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Data in Brief

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5 6 7	ELSEVIER	journal home	page: www.elsevier.com/locate/dib		
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9 10	Data Article				
11 12 Q1	Parameterized hemodynamic response function				
13 14	data of healthy individuals obtained from				
15	resting-state functional MRI in a 7T MRI scanner				
16 17 18	D. Rangaprakash ^{a,b} , Guo-Rong Wu ^{c,d} , Daniele Marinazzo ^c , Xiaoping Hu ^e , Gopikrishna Deshpande ^{a,f,g,*}				
19 20 21 22					
23 Q2 24 25 Q3	⁶ Department of Bioengineering, University, Southwest Oniversity, Chongqing, China ⁶ Department of Psychology, Auburn University, Auburn, AL, USA ⁸ Alabama Advanced Imaging Consortium, Auburn University and University of Alabama Birmingham, AL, USA				
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27 28	ARTICLE INFO ABSTRACT				
29 30 31	Article history: Received 13 February 2				
32	Received in revised form 22 December 2017		of the unmeasured latent neural signal and the hemodynamic response function (HRF). The HRF is known to vary across the brain		
33 34	Accepted 2 January 201	8	and across individuals, and it is modulated by neural factors. Three parameters characterize the		
35 36			which is obtained by performing deconvolution data: response height, time-to-peak and full-wi	on resting-state fMRI	
37 38			data provided here, obtained from 47 healthy a three HRF parameters at every voxel in the b	dults, contains these	
39			parameters from the default-mode network (DI	MN). In addition, we	
40 41			have provided functional connectivity (FC) data regions, obtained for two cases: data with	deconvolution (HRF	
42 43			variability minimized) and data with no decon bility corrupted). This would enable researchers	to compare regional	
44			changes in HRF with corresponding FC differ- impact of HRF variability on FC. Importantly, the		
45 46			a 7T MRI scanner. While most fMRI studies are field strengths, like 3T, ours is the first study		
47			neta strengths, nee 51, outs is the first study		
48 49	* Corresponding author at: AU MRI Research Center, Department of Electrical and Computer Engineering, Auburn University,				
50 51	Auburn, AL, USA. <i>E-mail address:</i> gopi@auburn.edu (G. Deshpande).				
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53 54	2352-3409/© 2018 The Authors. Published by Elsevier Inc. This is an open access article under the CC BY license (http://creativecommons.org/licenses/by/4.0/).				

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obtained at 7T. FMRI data at ultra-high fields contains larger con- tributions from small vessels, consequently HRF variability is lower for small vessels at higher field strengths. This implies that findings made from this data would be more conservative than from data acquired at lower fields, such as 3T. Results obtained with this data and further interpretations are available in our recent research study (Rangaprakash et al., in press) [1]. This is a valuable dataset for studying HRF variability in conjunction with FC, and for developing the HRF profile in healthy individuals, which would have direct implications for fMRI data analysis, especially resting-state con- nectivity modeling. This is the first public HRF data at 7T. © 2018 The Authors. Published by Elsevier Inc. This is an open access article under the CC BY license (http://creativecommons.org/licenses/by/4.0/).				
Specifications Table				
Brain imaging Functional magnetic resonance imaging, hemodynamic response variability, hemodynamic response function parameters, ultra-high field MRI, 7T MRI scanner Image: brain maps of HRF parameters for every participant Siemens Magnetom 7T MRI Scanner (Siemens Healthcare, Erlangen, Germany) NifTi (.nii) and Matlab matrix (.mat)				
Our data consisted of a single population of healthy adults from the general society Resting-state: participants kept their eyes open and fixated on a white cross, which was displayed on a dark background, using an Avotec projection system. They were instr- ucted to not dwell on specific thoughts. Each resting-state scan lasted for 11 minutes.				
Auburn, AL, United States of America (GPS coordinates: 32.586, -85.494)				
Data accessibility Data has been made available with this article. Value of the data				
 This dataset provides a characterization of the variability of hemodynamic response function (HRF) across the brain, and across individuals, which is a confounding negative factor in functional magnetic resonance imaging (fMRI) data [2], especially connectivity modeling [3]. This dataset, which also includes comparable functional connectivity (FC) data, is valuable for studying the impact of HRF variability on varieties of fMRI data analysis, including, but not limited to, resting-state FC modeling. This dataset characterizes voxel-level HRF variability, hence it could be utilized to develop a generalized whole-brain voxel-level HRF template, with applications in fMRI data analysis. This is the first study to present HRF data obtained in a 7T MRI scanner. With less noisy HRF estimates, findings from this dataset would be more conservative than that acquired at lower fields, such as 3T. 				
 Data The dataset presented here contains three parameters that characterize the shape of the [3] – response height, time-to-peak and full-width at half-maximum. In the first part of 				

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dataset, each parameter is available at every voxel of the entire brain for every participant, which
is provided as 3D NifTi images (*.nii). One image file per parameter per participant is provided. In
the second part of the dataset, each HRF parameter is available for the default-mode network
(DMN) regions defined by the Power et al. atlas [5], along with corresponding FC for the same
regions, thus enabling researchers to compare the two, like in our recent research study [1].

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116 **2. Experimental design, materials and methods**

118 2.1. Participants

120 Forty-seven healthy adults participated in the study. Resting-state fMRI data was obtained in a 7T MAGNETOM scanner (Siemens Healthcare, Erlangen, Germany) using T2* weighted multiband 121 122 echo-planar imaging (EPI) sequence [6]. The advantage of data acquisition at 7T is that within-subject 123 HRF variability is likely lower at 7T compared to 3T (thus less noisy), because of larger contributions 124 from smaller vessels [4]. Participants were instructed to have their eyes open, and not contemplate on 125 any specific thoughts. FMRI acquisition parameters were as follows: repetition time (TR) = 1000 ms, 126 echo time (TE)=20 ms, flip angle=70°, multiband factor=2, voxel size= $2\times2\times2.4$ mm³, acquisition 127 matrix=96×96, number of slices=45, and number of fMRI volumes=660 (11 min), with whole-brain 128 coverage. A 32-channel head coil was used. All participants provided informed consent; all proce-129 dures were approved by the Auburn University Institutional Review Board (IRB).

131 2.2. FMRI data pre-processing

133 The following standard pre-processing steps were performed on the resting-state fMRI data: slicetiming correction (since the data was acquired using a multiband sequence), realignment and 134 135 unwrapping, coregistering to the anatomical image, de-spiking, normalization to the MNI space, 136 spatial smoothing (8 mm Gaussian kernel), and regressing out nuisance covariates (six head-motion 137 parameters, Legendre polynomials of up to second order, top five principle components from parti-138 cipant-specific white matter (WM) signal and cerebrospinal fluid (CSF) signal). Finally, temporal 139 band-pass filtering was performed (0.008-0.1 Hz). Pre-processing was carried out in the Matlab© 140 R2013a platform using Statistical Parametric Mapping (SPM12) [7].

142 *2.3. Obtaining the HRF parameters*

144 The voxel-wise 3D + time fMRI data was utilized to perform temporal hemodynamic deconvolution. 145 Latent neural time series and corresponding HRF parameters were obtained at every voxel through this 146 process. For deconvolution, we used a popular technique developed by Wu et al. [8]. The technique has 147 gained increasing popularity and acceptance due to its interpretability, robustness, validity, simplicity of 148 implementation, and an awareness within the research community regarding the need for deconvo-149 lution. Several recent studies have utilized it (see for example [9–18]). Hemodynamic deconvolution is 150 blind because only one variable is accessible (fMRI time series), from which both the latent neural time 151 series and the HRF are estimated. In simple terms, the technique models resting-state fMRI as event-152 related time series, with randomly occurring events modeled as point processes [19,20], using which 153 the voxel-wise HRFs are estimated through Wiener deconvolution. The deconvolution code, on the 154 Matlab© platform, is available for download at [21]. A user-interface-based deconvolution toolbox 155 would be released separately in the near future.

Deconvolution provided the estimated HRF at every voxel of the brain, in every participant. It was characterized by three HRF parameters, as noted earlier – response height (RH), time-to-peak (TTP), and full-width at half-max (FWHM) (see Fig. 1 in [3]). The data being made available with this article are these voxel-wise HRF parameters for all the participants. All data analysis was performed on the Matlab® platform.

161 In addition, we have also provided these three HRF parameters obtained from the DMN, along 162 with the functional connectivity (FC) between corresponding regions. The DMN regions-of-interest

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163 (ROIs) were obtained as 10-mm diameter spheres around the DMN centroids as defined in Power et 164 al. [5] (template available with the data). Mean time series were first obtained from the 58 DMN ROIs, 165 and deconvolution was performed on them to obtained latent neural time series and HRF parameters. 166 FC was obtained for all pairwise connections using Pearson's correlation [22,23]. Our recent research 167 study, using this HRF and FC data [1], assessed the impact of HRF variability on FC, and concluded that 168 HRF variability confounds FC analysis. The implications of those findings are widespread, since most 169 of the resting-state fMRI FC studies (1200+ articles published each year and increasing exponentially) 170 do not perform deconvolution and do not account for HRF variability. This data can be utilized by 171 researchers to compare change in HRF parameters with the corresponding change in FC, using which 172 they could replicate our findings, as well as perform follow-up research and make new discoveries. 173 Our main findings associated with this dataset, along with further interpretations, are part of our 174 recent research study [1].

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Appendix A. Supporting information

Supplementary data associated with this article can be found in the online version at https://doi. org/10.1016/j.dib.2018.01.003.

189 Transparency document. Supporting information 190

191 **05** Transparency data associated with this article can be found in the online version at https://doi.org/ 10.1016/j.dib.2018.01.003.

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