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Comparison of two Metal Ion Implantation Techniques for Fabrication of Gold and Titanium Based Compliant Electrodes on Polydimethylsiloxane

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ABSTRACT

This study contrasts the implantation of 25 μ m thick Polydimethylsiloxane (PDMS) membranes with titanium and gold ions at 10 keV and 35 keV for doses from 1x10¹⁵ at/cm² to 2.5x10¹⁶ at/cm² implanted with two different techniques: Filtered Cathodic Vacuum Arc (FCVA) and Low Energy Broad Ion Beam (LEI). The influence of the ion energy, ion type, and implantation tool on the Young's modulus (E), resistivity and structural properties (nanocluster size and location, surface roughness) of PDMS membranes is reported. At a dose of 2.5x10¹⁶ at/cm² and an energy of 10 keV, which for FCVA yields sheet resistance of less than 200 Ω /square, the initial value of E (0.85 MPa) increases much less for FCVA than for LEI. For gold we obtain E of 5 MPa (FCAV) compared to 86 MPa (LEI) and for titanium 0.94 MPa (FCVA) compared to 57 MPa (LEI). Resistivity measurements show better durability for LEI than for FCVA implanted samples and better time stability for gold than for titanium.

INTRODUCTION

Using metal ion implantation (MII) we developed a method that allows micropatterning of very compliant and optically transparent electrodes that can sustain high strains and millions of cycles, and can be used to fabricate buckling type membrane actuators with a vertical displacement of more than 25 % of the membrane's diameter [1]. Starting with a PDMS membrane with a Young's modulus 0.85 MPa, Au ion implantation at 5 keV for doses of order 10^{16} ions/cm² results in less than 1 MPa increase in Young's modulus, electrical conductivity below 1 k Ω / square, and strain of over 175% can be reached while remaining conductive.

In this paper we will present the influence of two different implantation techniques on mechanical, structural and electrical properties of Polydimethylsiloxane (PDMS) implanted with Ti and Au, at 10 keV and 35 keV, and doses between 0.1×10^{16} at/cm² and 2.5×10^{16} at/cm².

EXPERIMENTAL SETUP

The two implantation instruments, used in this study, were Filtered Cathode Vacuum Arc (FCVA) and Low Energy Broad Beam (LEI) implanter. FCVA creates 600 μ s long pulses of plasma with a beam current of 300 μ A/cm². Pulse rate is of order 1 Hz. The beam is filtered from macroparticles, yielding mostly doubly charged ions. In our case, the beam is then accelerated toward the target with an acceleration potential of 5 kV. The acceleration potential drops during each pulse because of the current from the 17.5x10¹² at/cm² doubly charged ions. LEI delivers a continuous ion current of about 0.5 μ A/cm². The ion beam is filtered, accelerated and decelerated

at the desired energy. Beam energy is stable in time. Averaged over one second, the ion currents are in the same range for both implanters, but during a pulse, the ion current produced by FCVA is much higher than that produced by LEI.

Resistance measurements were performed on 25 μ m thick PDMS on Si substrates. Data for surface roughness, dose, mechanical and structural properties were obtained on 25 μ m thick PDMS films bonded on patterned silicon chips with 2 mm and 3mm through-holes. The initial Young's modulus was 0.85 MPa. The surface roughness was measured with a Digital Instruments D3100 AFM. The TEM images were obtained with TEM Philips CM, and TEM samples were prepared using a Cryo-ultra-microtome (Leica Ultracut E) at -130°C as described in detail in [2]. A bulge Test setup was used to extract the elasticity of membranes. Once implanted the doses were determined with Rutherford Backscattering Spectroscopy (RBS).

RESULTS

MII creates a nano-composite a few nm thick, located in the top tens of nm of the surface of the elastomer. The particle density and size distribution of clusters depend on the dose, as well as on diffusion. The depth of the implanted layer depends on the ion energy. The thickness of the layers varies according to the ion type and implantation condition, and can be approximately computed for low doses with the TRIM simulation program [3]. Figure 1 shows higher implantation energies lead to larger ion distribution and deeper ion penetration. Gold ions do not penetrate as deeply as titanium, because the stopping cross-section of the ion is proportional to its mass. Hence one may expect gold to form a metallic conducting network at a lower dose and energy than titanium.

Resistance

An important increase of electrical conduction is one of the consequences resulting from MII. The conductivity rises with the dose and depends additionally on ion energy and intrinsic properties of the implanted element (e.g. electronegativity). Microscopically the phenomenon of conduction relates to the size and concentration of the clusters, as well as distance in-between (see figures 3 and 4 for microstructure). As the dose increases, inter-particle spacing decreases as they're getting bigger, till the point where first randomly connected conduction path is formed. This domain is characterized by an abrupt decrease of polymer's resistivity and is referred to as percolation domain. Above this dose the continuous metallic layer is smoothly formed and electrical properties vary only moderately with the concentration, approaching slowly to those of a thin metallic film. The electrical properties of the implanted PDMS are presented in figure 2 and are very well described by the percolation model.

The highest ratio of the electrical conductivity to dose is obtained for gold ions implanted with FCVA at 10 keV (300Ω /square at $1.75 \times 10^{16} \text{ at/cm}^2$). Gold is a better conductor than titanium and also FCVA produces a narrower distribution of ions due to the drop of the acceleration potential: during each pulse, the gold is initially implanted, and the finally deposited as the acceleration voltage drops (see TEM cross-sections in figure 3 and 4). The slowest decrease of resistance with the dose was measured on the 35 keV titanium samples, as expected from the TRIM simulation.





Figure 1. TRIM simulation of Ti and Au ion penetration depth into PDMS versus ion energy. Lower energy leads to denser distribution of ions closer to the surface.

Figure 2. Surface resistance vs. measured ion dose for different energies and implantation techniques. No data is shown for gold implanted by LEI since sputtering prevents obtained conductive layers.



Figure 3. TEM micrographs and cluster morphology of PDMS following Gold ion implantation at 10 and 35 keV using LEI and FCVA. Au implantation leads to round crystalline clusters of diameter up to 30 nm. Doses are measured by RBS. The scale bar is for all 6 photographs. The PDMS is the gray area on the bottom half of each frame. The gold particles are darker, and the carbon grid is white or light gray. The particles depth ranges from 0 nm to roughly 40 nm.

No resistance could be measured for the gold samples implanted with LEI, which is explained by the limited ion concentration. The maximal dose measured by RBS for LEI samples was 2.4×10^{16} at/cm². The reason for this is the sputtering of the composite that leads to a steady state condition of the ion concentration.



Figure 4. TEM micrographs and cluster morphology of PDMS following Titanium ion implantation at 10 and 35 keV using LEI and FCVA. Ti implantation leads to nm-size amorphous aggregates unlike gold nanoparticles in Figure 3.

Time stability measurements of the conductivity showed that for FCVA implanted samples only the gold samples with doses above 1.75×10^{16} at/cm² retained the small electrical resistance. For the higher does, the conductivity remains constant for more than 2 years. At lower doses diffusion of ions and small clusters leads to Ostwald ripening and hence to discontinuity in the conductive network.

Titanium deposited by FCVA forms a thin layer on the surface composed of small clusters that oxidize within few hours. Concerning the LEI implanted titanium samples a small increase of resistance less than 0.1% was observed. Figure 4 shows that the dark layer of the implanted titanium ions is located deeper under the surface and is thus better protected from oxidation. Also stiffening (and probable higher density) of the implanted PDMS layer was observed caused by the radiation induced structural changes. This may prevent the diffusion of the oxygen and the diffusion of the implanted ions.

At high doses the electrical properties of all the samples didn't approach thin film properties, but were showing a saturation of conductivity. For FCVA implantations, AFM observations revealed that, despite the high dose, the metal ions on the surface didn't meld into a continuous film, but stayed clustered. In the case of LEI, the sputtering and the cracking of the surface, due to the increased hardness, prevent the formation of a conductive path.

Microstructure

The microstructure of the nanocomposites is shown in figure 3. Chemical and structural modifications of polymers, and therefore the change of the physical properties, as a function of energy, dose or element have already been studied by other groups [4-8]. The energy transferred from an incoming ion to the polymer matrix can be orders of magnitude higher than typical binding energies of a polymer (15 eV). The bond breaking, producing free radicals, excited

species and volatiles, is caused by excitation and ionization of the polymer molecules as well as direct nuclear collisions. If there is a high concentration of primary radicals, then scissioned polymeric bonds react with each other, recombining or initiating cross-linking. Ti implantation with LEI heavily damaged the implanted layer. This leads to cracks in the implanted membrane, which are due to the increased hardness of PDMS. Starting with the surface roughness of 2 nm for a virgin membrane, once implanted the surface buckles into an intricate wavy pattern with root mean square height values of several hundred nanometers (see figure 5).

LEI prepared samples fit quite well with distributions presented in figure 1. FCVA images show that the "implantation" ions are also deposited on the surface, because of the drop of the accelerating potential during each pulse. One also may observe that titanium ions are homogeneously distributed in the matrix forming an amorphous composite, whereas gold clusters into crystalline 30 nm round particles, whose size increases with dose and energy. The reason for this lies in the high chemical reactivity of titanium and the high stability of gold.



Figure 5. Surface roughness vs. ion dose. Inset: AFM topography for 10 keV FCVA implantation of Au with 2.3×10^{16} at/cm². The PDMS has initial surface roughness of 2 nm. Post irradiation the roughness is due to the different coefficient of thermal expansion between the implanted and non-implanted layer of PDMS. Owing to the very high concentration of ions on the surface, building a continuous metallic layer (see TEM), the roughness decreases again at the higher doses.

Elasticity

The percolation model, described above, elucidates also the changing of elasticity. At the percolation threshold the Young's modulus increases suddenly as a result of the interconnecting metallic clusters (see titanium in figure 6). Nevertheless for a given dose, important differences are observed between LEI and FCVA, as well as between gold and titanium. The low values of the Young's modulus measured on FCVA samples are explained by a partial deposition of the ions thanks to the energy spread from 50 eV to 10 keV. LEI, on the other hand, implants with a mono-energetic beam at 10 keV or 35 keV, rastering and heating the surface of PDMS for several hours. This is a big difference from the short pulsed implantation of a few minutes with FCVA; the influence of the energy on the chemical structure has been shortly summarized above. The Young's modulus for Au rises linearly with dose, contrarily to Ti, whose behavior can be explained with the percolation theory. This is probably due to the diffusion of gold.



Figure 6. Young's modulus of PDMS membranes after the implantation with Au and Ti. Membranes thickness is 25 μ m and the initial value of the Young's modulus is 0.85 MPa. Metal ion implantation has two main effects: formation of metallic clusters in the PDMS, and irradiation-induced chemical modification of the PDMS. A clear percolation threshold is seen for titanium, but not for gold.

CONCLUSIONS

FCVA implantation of gold is best suited for creating conductive electrodes in elastomers since it allows the lowest resistivity (300 Ω /square) to be reached at the smallest dose (1.75x10¹⁶ at/cm²) and hence with only limited stiffening of the membrane (5 MPa). This presents the best combination of high electrical conductivity and low compliance that are the main parameters for artificial muscle actuators and flexible electronics.

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