Acoustic Beamforming with Collaborating Hearing Aids

Olivier Roy and Martin Vetterli

Motivations

- Hearing aids are acoustic sensing devices (see Figure 1) that aim at compensating various hearing impairments:
- -Spectral shaping by means of frequency attenuation/amplification.
- -Beamforming by combining coherently signals acquired at multiple microphones.
- Most state-of-the-art systems involve two devices working independently of one another:
- -Limited beamforming capability.
- -Poor rejection of interfering signals.
- What is the need for collaboration between two hearing aids?
- -Uses the spatial extent offered by the head to provide better beamforming capability.

Distributed Source Coding

- Our setup is identified as a source coding problem with side information at the decoder (indirect, noisy or remote Wyner-Ziv [1]).
- The optimal rate-distortion tradeoff for stationary random sources can be computed as [2]:

$$R(\theta) = \frac{1}{4\pi} \int_{-\infty}^{\infty} \max\left\{0, \log_2 \frac{\Phi_e(\Omega)}{\theta}\right\} d\Omega \quad \text{[b/s]}$$
$$D(\theta) = \frac{1}{2\pi} \int_{-\infty}^{\infty} \Phi_{S_1|X_1, X_2}(\Omega) d\Omega + \frac{1}{2\pi} \int_{-\infty}^{\infty} \min\left\{\theta, \Phi_e(\Omega)\right\} d\Omega \quad \text{[MSE/s]}$$

where $\Phi_e = \Phi_{S_1|X_1} - \Phi_{S_1|X_1,X_2}$ and $\theta \in (0, \operatorname{ess\,sup}_\Omega \Phi_e(\Omega)]$. $\Phi_{X|Y}$ denotes the PSD of the error process X - E[X|Y].

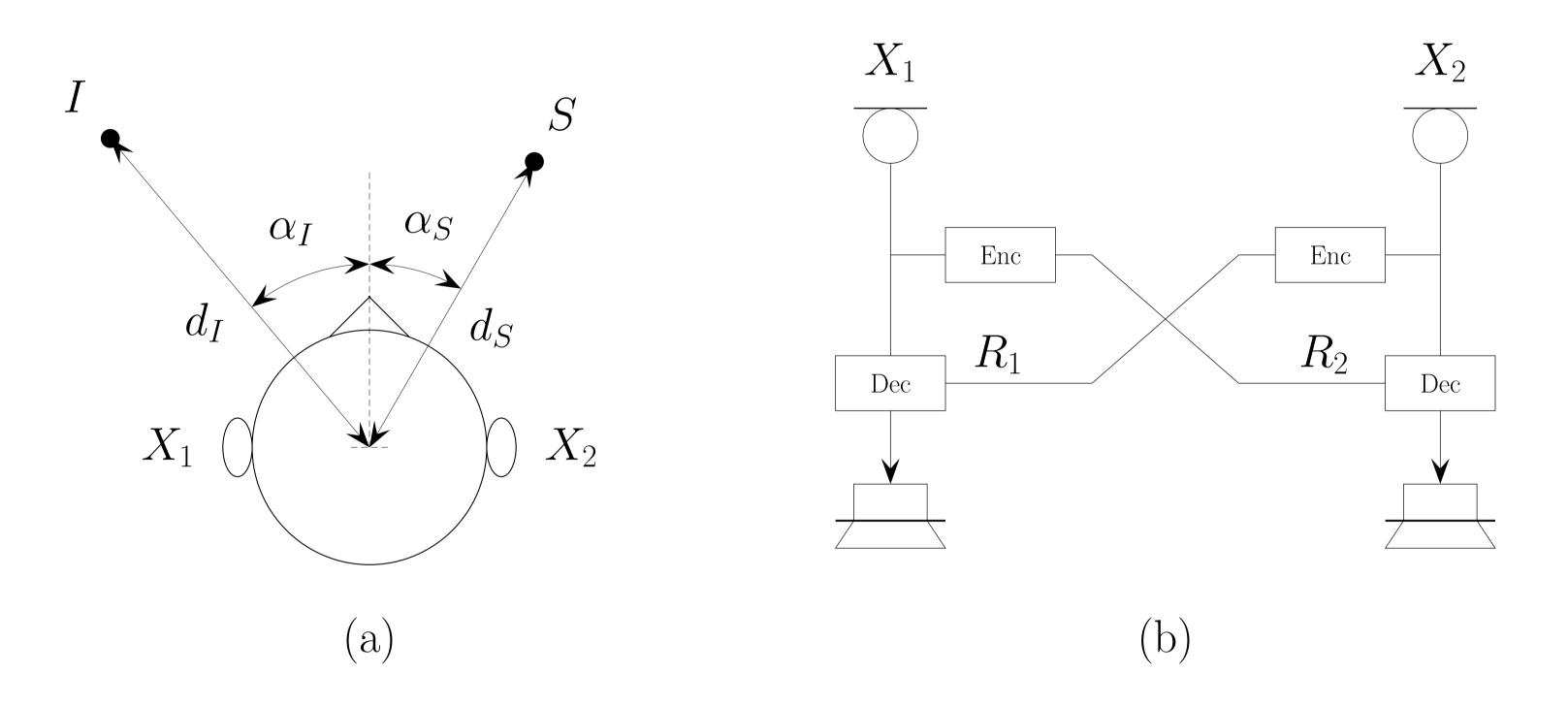
-Improves spatial noise reduction and increases speech intelligibility in noisy environments.



Fig. 1: Different types of hearing aids.

Problem Setup

• The auditory scene is composed of a desired source S, an interferer I and some ambient noise N [see Figure 2(a)].



• If the side information X_1 is disregarded in the encoding process, we obtain the following (suboptimal) rate-distortion tradeoff:

$$\tilde{R}(\theta) = \frac{1}{4\pi} \int_{-\infty}^{\infty} \max\left\{0, \log_2 \frac{\tilde{\Phi}_e(\Omega)}{\theta}\right\} d\Omega \quad [b/s]$$
$$\tilde{D}(\theta) = \frac{1}{2\pi} \int_{-\infty}^{\infty} \Phi_{S_1|X_2}(\Omega) d\Omega + \frac{1}{2\pi} \int_{-\infty}^{\infty} \min\left\{\theta, \tilde{\Phi}_e(\Omega)\right\} d\Omega$$
$$- \frac{1}{2\pi} \int_{-\infty}^{\infty} \Phi_{S_1}(\Omega) - \Phi_{S_1|V}(\Omega) d\Omega \quad [MSE/s]$$

where $\tilde{\Phi}_e = \Phi_{S_1} - \Phi_{S_1|X_2}$, $V = X_1 - \mathbb{E}[X_1|U]$ and $\theta \in (0, \operatorname{ess\,sup}_\Omega \tilde{\Phi}_e(\Omega)]$. The process U corresponds to the signal received at the decoder and can be described by an optimal forward test channel for the remote source coding problem.

Rate-Constrained Beamforming Gain

- We model the head as a sphere for which an analytical expression of the HRTFs can be computed [3].
- An example of gain-rate function in the absence of interferer is given in Figure 3(a). We observe the rate-loss incurred by neglecting the presence of side information.
- The normalized distortion obtained for a particular rate and frequency as a function of the interferer's position is plotted in Figure 3(b).

Fig. 2: Our hearing aids setup. (a) Typical head-related configuration. (b) Collaboration using a wireless communication link.

• The signal observed at hearing aid k (k = 1, 2) can be written as

 $X_k(t) = S_k(t) + I_k(t) + N_k(t)$ $= h_k(t) * S(t) + g_k(t) * I(t) + N_k(t).$

- S, I and N_k are independent jointly Gaussian stationary random processes with mean zero and bandlimited power spectral density (PSD) Φ_S , Φ_I and Φ_{N_k} , respectively.
- The filter h_k (resp. g_k) denotes the head-related impulse response (HRIR) from the source (resp. the interferer) to hearing aid k. Their Fourier transform is referred to as head-related transfer function (HRTF).
- The two hearing aids are allowed to collaborate using a wireless communication

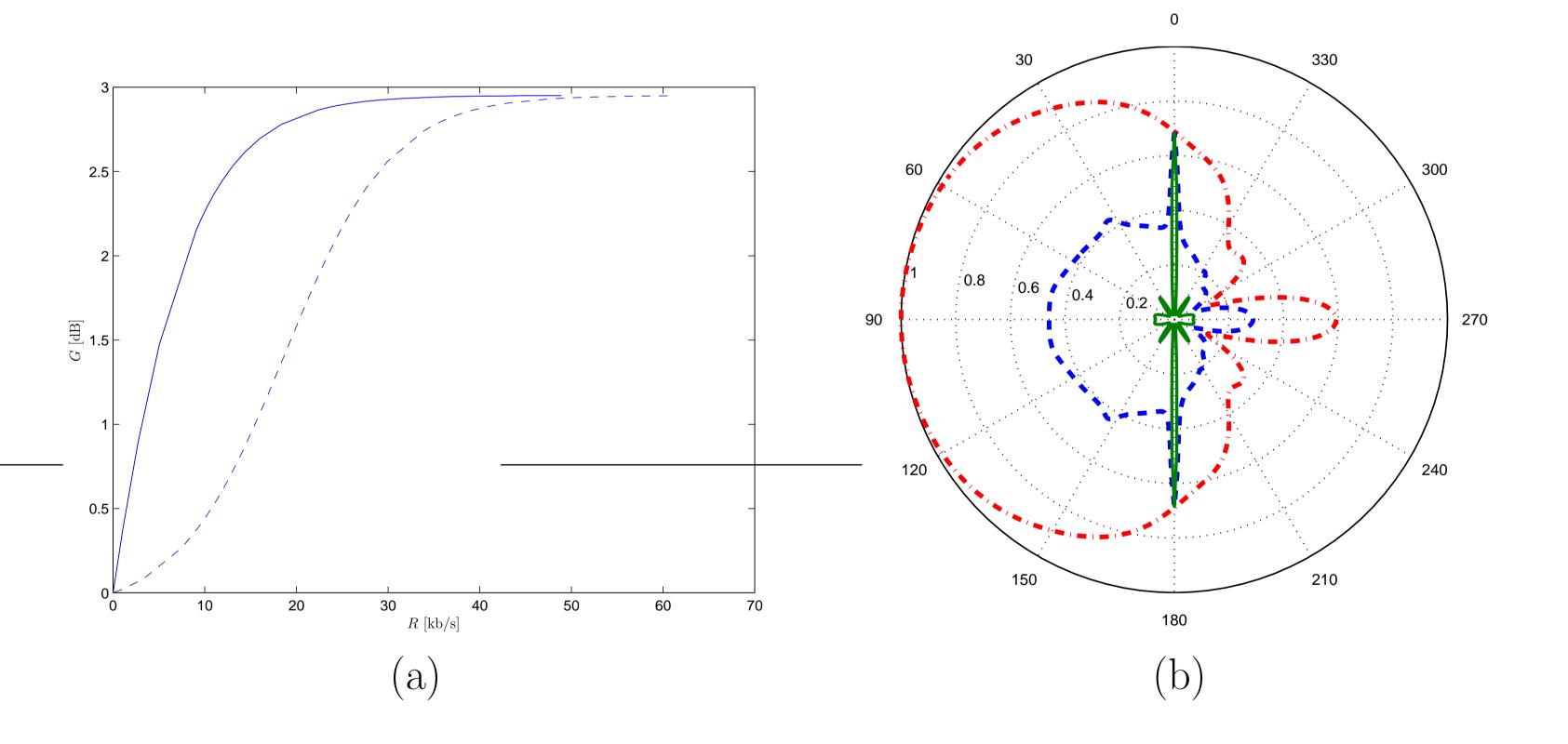


Fig. 3: Collaborative beamforming. (a) Gain-rate function with (plain) and without (dashed) Wyner-Ziv coding. (b) Normalized distortion for $f = \Omega/2\pi = 3000[Hz]$ and R = 0 (dash-dotted), R = 0.1 (dashed) and R = 1 (solid) [b/s/Hz].

References

[1] H. Yamamoto and K. Itoh, "Source coding theory for multiterminal communication systems with a remote source," Trans. IECE Japan, vol. E63, pp. 700–706, October 1980.

link [see Figure 2(b)]:

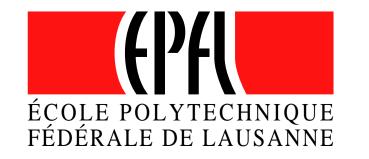
- -The problem is symmetric. We look at it from the perspective of hearing aid 1. -Hearing aid 2 relays its acquired signal to hearing aid 1.
- -We want to reconstruct S_1 with minimum mean-squared error (MMSE). • We define the *gain-rate* function

 $G(R) = \frac{D(0)}{D(R)}.$

• Goal: to characterize the optimal gain-rate tradeoff provided by this collaboration.

[2] O. Roy and M. Vetterli, "Rate-constrained beamforming for collaborating hearing" aids," accepted to IEEE International Symposium on Information Theory, 2006.

[3] R. O. Duda and W. L. Martens, "Range dependence of the response of a spherical head model," Journal of the Acoustical Society of America, vol. 5, pp. 3048– 3058, November 1998.



Audiovisual Communications Laboratory (LCAV), École Polytechnique Fédérale de Lausanne (EPFL), CH-1015 Lausanne email: {olivier.roy,martin.vetterli}@epfl.ch web: http://lcavwww.epfl.ch/~{oroy,vetterli}

