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Xiao, Sanshui ; Mortensen, N. Asger

Published in:
European Optical Society. Journal. Rapid Publications

Link to article, DOI:
[10.2971/jeos.2006.06026](https://doi.org/10.2971/jeos.2006.06026)

Publication date:
2006

Document Version
Publisher's PDF, also known as Version of record

[Link back to DTU Orbit](#)

Citation (APA):
Xiao, S., & Mortensen, N. A. (2006). Highly dispersive photonic band-gap-edge optofluidic biosensors. European Optical Society. Journal. Rapid Publications, 1(06026). DOI: 10.2971/jeos.2006.06026

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Highly dispersive photonic band-gap-edge optofluidic biosensors

Sanshui Xiao
sanshui.xiao@mic.dtu.dk

MIC – Department of Micro and Nanotechnology, NanoDTU, Technical University of Denmark, DK-2800 Kongens Lyngby, Denmark

Niels Asger Mortensen

MIC – Department of Micro and Nanotechnology, NanoDTU, Technical University of Denmark, DK-2800 Kongens Lyngby, Denmark

Highly dispersive photonic band-gap-edge optofluidic biosensors are studied theoretically. We demonstrate that these structures are strongly sensitive to the refractive index of the liquid, which is used to tune dispersion of the photonic crystal. The upper frequency band-gap edge shifts about 1.8 nm for $\delta n = 0.002$, which is quite sensitive. Results from transmission spectra agree well with those obtained from the band structure theory. [DOI: 10.2971/jeos.2006.06026]

Keywords: Biosensor, photonic crystal, optofluidics

1 Introduction

Photonic crystals (PhCs) are attractive optical materials for controlling and manipulating the flow of light [1]–[3]. One well-know property is the existence of photonic band gaps, i.e., regions of frequencies where electromagnetic wave propagation is prohibited. Another equally important aspect of a PhC is the existence of an unconventional ultra-strong dispersion. Such an ultra-strong dispersion was firstly reported by Lin *et al.* and demonstrated experimentally in the millimeter-wave spectrum [4]. Kosaka *et al.* subsequently demonstrated the superprism effect in a highly dispersive photonic microstructure [5]. These unusual properties provide an exciting possibility for obtaining microphotonic and nanophotonic devices that can focus, disperse, switch, and steer light.

Optofluidics, the marriage of nano-photonics and microfluidics, refers to a class of optical systems that integrate optical and fluidic devices [6]. Due to unique properties of fluids, such integration provides a new way for dynamic manipulation of optical properties and shows many potential applications [7]–[14]. In particular, PhCs are interesting for optofluidics since they naturally have voids where fluids can be injected. Optical properties of the PhC can be easily re-configured by selectively filling specific voids with liquid. Chow *et al.* demonstrated an ultra compact biosensor employing a two-dimensional (2D) photonic crystal microcavity [15]. Recently, we proposed simple biosensor structures based on highly dispersive PhC waveguides [16]. In this paper we will propose biosensor structures based on complete PhCs and the strong dispersion occurring near the Brillouin zone. In particular, the bandgap edges of the PhCs are strongly sensitive to the refractive index of the liquid which is used to tune the dispersion of the PhC. The suggested structures show a potential for biochemical sensing applications.

2 BIOSENSOR STRUCTURES AND RESULTS

Let us first consider a 2D triangular PhC with air holes extending through a high index $\epsilon = 10.5$ dielectric material, shown in the inset of Figure 1.

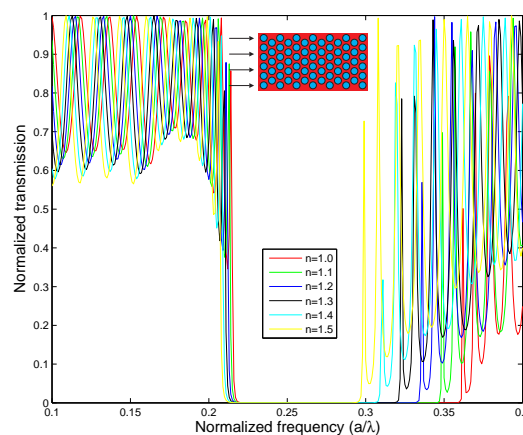


FIG. 1 Transmission spectra for the light normally incident into a triangular PhC, see inset, with air holes being filled by different liquids with refractive indices varying from $n=1.0$ to 1.5 in steps of 0.1 . The PhC is a triangular lattice with holes extending through a high-index $\epsilon = 10.5$ dielectric slab and the radius of holes is $0.36a$, where a is the lattice constant.

The holes have a radius of $0.36a$, where a is the lattice constant. Here, we will focus our study on transmission spectra of the PhC with air holes being filled with different liquids. It was shown in our previous work that both the surface termination and surface direction of the PhC are critical for high transmission (i.e., coupling) at an interface between air and

the PhC [17, 18]. Consider the TE-polarized (magnetic field parallel to the air holes) light normally incident into the PhC. To enhance the coupling at the interface, we choose to couple light to the PhC along the ΓM direction, i.e., the surface of the PhC slab is along ΓK direction. The symmetric PhC slab is composed of 11 layers along the ΓM direction and the distance (surface termination) between right boundary and the centers of the first right holes is $0.5a$. Transmission spectra for the PhC are obtained using the 2D finite-difference time-domain (FDTD) method [19]. For this case, we use the periodic condition in ΓK direction and perfectly matched layers in the ΓM direction [20] as the numerical boundary treatment. Figure 1 shows transmission spectra for the PhC with air holes being filled by different liquids with the refractive index increasing from $n = 1.0$ to $n = 1.5$ in steps of $\delta n = 0.1$. One can see clearly that there exist band gaps for the PhCs. Transmissions outside the band gaps are quite large and close to unity for some frequencies. Peaks in the transmissions arise from the Fabry–Perot oscillations from the two boundaries and the shifts of peaks are due to the change of the effective index of the PhC when filling air holes with different liquids.

For the present application we are not interested in the details of the Fabry–Perot pattern in Figure 1, but rather the spectral position of the band-gap edge which is a highly sensitive measure for changes in the refractive index of the liquid. To see it more clearly, the change of the band-gap edge as a function of the refractive index of the liquid is shown in Figure 2.

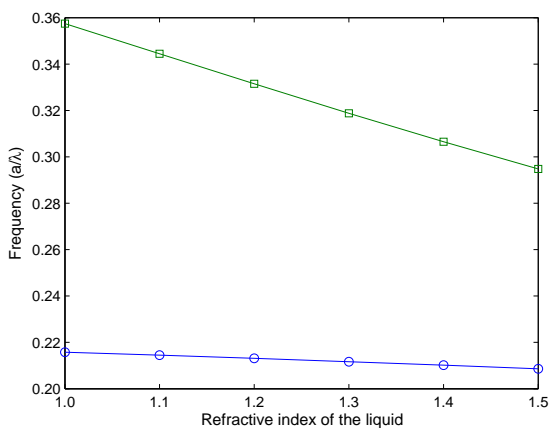


FIG. 2 Band-gap edges as a function of the refractive index for the filled liquid.

As seen, the low-frequency mode-gap edges slightly change with the refractive index of the liquid. However, the high-frequency mode-gap edge is strongly dependent on the refractive index of the liquid, as shown by squares in Figure 2. As an example, the high-frequency band-gap edge shifts $\delta(a/\lambda) = 0.012987$ when the air holes (with index $n = 1$) are filled by a liquid of index $n = 1.1$. For comparison, it is only $\delta(a/\lambda) = 0.001278$ for the low-frequency band-gap shift. Now, consider a commercial silicone fluid with a calibrated refractive-index accuracy of $\delta n = 0.002$, as mentioned in Ref. [15], where the refractive index of the liquid varies from $n = 1.446$ to 1.454 in increments of 0.002 . For the working wavelength around $1.55\mu\text{m}$ (here we choose $a = 450\text{nm}$), the high-frequency band-gap edge shifts up to 1.17 nm for $\delta n = 0.002$, while 0.33 nm

for the low-frequency band-gap edge. For comparison, we note that the shift in resonant wavelength for the high-quality-factor PhC cavity is about 0.4 nm for $\delta n = 0.002$ [15]. The above results demonstrate that even such a simple PhC has potential applications as a sensitive biosensor.

To further elucidate the physics behind the strong sensitivity, we next support the picture by dispersion calculations for the PhC. For this purpose we use a Block-iterative frequency-domain method [21]. The dispersion of the PhC, in absence or presence of a fluid, is shown in Figure 3.

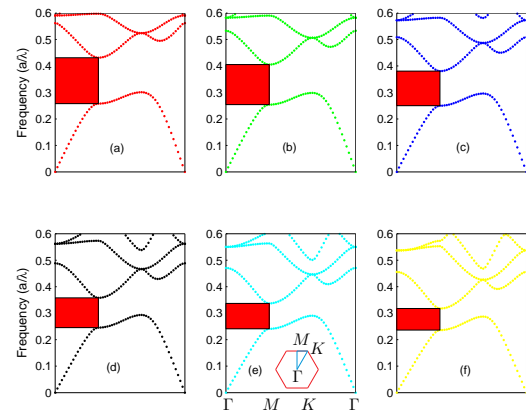


FIG. 3 Dispersion of the triangular photonic crystal shown in the inset of Figure 1a, where the air holes are filled by liquids with refractive indices varying from $n=1.0$ to 1.5 in steps of $\delta n = 0.1$. The red regions denote the bandgap regions along ΓM direction.

Figure 3a–f summarize the dispersions for the PhC, where the air holes are filled by a liquid with a varying refractive index. One can clearly see that these PhCs have photonic band gaps for the TE polarization, which are related to the band gaps in Figure 1, though the band-gap regions appear slightly different with those obtained from the transmission spectra. Note that the band gaps in Figure 1 are larger than those in Figure 3. This is because the band gaps in Figure 3 are for all incident directions while the band gaps in Figure 1 are only for propagation along the normal direction. From Figures 1 and 3, we also observe that the position of the gap in the transmission spectra, which are obtained for plane electromagnetic waves incident normally on the PhC, agree very well with the position of the gaps in the frequency band structure of the corresponding infinite crystal along the ΓM direction (denoted by red regions). When increasing the refractive index of the liquid [going from panel (a) toward panel (f)], the high-frequency band-gap edge is significantly downward shifted, while the low-frequency band-gap edge slightly decreases. We emphasize that all results obtained from band structures are consistent with those from the transmission spectra. The sensitivity of this structure is mainly attributed to the strong dispersion of the PhC mode. Figures 4a and 4b show the first and second PhC Bloch modes at the band-gap edge (M point, $k = \pi/a$), where air holes in the PhC are filled by the liquid with a refractive index of $n = 1.0, 1.5$, and 2.0 , respectively.

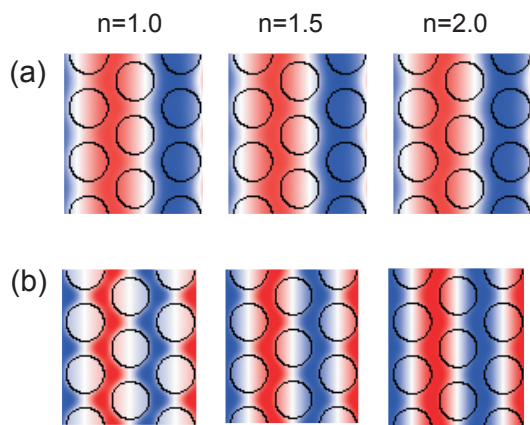


FIG. 4 Bloch mode at the band edge (M point, $k = \pi/a$) for the (a) first band (b) second band, in which air holes in the PhC are filled by the liquid with a refractive index of $n = 1.0, 1.5,$ and 2.0 , respectively.

As seen, the low-frequency band-edge Bloch mode hardly changes with varying refractive index of the liquid. However, for the high-frequency band-edge mode, the ratio of the energy in holes becomes larger as the refractive index of the liquid increases, i.e., this mode distribution is strongly dependent on the refractive index of the liquid, which is in agreement with the results in Figures 1–3. A somewhat similar structure has been realized experimentally by Okamoto *et al.* [22], but in this paper we have studied the shift for the band-gap edges in details and offered a physical explanation for the shifts. Besides, compared to the device in Ref. [22], our proposed device offers a better resolution.

Let us next consider a square PhC with dielectric rods in air, as shown in the inset of Figure 5.

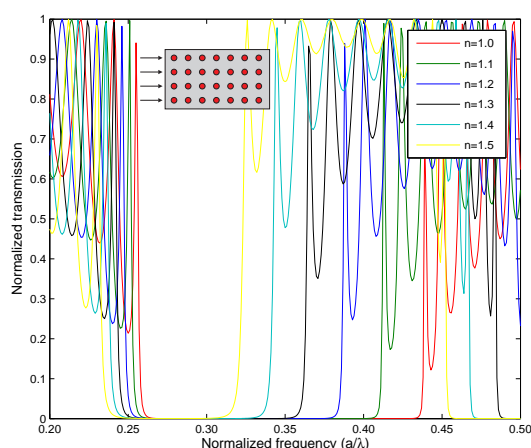


FIG. 5 Transmission spectra for the light normally incident into a square PhC, see inset, with the background being filled by different liquids with refractive indices varying from $n=1.0$ to 1.5 in steps of 0.1 . The PhC is a square lattice with dielectric rods in air. The rods have a refractive index of $\epsilon = 10.5$ and the radius of $0.2a$.

The permittivity of the rods is $\epsilon = 10.5$, and the radius of the rods is $r=0.2a$. Transmission spectra for TM polarization are shown in Figure 5, where the background of the PhC is filled

by different liquids. The band-gap edge as a function of the refractive index of the liquid is shown in Figure 6.

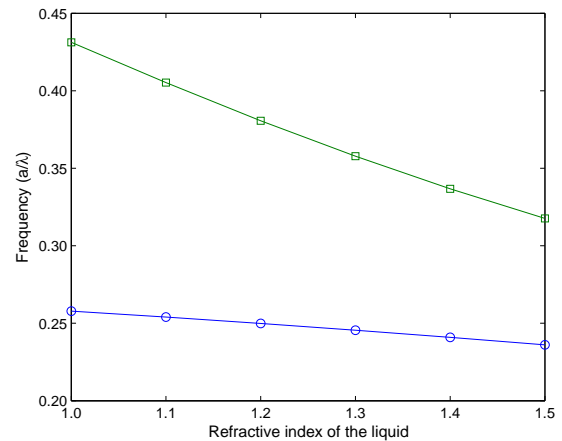


FIG. 6 Band-gap edges as a function of the refractive index for the filled liquid.

Similar to the result shown in Figure 2, the low-frequency band-gap edge hardly changes as the refractive index of the liquid increases, while the high-frequency band-gap edge is strongly dependent on the liquid. Compared with the result for the high-frequency band-gap edge shown in Figure 2, the results in Figure 6 illustrate a higher sensitivity. The high-frequency band-gap edge shifts $\delta(a/\lambda) = 0.025939$ when the air holes are filled by a liquid of index $n = 1.1$. For comparison we have $\delta(a/\lambda) = 0.012987$ for the structure shown in the inset of Figure 1.

Band structures are shown in Figure 7, where red regions represent the band gap for ΓX direction.

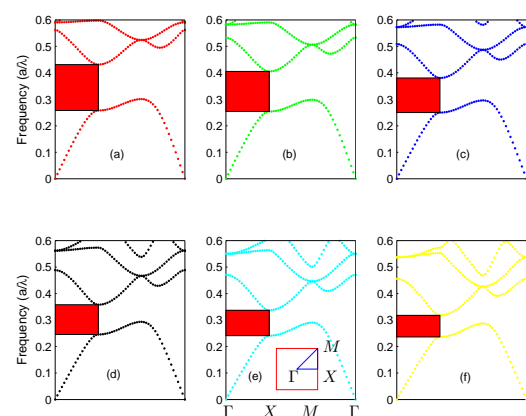


FIG. 7 Dispersion of the square photonic crystal shown in the inset of Figure 5a, where the background is filled by liquids with refractive indices varying from $n=1.0$ to 1.5 in steps of $\delta n = 0.1$. The red regions denote the bandgap regions along ΓX direction.

From Figure 5 and Figure 7, we find that the position of the gap in the transmission spectra agree very well with the position of the gaps for the PhC along the ΓM direction. When increasing the refractive index of the liquid [going from panel

(a) toward panel (f)], the high-frequency band-gap edge is significantly downward shifted, while the low-frequency band-gap edge slightly decreases. Again we consider a commercial silicone fluid with a calibrated refractive-index accuracy of $\delta n = 0.002$. For the working wavelength around $1.55\mu\text{m}$ ($a = 450\text{nm}$), the mode-gap edge shifts up to 1.60 nm for $\delta n = 0.002$. The proposed biosensor relies strongly on the dispersion of the PhC band-edge mode and the presence of a band gap. To further improve the sensitivity, we optimize the PhC structure by varying the radius of the rods. By a careful design of the structure shown in the inset of Figure 5, we have been able to improve the design further. For the working wavelength around $1.55\mu\text{m}$ ($a = 450\text{nm}$), the band-gap edge shifts about 1.8 nm for $\delta n = 0.002$, when r is tuned to $0.1a$. Compared to the biosensor we proposed before [16], this structure not only shows much better sensitivity but it also seems relatively easy to realize experimentally, since the design involves no cavities or waveguide structures. Finally, this device, with a size of $5\mu\text{m} \times 5\mu\text{m}$, is sufficiently compact for most applications.

3 CONCLUSIONS

To conclude, we have theoretically studied optofluidic biosensors based on highly dispersive 2D photonic crystal. Our study shows that these structures are strongly sensitive to the refractive index of the liquid, which is used to tune dispersion of photonic crystal. For the working wavelength around $1.55\mu\text{m}$, we predict shifts in the band-gap edge up to 1.8 nm for $\delta n = 0.002$. Although our study is based on 2D photonic crystals, it can be extended to the case of a 2D photonic crystal slab. For a 2D photonic crystal slab, the field will attenuate due to out-of-plane loss, but the shift of the high-frequency mode-gap edge at X/M point (when tuning by liquid) is unaffected by the out-of-plane radiation. The high sensitivity makes such devices interesting for biochemical sensing applications.

ACKNOWLEDGMENTS

This work is financially supported by the *Danish Council for Strategic Research* through the *Strategic Program for Young Researchers* (grant no: 2117-05-0037).

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