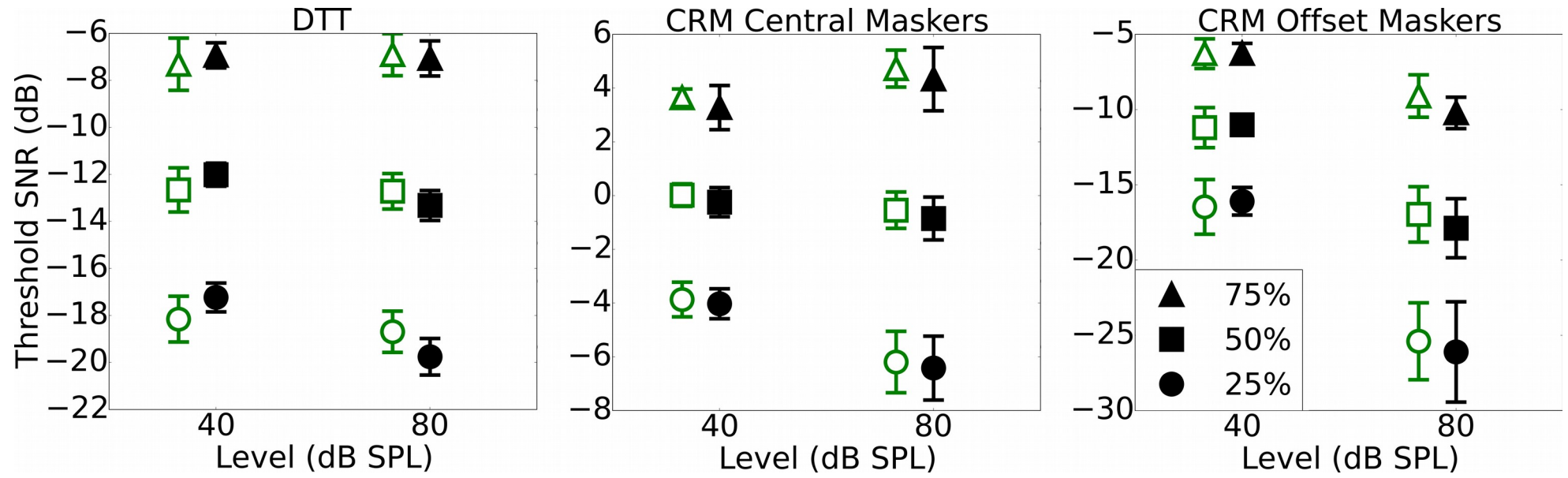
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1247 Figure 4

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1258 Figure 5

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