



Dhvar5 antimicrobial peptide (AMP) chemoselective covalent immobilization results on higher antiadherence effect than simple physical adsorption

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Abstract

Bacterial colonization and subsequent biofilm formation is still one of the major problems associated with medical devices. Antimicrobial peptides (AMP) immobilization onto biomaterials surface is a promising strategy to avoid bacterial colonization. However, a correct peptide orientation and exposure from the surface is essential to maintain AMP antimicrobial activity.

This work aims to evaluate the effect of the immobilization on antibacterial activity of Dhvar5 (LLLFLKKRKRKY), an AMP with a head-to-tail amphipathicity. Dhvar5 was linked to thin chitosan coatings in i) a controlled orientation and exposure, testing covalent immobilization of its N- or C-terminus and using spacers with different lengths and flexibilities or in ii) a random orientation by physical adsorption. Chitosan coating was chosen due to its antimicrobial properties and readiness to be functionalized.

Surface characterization demonstrated the chemoselective immobilization of the peptide with different spacers in a similar concentration (~2 ng/cm²).

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Efficacy assays demonstrated that covalent immobilization of Dhvar5 exposing its cationic end, improves the chitosan coating antimicrobial effect by decreasing Methicillin-resistant *Staphylococcus aureus* (MRSA) colonization. This effect was enhanced when longer spacers were used independently of their flexibility. In opposite, immobilized Dhvar5 exposing its hydrophobic end has no effect on bacterial adhesion to chitosan, and when adsorbed in a random orientation even induces bacterial adhesion to chitosan coating.

1. Introduction

Prevention of bacterial adhesion and biofilm formation on the surface of biomaterials remains a serious clinical issue yet unsolved. A number of different coating strategies, either for exposure or release of bactericidal substances (e.g., silver, quaternary ammonium compounds, and classic antibiotics) have been tested along the past years [1-4]. However, the application of such coatings has been limited by associated side-effects, as cytotoxicity, hypersensitivity or the progressive alarming emergence of multi-resistant pathogens.

Antimicrobial peptides (AMP) are a class of promising antibiotic compounds with the major advantages being broad spectrum of activity, high efficiency at low concentrations, fast killing, good cytotoxic profile, and importantly, they rarely promote the rise of bacterial resistance [5,6]. For the majority of these peptides, the mode of action suggested is peptide insertion into bacterial membranes with subsequent cell death induction by, in some cases, cell lysis. Dhvar5 is a synthetic peptide, derived from the histatins family, which are produced by the salivary glands. Dhvar5 is a variant of Dh-5 (histatin 5 active domain, amino acids 11e24) with an N- to C-terminal amphipathicity. It was firstly described as strongly active against *Candida albicans*, but has also a potent and broad antibacterial activity, even against methicillin-resistant *Staphylococcus aureus* (MRSA) [7-9]. The exact mechanism of action of soluble Dhvar5 is still not fully elucidated. Some cues emerged from the work by Amerongen and co-workers [10,11], where it was demonstrated that Dhvar5 binds to the membrane of yeast cells and induces leakage of intracellular content, but without permanent pore formation. The broad spectrum of Dhvar5, together with its safe cytotoxic profile, prompted its application on osteomyelitis prevention models. However, although the peptide revealed *in vivo* activity, it did not achieve the same treatment levels than gentamicin [12]. This situation may be associated with the pharmacokinetics challenges posed by AMP, as these are prone to undergo proteolytic degradation, self-aggregation and aggregation with plasma proteins. As previously summarized by us [13], covalent immobilization of AMP may offer the answer to such difficulties. Moreover, this strategy prevents the formation of a peptide concentration gradient from the implant surface, avoiding the side-effects associated with releasing therapies. Still, peptide immobilization is not a straightforward issue, as a number of different parameters should be taken into account, such as proper orientation (N- vs. C-terminal immobilization) and selection of an adequate spacer/linker (length and flexibility) for an optimal exposure.

2. Materials and Methods

2.1- Dhvar5 synthesis and characterization

Peptide Dhvar5 (LLLFLLLKKRKKRKY C-terminal amide) and its derivatives (Table 1) were produced by Fmoc/tBu solid-phase peptide synthesis methodologies assisted with microwave (MW) energy (Liberty 1 Microwave Peptide Synthesizer, CEM Corporation) [14,15]. Dhvar5-

derived peptides were produced in order to introduce a terminal cysteine for subsequent immobilization. Different spacers were placed between the additional Cys and the bioactive sequence: 4-aminobutanoic (ABA) and 6-aminohexanoic (AHA) acids were used as flexible spacers of different length, whereas the dipeptide GlyGly (GG) was used as a spacer with comparable length to that of AHA, but lower flexibility, as peptide bonds do not allow the same conformational freedom as that of alkyl chains.

The crude peptides were purified by reverse-phase liquid chromatography and confirmed by High Performance Liquid Chromatography (HPLC) (Hitachi-Merck LaChrom Elite), Liquid Chromatography-Electrospray Ionization/Ion Trap Mass Spectrometry (LC-ESI/IT MS) (LCQ-DecaXP LC-MS system, ThermoFinnigan). Purified peptides used presented a purity level higher than 90%.

2.2. *Dhvar5* surface immobilization

2.2.1. Substrates preparation

Titanium substrates (Ti) were used to represent prosthesis surface and gold substrates (Au) were used due to their higher suitability for some of the surface characterization techniques used, such as ellipsometry and Infrared Reflection-Absorption Spectroscopy Analysis (FT-IRRAS). Ti and Au (1 x 1 cm²) were produced, cleaned and characterized according to references [16] and [17], respectively. Briefly, TiO₂ films (50 nm) were deposited on silicon wafers (polished/etched, crystal orientation <100>, from AUREL GmbH) by ion beam sputtering from a Ti cp target, in the presence of a mixed Ar-O₂ beam coming from the assist gun (15.02% O₂ in Ar). For the Au substrates, chromium (5 nm) and gold (25 nm) layers were deposited by ion beam sputtering from chromium and gold targets (99.9% purity) on silicon wafers (AUREL, GmbH). Chromium was used to improve gold adhesion to silicon. Both substrates were cleaned with "piranha" solution (7 parts of H₂SO₄ and 3 parts of 30% H₂O₂) for 90 s (Ti) and 5 min (Au) (*caution: this solution reacts violently with many organic materials and should be handled with extreme care*) and successively rinsed with ethanol, MilliQ water, ethanol and dried with a gentle stream of argon.

2.2.2. Preparation of chitosan ultrathin films

Chitosan ultrathin films were produced as previously described [18]. Briefly, commercial squid pen chitosan (France Chitine) was purified by the re-precipitation method [19] resulting on a molecular weight of 283,000-472,000 with a deacetylation degree (DD%) of ~85%. Chitosan ultrathin films (Ch) were prepared by spin coating (9000 rpm during 1 min; Laurell Technologies Corporation, North Wales) a chitosan solution (0.4% in acetic acid w/v) [20] on the center of the Au substrates. The ultrathin films produced were then neutralized with 0.1 M NaOH and rinsed with MilliQ water. Each sample was dried with a gentle stream of argon and stored in plastic Petri dishes saturated with argon.

2.2.3. Introduction of SH groups onto chitosan films

Functionalization of chitosan thin films with *N*-acetyl cysteine (NAC), for introduction of SH groups, was previously optimized by Costa et al. [18], through employment of carbodiimide chemistry. Briefly, chitosan thin films were treated with a solution of 0.2 m 1-Ethyl-3-[3-dimethylaminopropyl] carbodiimidehydrochloride (EDC; Sigma-Aldrich), 0.05 m *N*-hydroxysulfosuccinimide (NHS; Sigma-Aldrich) and 25 mM NAC (Merck), in 0.1 m (*N*-morpholino)ethanesulfonic acid (MES; Sigma-Aldrich) buffer at pH = 6.5, for 1 h, at 37 °C and

100 rpm. The modified films were then rinsed with MilliQ water and immersed 1 min on an ultrasound bath (Bandelin Sonorex Digitec Bath 35 kHz) and rinsed again with MilliQ water.

2.2.4. Peptide immobilization

Dhvar5 immobilization on chitosan thin films was obtained through disulfide bridge formation between the side chain thiol of the terminal cysteine of the peptide and sulfhydryl groups (SH) on pre-functionalized chitosan (Fig. 1).

Functionalized chitosan substrates were incubated with 1.5 mg/ml peptide solutions in 10 mM TrisHCl pH = 8.0, under oxidative conditions (20% dimethyl sulfoxide (DMSO)) for 18 h at 37 °C and 120 rpm. A control Dhvar5-adsorbed sample was prepared by incubation with a non-functionalized chitosan film in the same reaction conditions.

2.3. Surface characterization

2.3.1. FT-IRRAS

Measurements were performed on a Perkin Elmer FTIR spectrophotometer, model 2000, coupled with a VeeMax II Accessory (PIKE) and a liquid-nitrogen-cooled MCT detector. In order to ensure that there was no water vapor adsorption, dry nitrogen was purged into the instrument for 5 min before and during measurement of each sample. For each substrate, a similar gold surface was used as a background. Incident light was p-polarized and spectra were collected using the 80° grazing angle reflection mode. For each sample, 100 scans were collected with 4 cm⁻¹ resolution.

2.3.2. Ellipsometry

Ellipsometry measurements were performed using an imaging ellipsometer, model EP³, from Nanofilm Surface Analysis. This ellipsometer was operated in a polarizer-compensator-sample-analyzer (PCSA) mode (null ellipsometry). The light source was a solid-state laser with a wavelength of 532 nm. The gold substrate refractive index ($n = 0.5837$) and extinction coefficient ($k = 2.5113$) were determined by using a delta and psi spectrum with an angle variation between 65° and 71°. These measurements were made in four zones to correct for any instrument misalignment. The thickness of the chitosan films was determined considering $n = 1.54$ and $k = 0$, for the chitosan film [21]. Results are presented as the average of three measurements on each of two samples.

2.3.3. Water contact angle measurements

Water contact angle measurements were performed using the sessile drop method with a contact angle measuring system from Data Physics, model OCA 15, equipped with a video CCD-camera and SCA 20 software, as described at [17]. After deposition of 4 µl drops of MilliQ water, images were taken every 2 s over 300 s. Droplet profiles were fitted using Young-Laplace formula, to calculate the contact angle. The water contact angle of each substrate was calculated by extrapolating the time dependent curve to zero. Results are the average of three measurements on three independent samples.

2.3.4. Peptide surface density determination

The quantification of the immobilized peptides was performed through colorimetric reaction using 9,10-phenanthrenequinone (PHQ, Fluka), that reacts with arginine forming a stable

compound which gives out fluorescence upon excitation [22]. The protocol used was adapted from Ref. [23]. Substrates were sonicated 1 h in 0.1 M HCl (1 ml) in an ultrasound bath to dissolve the modified chitosan films. Then, 1 ml of each sample solution was added to 3 ml of 3.5 μ M PHQ in absolute ethanol, followed by the addition of 0.5 ml of 2 M NaOH. The mixture was then incubated at 30 °C for 3 h. Finally, 2.25 ml of 2.4 M HCl was added to stop the reaction. The fluorescence emission was measured using a fluorescence microplate reader (Biotek Synergy Mx Luminometer) using an excitation wavelength of 256 nm, and detecting the emission at 380 nm. The amount of Dhvar5 was calculated based on a calibration curve prepared with standard solutions of free L-arginine (Fluka) and free Dhvar5. Standard solutions of free Dhvar5 were adjusted by quantification at 280 nm in a Thermo Scientific NanoDrop® 1000 spectrophotometer.

2.4. Bacterial assays

2.4.1. Bacterial strains, media and growth conditions

An MRSA strain of *S. aureus* was obtained from the American Type Culture Collection (ATCC 33591). Bacteria were firstly grown on Tryptic Soya Agar (TSA) (Merck) and then overnight on Tryptic Soya Broth (TSB) (Merck) at 37 °C, 150 rpm. Bacterial suspensions were adjusted by measuring Optical Density (600 nm). Bacterial numbers were confirmed by a retrospective viable count.

2.4.2. MIC

Minimal Inhibitory Concentration (MIC) was established with a modified broth microdilution method in Mueller Hinton Broth (MHB) [24].

2.4.3. Surface antimicrobial activity characterization

2.4.3.1. Sample preparation. All substrates were washed successively in 70% ethanol and sterile water, and then dried in sterile environment. Samples were then tape glued onto flat-bottomed 24-well cell suspension culture plates (Sarstedt, Ltd, Newton, USA).

2.4.3.2. Surface viability assay. Bacterial solution (10^7 CFU/ml) was added to each well and incubated at 37 °C and 150 rpm for 2 h in MHB. Surrounding wells were filled with sterilized deionized water, in order to avoid medium evaporation. Substrates were rinsed with 0.9% NaCl sterile solution, and then stained with a combination dye of the LIVE/DEAD® Bacterial Viability Kit (*BaClight*™) for 15 min in the dark. Briefly, the kit contains two fluorescent dyes, *Syto9* which stains all bacteria in green, and propidium iodide (PI) which can only crossover damaged cells membranes and gives red stained cells. Thus, because PI quenches the fluorescent emission of *Syto9*, it is assumed that green cells are alive whereas red cells are dead. Images were obtained with an inverted fluorescence microscope (Axiovert 200M, Zeiss, Germany). For quantifying the viability of adherent bacteria, eight fields on each of triplicate replicates were obtained with a 1000x magnification, corresponding to a net area of about 0.1181 mm²/sample. The bacteria count was performed using the manual counting software included in ImageJ software.

2.4.3.3. Long-term surface adhesion assay. Bacterial solution (10^7 CFU/ml) in MHB was added to each well containing the substrates. Cells were allowed to adhere for 2 h at 37 °C and 120 rpm. Non-adherent bacteria were removed by washing three times with PBS at 120 rpm for 5 min. Thereafter, samples were placed on a new 24-well plate and incubated with fresh MHB for 24 h at 37 °C and 120 rpm. Again, all unused wells were filled with sterilized deionized water, in order to avoid medium evaporation. At this point samples were rinsed with PBS, and fixed with

4% (w/v) paraformaldehyde solution (Merck) for 20 min. Samples were rinsed again with PBS and stained with VECTASHIELD® Mounting Medium with DAPI (40,6-diamidino-2-phenylindole; Vector). DAPI bound to bacterial DNA is excited at about 360 nm and emits at about 460 nm, resulting on blue fluorescence. Images were obtained with an inverted fluorescence microscope (Axiovert 200M, Zeiss, Germany). The quantification of adhered bacteria was performed as previously explained.

2.4.3.3.1. Growth inhibition assay. After the 24 h incubation period, supernatants were successively diluted and plated in triplicate on TSA. Before counting the colonies, plates were incubated at 37 °C for 18 h.

2.5. Statistical analysis

Statistical analysis was performed using One way ANOVA with Bonferroni multiple comparison post-hoc test. When Gaussian distribution was not confirmed, non-parametric test Kruskal-Wallis was applied using the Graphpad Prism program. Data is expressed as the mean \pm standard deviation (SD) and p values of <0.05 were considered significant.

3. Results

3.1. Surface characterization

Control and Dhvar5-modified surfaces were analyzed by ellipsometry, water contact angle measurement, FT-IRRAS and fluorimetric assays.

3.1.1. Ellipsometry

The spin-coating process resulted on chitosan ultrathin films of 9.3 ± 1.0 nm, which remained stable even after the reaction protocols, as there were no thickness changes between freshly made films and buffer-incubated films (Ch_b) (data not shown). Fig. 2A presents chitosan films thickness before and after surface modification.

The thickness of the chitosan films (Ch_b) was augmented after functionalization with NAC (Ch_NAC). The significant increase of the Ch_NAC film thickness after incubation with Dhvar5, supports the success of peptide attachment. Also, a similar increase was observed on Ch film after its incubation with Dhvar5 solution (Ch_Dhvar5_ads), suggesting peptide adsorption to the film. No significant difference was observed between the distinct orientations and spacers applied.

3.1.2. Water optical contact angle (OCA) analysis

Water optical contact angles of the control and modified Ch films are presented on Fig. 2B. The incorporation of NAC on Ch films increased significantly the hydrophilicity of the film decreasing the water contact angle from 65° to 31°. After Dhvar5 binding by its Cterminus (exposition of the more hydrophobic portion of the peptide) the water contact angle increases ($\theta_w = 67^\circ$). On the other hand, all Nt-Dhvar5 immobilized samples showed a more hydrophilic behavior ($\theta_w = 54-56^\circ$) than Ch_b, consistent with the immobilization of the peptide exposing its positively charged amino acids. No significant difference was observed between the samples with peptide immobilized by its N-terminus. Ch_Dhvar5_ads presented a water contact angle lower than

Ch_b. Its value ($\Theta_w = 60^\circ$) is between the surfaces with peptide immobilized by its N-terminus and its C-terminus, suggesting some adsorbed peptide in a random orientation.

3.1.3. FT-IRRAS

FT-IRRAS results of the chitosan thin films, before and after immersion on buffer solution, showed that the films remained stable even after chemical procedures (Data not shown). FT-IRRAS analysis of Dhvar5 immobilized onto chitosan showed very similar spectra, therefore Fig. 3A depicts spectra of control Ch (Ch_b), and a representative spectrum of Dhvar5 immobilized onto Ch films.

Ch_b spectrum allowed the identification of characteristic absorption bands of chitosan, as previously described [19,20,25-27]. After Ch functionalization with NAC, an increase of amide I absorption band (1654 cm^{-1}) was observed. This is consistent with the carbodiimide-mediated coupling reaction applied, leading to formation of an amide bond between free amine groups in Ch and the carboxylic groups of NAC. Subsequent covalent immobilization of Dhvar5-derived peptides also implies an increase of amide I band, characteristic of peptides/proteins. To assess Dhvar5 immobilization, a peak height ratio (amide I peak height (1654 cm^{-1})/C-O-C glucopyranose peak height (1083 cm^{-1})) was calculated (Fig. 3B). As expected, the aforementioned ratio increased in the following order: Ch_b < Ch_NAC < Ch films with covalently bound Dhvar5. All samples with covalently immobilized peptide presented a nearly identical ratio that was around 1.5 fold higher than Ch_NAC and about 3 fold higher than Ch_Dhvar5_ads. Altogether, FT-IRRAS results clearly support the success of the covalent immobilization chemistry applied.

3.1.4. Peptide quantification

The average surface peptide density is presented on Table 2. The average surface density was similar between all Ch films with covalently bound Dhvar5 ($\sim 2.0\text{ ng/mm}^2$). The film with adsorbed Dhvar5 (Ch_Dhvar5_ads), although with a higher density (4.0 ng/mm^2), was not significantly different from the covalently immobilized samples, with the exception of Ch_AHA_Nt-Dhvar5.

3.2. Antimicrobial activity characterization

Dhvar5 antimicrobial activity was firstly assessed in solution, by an adaptation of the microtiter broth dilution method proposed elsewhere [24,28]. *S. aureus* strain used presented a MIC of $0.5\text{ }\mu\text{g/ml}$.

3.2.1. Viability assays

Viability of bacteria attached to the surfaces was evaluated using LIVE/DEAD® Bacterial Viability Kit (Baclight™). Fig. 4A presents the average number of bacteria per mm^2 of each surface sample, after 2 h incubation at $37\text{ }^\circ\text{C}$.

Regarding total adhered bacteria, control samples (Ti and Au) exhibited high values, whereas Ch coating (Ch_b) promoted a reduction of around 40% (47% comparing to Ti and 39% comparing to Au). This result was expected, since we previously demonstrated the antimicrobial properties of this chitosan ultrathin films [18]. Remarkably, films with adsorbed peptide (Ch_Dhvar5_ads) did not significantly differ from Ti neither from Au in total adhered bacteria, demonstrating that the adsorbed Dhvar5 induced bacterial adhesion to chitosan film. In opposite, samples with peptide covalently immobilized through its N-terminus exhibited a

marked decrease as compared to Ti, reaching an ~80% reduction when a longer spacer was used (Ch_AHA_Nt-Dhvar5 and Ch_GG_NtDhvar5) ($p < 0.05$). These two Dhvar-bearing surfaces did not significantly differ from each other and revealed an anti-adherence behavior ~62% plus effective than that of Ch_b. In turn, C-terminus immobilization of Dhvar5 did not significantly differ from control Ch_b film regarding anti-adherence properties. Hence, these results clearly show that, amongst all surfaces analyzed, those coated with Ch covalently bound to Dhvar5 through a longer spacer and exposing the more hydrophilic and cationic end of the peptide were the best suited to avoid bacterial colonization.

It was also observed that most of the adhered bacteria were not dead, in all surfaces. Still, N-terminally immobilized Dhvar5 exhibited a total number of live adhered bacteria two-fold lower than Ch_b samples and five-fold lower than Ti substrates.

3.2.2. Long-term anti-adherence assays

The objective of this assay was to verify if the live adhered bacteria would proliferate if time and proper nutritional conditions were given. For that, surfaces with the 2 h incubation resulting adherent bacteria were immersed on fresh medium for 24 h. The results are presented in Fig. 4B.

Ti and Au exhibited a similar and high number of adhered bacteria that allowed an increase of the number of adherent bacteria on their surfaces regarding to the initial adherent bacteria (~2000 bacteria/mm²). Similar results were obtained for Ch_Dhvar5_ads. Ch films with immobilized Dhvar5 by its N-terminus presented the lowest bacterial adhesion levels (~70% and ~40% reduction as compared to Ti and Ch_b, respectively). However, these surfaces were not able to completely avoid bacterial proliferation, since there is an increase of the adherent bacteria during incubation (24 h). Ch coating and Ch_Dhvar5_ads were the surfaces that allowed the lowest proliferation. However, the number of adherent bacteria on these surfaces was very high.

Growth inhibition assays of the supernatants of the long-term incubation experiments are depicted on Fig. 4C. Ti substrates presented the highest value of CFU/ml, which adding to the high amount of adhered bacteria at the substrate (see Fig. 4B), confirms its lack of antimicrobial activity. No significant difference was found between Au, Ch_b and surfaces with immobilized Dhvar5. Ch_Dhvar5_ads was the substrate that contributed to the lowest number of CFU/ml in the supernatant, which may be related to elution of the peptide into the MHB.

4. Discussion

Dhvar5 presented a promising MIC of 0.5 µg/ml against a methicillin-resistant *S. aureus* (MRSA) that is lower than the reported elsewhere [8,9,12,29,30]. However, direct comparison of such values is very difficult, as a result of the lack of universal standardized methods to assess AMP activity, besides the use of different *S. aureus* strains. We chose to use the standard conditions already proposed by Wiegand et al., [24].

In this study, Dhvar5 was covalently immobilized onto chitosan thin films in order to evaluate if this strategy is able to prevent bacterial adhesion in a sustainable way. Different immobilization parameters were tested, to assess the immobilization profile that would most contribute to such goal. Different surface characterization techniques - ellipsometry, FT-IRRAS, OCA and fluorimetric peptide quantification - confirmed the production of stable chitosan thin films, with

a chemoselective covalent immobilization of the peptide in different orientations. The stability of chitosan films was confirmed using ellipsometry and FT-IRRAS. Ellipsometry measurements demonstrated a clear thickness increase of Dhvar5-modified chitosan films comparing to controls (Ch_b and Ch_NAC). However, such analysis alone did not prove the covalent immobilization of the peptide, nor its proper orientation. Demonstration of the covalent immobilization of the peptide was suggested by FTIRRAS analysis, namely through comparison of the amide I peak height (1654 cm^{-1})/C-O-C glucopiranosose peak height (1083 cm^{-1}) ratio, that was clearly increased when Dhvar5 was covalently bound to chitosan, as compared to NAC-functionalized chitosan and Ch_Dhvar5_ads. The peak height ratio was also increased on Ch_Dhvar5_ads comparing to unmodified chitosan. In this case the amide I peak is related to the peptide bonds of the adsorbed peptide and not to the covalent immobilization amide bond, noticeable by a lower peak ratio increase. Regarding the specificity of the immobilization orientation, useful information was brought by OCA measurements. NAC-functionalized chitosan films became significantly more hydrophobic (2.1 fold) upon immobilization of Dhvar5 through its C-terminus (Dhvar5 hydrophobic portion exposed) and only 1.7 fold more hydrophobic when immobilization was made through the N-terminus of the peptide (cationic residues exposed). OCA also enabled the confirmation of Dhvar5 adsorption, by the small but significant contact angle shift in Ch_Dhvar5_ads comparing to Ch_b. This shift may be the result of multiple orientations of the adsorbed peptide, rather than one preferential orientation established by the covalently immobilization process, as also proposed by Chen et al., [31].

Antimicrobial activity of control and peptide-bearing surfaces was assessed through two levels of stringency: adhesion and viability after 2 h of incubation, and after long-term incubation (24 h). All Dhvar5 modified surfaces presented a significant bacterial adhesion reduction when compared to Ti and chitosan with the exception of Dhvar5 adsorbed sample. Interestingly, the adsorbed strategy exhibited an amount of adhered bacteria quite similar to controls (Ti and Au). Also, Williams et al. [32], reported a study where contact lenses with adsorbed lactoferrin exhibited a high adherence of *Pseudomonas aeruginosa*.

Covalently immobilized Dhvar5 resulted in different profiles depending on the exposed peptide terminus. C-terminally immobilized Dhvar5 maintained the level of bacterial adhesion of Ch_b after 2 h incubation, but had a higher number of adhered bacteria on 24 h incubation. This suggests that in a long-term incubation, exposure of the hydrophobic portion of the peptide masks Ch_b intrinsic activity, resulting in unwanted adhesion. In opposite, N-terminally immobilized Dhvar5 have the lowest bacterial adhesion in both incubation periods. However, the viability of adhered bacteria was high independent of the terminus used for immobilization, suggesting that we have a stronger anti-adherence rather than antimicrobial effect. Confronting the levels of surface-adhered bacteria with those of free bacteria at the supernatants, we came to the conclusion that, in the absence of surface coating (i.e., on the Ti control), a high number of bacteria is found both at the surface and in solution. In turn, all the chitosan-coated surfaces, with or without further modification, presented similar amounts of free bacteria at the supernatants, which do not correlate with the respective lower amount of surface-adhered bacteria. Nevertheless, the high amount of bacteria at the supernatant may be the result of the proliferation of planktonic bacteria that were never in contact with the surfaces.

The lowest CFU count found in supernatants regards the surface with adsorbed Dhvar5, presumably as the result of peptide elution to the bulk phase. However, this result loses relevance given the ~70% increase of adhered bacteria in this sample, as compared with best performing Dhvar5-grafted surfaces.

Recently, Chen et al. [33], reported that melimine, a 28mer peptide with an N-terminus hydrophobic domain and cationic C-terminus, presented higher antimicrobial activity with a clear antiadherence effect when immobilized through its N-terminus, exposing the cationic

domain away from the substrate. This comes in accordance with our results. In contrast to these results, Hilpert et al. [34], found that immobilized AMP exposing their hydrophobic termini exhibited higher bactericidal activity. They stated that the hydrophobic domain should be free to be able to interact with the lipophilic portion of the bacterial membrane. However, they used a peptide library that did not include peptides with a clear 'head-tail' amphipathicity, but rather a conformation-dependent amphipathicity. Indeed, they hypothesized that a concentration of cationic residues on the exposed terminus could similarly lead to high antimicrobial activity.

Within the *N*-terminal immobilizations, differential antiadherence effects were obtained depending on the length of the spacer applied. It was clear that longer spacer (AHA or GG) had better results than shorter (ABA) spacers. The two longer spacers had very similar results, suggesting that, with this particular peptide, spacer length is more important than spacer flexibility. Bagheri et al. [35], demonstrated the importance of a longer spacer on AMP antimicrobial activity. Nevertheless, reports diverge in their general conclusion about the specific characteristics of the applied spacer, suggesting that it may be peptide-dependent. More recently, Bagheri et al. [36], tried to assess whether the mechanism of action of soluble AMP could be relevant for the correct configuration of immobilization. To that end, those authors chose different AMP with distinct putative mechanisms of action, and tested them after different tethering approaches. Overall, they concluded that peptides with intracellular targets lose activity upon covalent immobilization whereas the behavior of membrane permeabilizing peptides depend on their amphipathicity distribution. Thus, the activity of covalently immobilized peptides whose amphipathicity is conformation-dependent (as the KLAL model peptide) is not significantly affected by the orientation of immobilization. On the other hand, peptides with sequence-based amphipathicity (as melittin) should be covalently immobilized through the position farthest away from the hydrophobic domain. In other words, these authors concluded that membrane-active AMP should have their hydrophobic domain exposed in order to insert into the bacterial lipid bilayer. As reported by Ruissen et al., [10], Dhvar5 can cause cytoplasmic membrane depolarization suggestive of membranolytic activity, but not through permanent pore formation. This mechanism of action, in addition to the sequence-based amphipathicity of Dhvar5, would suggest that its optimal immobilization position should be through the *C*-terminus, as this would result on greater exposition of the hydrophobic domain. However, this does not correlate with our results, nor with the aforementioned report by Chen et al., in Ref. [33]. Our results demonstrated that immobilized Dhvar5 lost part of their antimicrobial effect against *S. aureus* independently of their immobilization orientation. Nevertheless, immobilization by the *N*-terminus, exposing the cationic part, demonstrates a high anti-adhesive effect. These apparently contradictory findings highlight the little that is known about the mechanisms of action of AMP, mostly immobilized ones, suggesting once again that soluble and immobilized AMP may not share the same mechanism of action, as recently proposed by Kizhakkedathu et al., [37]. Therefore, each individual AMP must be carefully studied regarding main parameters of immobilization towards creation of effective antifouling coatings, as herein reported for Dhvar5.

5. Conclusions

Dhvar5 covalently immobilized onto a chitosan thin coating by the *N*-terminus (exposing the cationic end), improves the antimicrobial effect of the coating by decreasing *S. aureus* colonization. This effect was enhanced when longer spacers were used independently of its



flexibility. In opposition, Dhvar5 covalent immobilization by the C-terminus did not change bacterial adhesion to chitosan and Dhvar5 physically adsorbed even induced bacterial adhesion to chitosan coatings.

This work demonstrated that, after surface immobilization, the exposition of the cationic end of this amphipathic peptide (Dhvar5) is fundamental to create antimicrobial surfaces by avoiding bacterial colonization.

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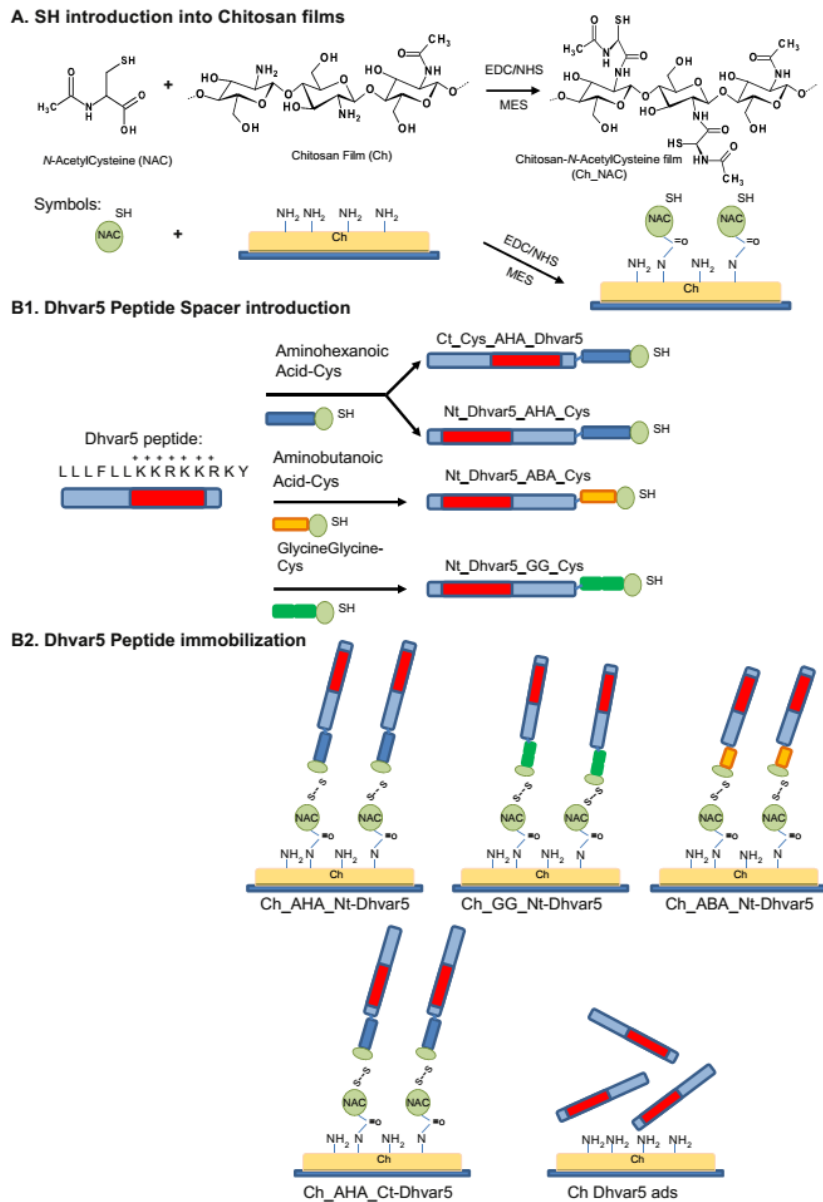


Fig. 1. A) Chitosan modification with N-acetyl cysteine (NAC); B1) Dhvar5 peptide spacer introduction; B2) Immobilization of Dhvar5-derived peptides by disulfide bridge formation (a control surface, Ch Dhvar5 ads, was used where peptide was only adsorbed, not covalently bound).

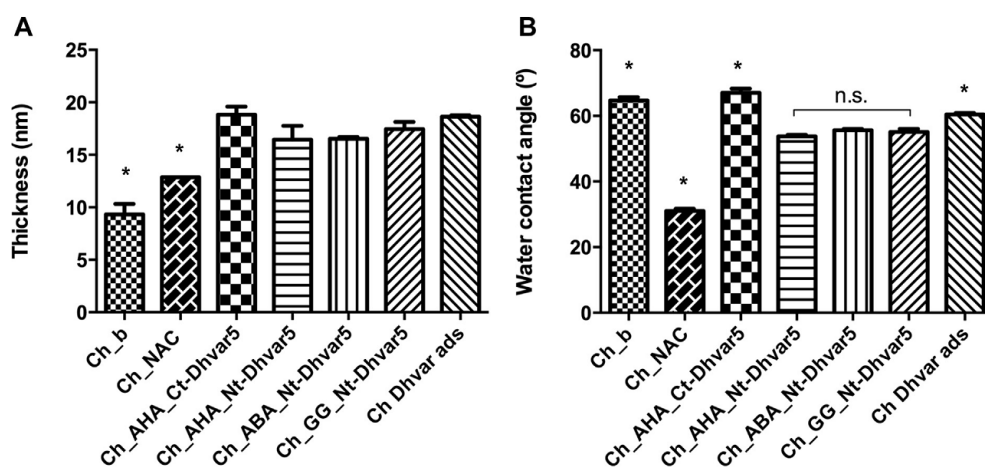


Fig. 2. A) Ellipsometry analysis of the chitosan and chitosan-functionalized films; B) Water optical contact angles of chitosan and chitosan-functionalized films. * Statistically different from all other samples ($p < 0.05$) (non-parametric Kruskal-Wallis test).

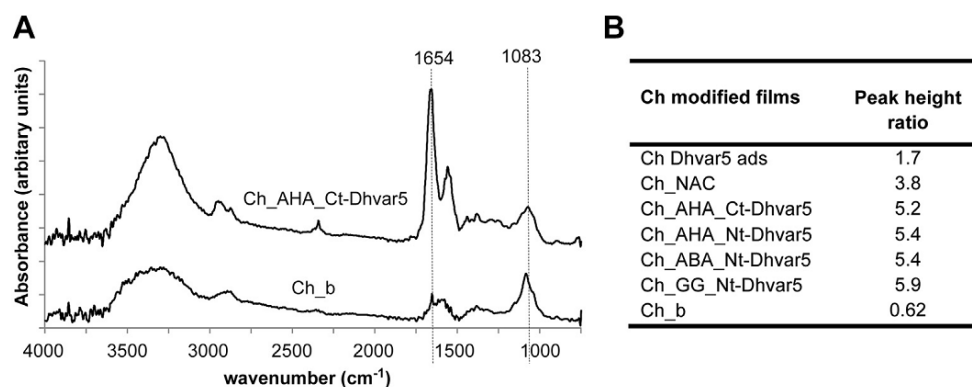


Fig. 3. A) FT-IRRAS spectra of Ch and a representative spectrum of Dhvar5 covalently immobilized onto Ch film (Ch_AHA_Ct-Dhvar5); B) Peak height ratio (amide I peak (1654 cm^{-1})/C-O-C peak (1083 cm^{-1})) of modified Ch films.

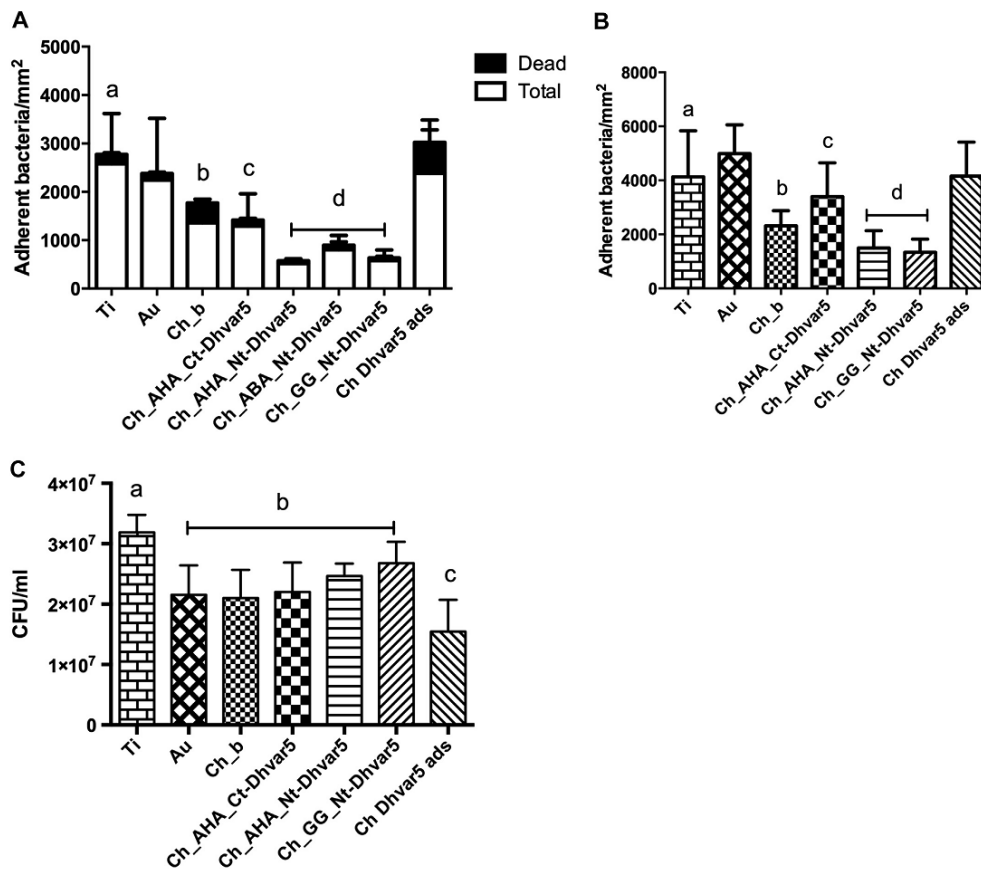


Fig. 4. A) Viability of adhered *S. aureus* incubated at 37 °C for 2 h a) statistically different from all Ch samples with the exception of Ch Dhvar5 ads ($p < 0.05$); b) statistically different from Ch_AHA_Nt-Dhvar5, Ch_GG_Nt-Dhvar5 and Ch_Dhvar5_ads ($p < 0.05$); c) statistically different from Ch_AHA_Nt-Dhvar5, Ch_GG_Nt-Dhvar5 and Ch Dhvar5 ads ($p < 0.05$); d) not statistically different; B) Total *S. aureus* adherence to surfaces after 24 h incubation period of pre-adhered inoculum. a) statistically different from Ch_b, Ch_AHA_Nt-Dhvar5, Ch_GG_Nt-Dhvar5 ($p < 0.05$); b) statistically different from Ch_AHA_Ct-Dhvar5, Ch_GG_Nt-Dhvar5 and Ch Dhvar5 ads ($p < 0.05$); c) statistically different from Nt-immobilized Dhvar5 ($p < 0.05$); d) not statistically different; C) Number of CFU/ml found on the supernatants after a 24 h period of incubation. a) statistically different from all surfaces with the exception of Ch_GG_Nt-Dhvar5 and Ch_NAC ($p < 0.05$); b) not statistically different from each other; c) statistically different from all surfaces with the exception of Au and Ch_b (One-Way ANOVA analysis).

Table 1
Dhvar5 derived-peptides for immobilization.

Peptide	Sequence
Dhvar5	LLLFLKKRKKRKY
Dhvar5-Ct_AHA_C	Dhvar5-(6-amino-hexanoyl)-Cys
C_AHA_Nt-Dhvar5	Cys-(6-amino-hexanoyl)-Dhvar5
C_ABA_Nt-Dhvar5	Cys-(4-aminobutanoyl)-Dhvar5
C_GG_Nt-Dhvar5	Cys-GlyGly-Dhvar5

Table 2

Dhvar5 surface density evaluation, based on fluorescent intensities.

Ch modified films	Dhvar5 surface density (ng/mm ²)
Ch_AHA_Ct-Dhvar5	2.4 ± 0.7
Ch_AHA_Nt-Dhvar5	1.5 ± 0.0 ^a
Ch_ABA_Nt-Dhvar5	2.1 ± 0.4
Ch_GG_Nt-Dhvar5	1.8 ± 0.2
Ch Dhvar5 ads	4.0 ± 0.9 ^a

^a Statistically different from each other ($p < 0.05$) (non-parametric Kruskal–Wallis test).