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The influence of endogenous surfactant on the structure and drug-release properties of Eudragit NE30D-matrices

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The influence of an endogenous surfactant present in Eudragit NE30D on the structure and drug release (clenbuterol) properties of thin matrices has been examined. Both drug-free and drug-loaded matrices were found to be non-isotropic in structure, the former having a marbled appearance under the polarising light microscope, and the latter showing numerous needle-shaped crystals. At loading above approx. 10% w/w clenbuterol it was also possible to observe aggregates of the drug. Differential scanning calorimetry enabled the identification of melting peaks at approx. 50°C for the needle-shaped crystals and approx. 80°C for the larger drug aggregates. The former are **composed** of a surfactant used by the manufacturer for the synthesis of Eudragit NE3OD by emulsion polymerization. This surfactant undergoes a phase separation from the polymer oo storage at room temperature. It could, however, be extracted from the polymer hy refluxing in water to yield an isotropic system. The extract showed a melting peak at SO'C and also UV, IR, NMR, **and mass** spectra in accordance with an o-substituted nonyl phenol surfactant. Matrices prepared from the purified Eudragit NE30D showed drug release rates of only one third the magnitude of those found with matrices prepared from the raw polymer. Substantially reduced scatter in the release data was also found with the purified polymer.

Key words: Polyacrylate polymer: Surfactant; Diffusion

Introduction

We have been interested for some time in the use of Eudragit NE30D as a carrier for the sustained release of drugs. Matrix-type carriers can easily be prepared from thin films of the polymer cast by solvent evaporation [1]. The rate of release of the drug clenbuterol from such matrices has heen examined using a simple diffusion cell [2]. The accurate evaluation of the kinetic data so obtained requires, however, knowledge of the mechanism of drug release from the polymer. Of elemental importance in this respect is tbe physical state of the drug within the polymer matrix, as the release kinetics depend inter alia on whether the drug exists in the dissolved or suspended condition [3]. We deemed it expedient, **therefore, to** determine the solubility of the cleobuterol in the Eudragit NE30D. To that end an examination of drug-loaded polymer matrices was undertaken using polarising light microscopy. We were surprised to observe that the matrices were strikingly anisotropic in structure, showing either a marbled appearance or the presence of variously-shaped crystals and fractal aggregates. Indeed, it was not possible to distin-

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guish unequivocally between drug crystals and the other structures observed. We found little information in the literature concerning the structure of Eudragit NE30D. despite its use to produce matrix tablets as a drug carrier [4]. Only two differential scanning calorimetric studies of Eudragit NE30D [51 and the related Eudragit 7972-55 PMMA ON [6] have been published. neither of which offered a satisfactory explanation of our observations.

It soon became clear from further experiment that the puzzling microscopical appearance of the matrices was a result of the presence of small amounts of a water-soluble contaminant within the Eudragit NE30D. This is almost certainly a surfactant used by the manufacturer for the synthesis of the polymer by emulsion polymerization [7a]. It was possible to remove this endogenous contaminant from the polymer by extraction with water to yield an isotropic system. We present in this paper our findings concerning the effects of the endogenous surfactant on the physical state of clenbuterol within the Eudragit NE30D-matrices and the consequences for drug release rate which ensue from its removal.

Materials and Methods

Materials

The basic drug clenbuteroi of molecular weight 277 and pKa $\frac{5}{10}$ was used as received from Boehringer Ingelheim. KG (Ingelheim. Ingelheim Germany):

Eudragit NE30D (Röhm, Weiterstadt, Germany) is a neutral, poly(ethylacrylate-methylmethacrylate) copolymer with a molecular weight of approx. 800,000, and which exists in the rubbery state at room temperature (glass transition at -8 ^{\degree C):}

CH3 ..-CH,-CH-CH,-ti-... LO &IF dCH>

Although insoluble at all pHs, it swells in water. It was obtained as a 30% aqueous dispersion and freeze dried at -25° C to vield a white solid. All solvents and buffer salts were pA grade. Water was double-distilled from an all-glass apparatus.

Experimental methods

Preparation of Eudragit NE30D-matrices

Films of 50 μ m thickness containing various concentrations of clenbuterol in the range O-20% w/w were prepared on a siliconized paper base by the casting of a 15% w/w acetone sulution of the raw polymer. The product was dried at room temoerature for 12 h. after which less than 50 ppm acetone remained as determined by gas chromatography. Round matrices (\varnothing 2 cm) were then cut from the film using a punch.

According to the manufacturer, Eudragit NE3QD contains traces of a water soluble, neutral surfactant of the nonyl-phenol-type I7bl. We attempted to extract the surfactant from Eudragit NE30D by refluxing the freeze-dried polymer in a Soxlct for 90 h with water. The resulting purified polymer was a white solid. The dried extract took the form of a yellowish-white, crystalline solid, which was found to represent approx. 3.3% of the total mass of the dried raw oolvmer. Matrices of the purified Eudragit NE30D were then prepared as described above, also containing concentrations ofclenbuterol in the range O-20% w/w.

Polarising light microscopy

The matrices were examined at various times after their preparation using a Zeiss Standard microscope fitted with a polarizing objective and condenser, a hot stage for examining thermal behaviour, and a Nikon C35 camera. The extract and pure clcnbuterol were also examined.

Differential scanning calorimetry (DSC)

A Mettler model TC10A (Greifensee, Switzerland) was used to examine the matrices at various times after their preparation, as well as the extract and pure clenbuterol. A heating/cooling speed of IO **K/min was** selected.

UV , **IR and mass spectrophotometry; NMR** An attempt was made to confirm if the crystalline extract obtained from the raw polymer con-

tained a surfactant of the type declared by the manufacturer. To that end, UV (Zeiss DMR 21), IR (Beckman Aculab 6), and mass spectrophotometry were employed. 250 MHz-NMR spectra were also obtained in D,O. In all cases the solid extract was **firsi** recrystallized from methanol to remove any inorganic contaminants.

Measurement of drug release

The release of clenbuterol out of matrices prepared from both raw and purified Eudragit

Fig. 1. Photographs of 8-days' old matrices prepared from raw Eudragit NE30D viewed under crossed polarisers; (a) drug-free, **(b) 6% wlwdrug (clenhuteml) loading, (c) 12% drug loadmg. Cd) 20% drugloading.**

NE30D into pH_1 8 phosphate buffer was mea-
sured at $35^{\circ}C$ using an all-glass diffusion cell of calculated by fitting each release profile to a nusured at 35°C using an all-glass diffusion cell of calculated by fitting each release profile to a nu-
standard design [2]. The results were expressed merical solution to the diffusion equation under standard design $[2]$. The results were expressed merical solution to the diffusion equation under as release profiles of $m(t)/A$ versus time, where non-sink conditions, as described in detail elseas release profiles of $m(t)/A$ versus time, where non-sink conditions, as described in detail else-
 $m(t)$ is the mass of clenbuterol in the acceptor where [2]. Of relevance to this study is that the $m(t)$ is the mass of clenbuterol in the acceptor medium at time t and A is the release area. The

 $solution$ assumes the linear diffusion of drug with

Fig. 2. DSC-scans of clenbuterol-loaded, raw Eudragit NE30D matrices taken 1 and 32 days after their preparation. Key: day/ drug loading [%].

constant diffusivity. D, in a finite, isotropic, plane matrix with spontaneous partitioning at all boundaries. The initial condition used specifies the existence only of dissolved drug.

Results and Discussion

Structure of Eudragit NE30D-matrices

When viewed under the light microscope with crossed polarizers the raw Eudragit NE3OD-matrices reveal a complex structure that depends on time elapsed since preparation and drug-loading. A stable picture first emerges after 6-8 days' storage at room temperature. This is illustrated by the photographs taken of 8-days' old Eudragit NE30D-matrices having selected loadings of 0%, 6% , 12%, and 20% w/w clenbuterol (Fig. 1a-d, respectively). Thus, the two matrices of highest drug loading clearly show a population of large, irreguiarly-shaped crystals, some ofwhieh are not euclidian but rather of fractal shape. These were observed to melt when the temperature was raised to approx. SO-90°C. and certainly come from the incorporated drug, even though this melting point lies well below that of pure clenbuterol $(135^{\circ}$ C). Careful scrutinization of these two photographs also reveals the presence of a second type of much smaller, needle-shaped crystal, which melted at approx. 50° C. The matrix containing only 6% w/w clenbuteroi (Fig. lb) shows none of the large crystals or fractal forms, indicating that the drug is soluble in the polymer at this concentration. The needle-shaped crystals are, however, still clearly visible at this drug loading. Although they do not appear within the drug-free matrix (Fig. 1a), the polymer has a distinctly marbled appearance under crossed polarisers and is thus also anisotropic.

The DSC-scans for these matrices (Fig. 2) at 12% and 20% drug loading both develop on storage a slight endothermic transition at approx. 80°C. **This** coincides with the **melting** of the large crystals and fractal aggregates of **drug** within the polymer at this temperature, as could be observed directly under the microscope. Accordingly, this peak is not seen on the scans for matrix containing 6% clenbuterol, where tbe microscopy results indicate that the drug is fully dissolved, or the drug-free matrix. Witb ah the matrices **examined,** however, a clear endothermic peak is visible at approx. 50°C. For the drugfree matrix, this peak develops slowly on storage, first appearing clearly after 8 days. Simultaneousfy the marbled areas become noticeable within this matrix. All of the drug-containing matrices show a clear peak even after the first day's storage. The needle-shaped crystals can be observed to grow correspondingly. This endothermic peak is, therefore, clearly not caused purely by the existence of drug within the polymer, developing even for the drug-free matrix, albeit more slowly.

The existence of such an endothermic peak has already been noted in the literature [6] and assigned to a glass transition of the polymer at this temperature. Furthermore, there exists a proposal (5 1. also based on the results of DSC measurements, that crystalline structure exists within Eudragit NE3QD. It is not, however, possible to reconcile the results of our experiments with this earlier work. Thus, the DSC-scan for the drugfree matrix prepared from the purified Eudragit NE30D shows no signs 01 an endothermic transition at 50° C, even after storage at room temperature for 128 days (Fig. 3). The thermogram for the crystailine solid extracted from the Endragit NE3OD (Fig. 4). however, cieariy shows such a peak at 5O'C, corresponding to the melting point of thrs extract as observed under the light microscope. When a drug-free matrix prepared from the purified Eudragit NE30D is viewed under the light microscope an isotropic system is seen (Fig. 5a); the marbled areas observed within the raw polymer are not present and do not develop on storage. Furthermore, the matrix prepared from the purified Eudragit NE30D and containing 6% clenbuterol (Fig. Sb) shows neither drug nor needle-shaped crystals and its DSC-scan has no visible peaks (Fig. 3). With 12 and 20% drug loading the usual crystal and fractal forms of the drug can be observed un-

Fig 3. USC-scans of clmburorol-ioadcd, purified Eudragit NE30D matrices taken I and 32 days alter their preparation. Key: day/dmgiosding f%l.

der the microscope (Fig. 5c,d). but again none of the needle-shaped crystals. The DSC-scans show only the slight melting peaks for the drug crystals and aggregates at $80-90^{\circ}$ C and no endothermic transition at 5O'C (Fig. 3).

On the basis of these results it appears that the endothermic transition observed at approx. 50°C for the raw Eudragit NE30D arises from the phase separation of some water-soluble, endogenous substance within the polymer. At this point we must bear in mind the manufacturer's declaration that Eudragit **NE300** contains traces of a water-soluble, o-substituted nonyl-phenol surfactant having a molecular weight of 5000-6000 [7b]. The spectroscopic data we obtained from the extract provides evidence to suggest that the extract contains such a surfactant. Thus, the strong UV-absorbance of the extract at 247 nm

Fig. 4. DSC-scan of crystalline solid extracted from raw Eudragit NE30D.

(Fig. 6a) indicates a substituted aromatic structure. The band seen in the IR spectrum (Fig. 6b) at 2900 cm-' comes from C-H vibrations, whilst that at 830 cm^{-1} can be assigned to out-of-plane vibrations of an o-substituted aromatic. Furthermore, the large band at 1100 cm⁻¹ indicates a large content of C-O groups, as would arise from a high degree of ethoxylation of the molecule. The three major peaks of the mass spectrum (Fig. 6c) occur at 45 m/e. 89 m/e and 133 m/e. the difference between each being always 44 units. This finding can be explained if etboxy chains arc broken up into units of $[-CH₂-O-C₂H₂-]$. The NMR spectrum (Fig. 6d) can be used to estimate the ratio between aromatic protons (peaks at 6.8 and 7.2 ppm) and protons originating from the supposed ethoxy groups (peak at 3.7 ppm). A value of approx. 100-150 ethoxy units is obtained. Although these spectra are not sufficient per se to allow an unequivocal identification of the substance, it seems very probable. Any incompatibility of this substance with the polyacrylate - by virtue of the former's hydrophilicity - would lead to a phase separation from the polymer on storage. In a drug-free matrix this results in the marbled appearance of the polymer illustrated in Fig. la. The presence **of drug** within the matrix evidently causes the surfactant to crystallize out rapidly as needle-shaped crystals (cf. Fig. lb).

Drug release from Eudragit NE30D-matrices

The **extraction** of the endogenous contaminant from Eudragit NE30D affects the rate of release of clenbuterol from the matrices. Fig. 7a iilustrates **for the** example of 8% drug-loading how the release profiles for the matrices prepared from the purified Eudragit NESOD are much lower tban those for the matrices prepared from the raw

Fig. 5. Photographs of 8-days' old matrices prepared from purified Eudragit NE30D viewed under crossed polarisers; (a) drug**free, (b) 6%w/wdrug tclenbutcrol) loading, (c) 12%drugloading, (d) 2O%dmgloadmg.**

Eudragit NE30D (latter taken from ref. 2). The diffusivities calculated from the individual profiles are concentration-dependent for both raw and purified Eudragit NE30D-matrices (Fig. 7b). Increasing diffusivity with greater drug loading has already been observed for the nonextracted polymer [**I,2].** The subsequent dccrease observed here at high drug loading is readily explained by the influence of the presence of substantial amounts of suspended drug within the polymer. For the calculation of diffusivity from the release profile, the concentration of drug in the matrix must be specified [2], all of which is assumed to exist in the dissolved state. **In the presence of** suspended drug, this value will be overestimated and cause an underestimation in the calculated diffusivity.

Fig. 7b also illustrates that the diffusivities for the purified Eudragit NE30D-matrices are about I/3 of the magnitude of those for the raw Eudragit NESOD-matrices (latter also taken from ref. 2). The degree of scatter in the diffusivities ob-

Wavenumber $[cm^{-1}]$

Fig. 6. Spectra obtained from the extract; (a) UV-spectrum, (b) IR-spectrum, (c) mass-spectrum, (d) NMR-spectrum,

Fig. 7. (a) Drug release profiles for elenbuterol from raw and purified Eudragit NE30D matrices with 8% w/w drug loading; (b) calculated diffusivities for clenbuterol in raw and purtified Eudragit NE30D-matrices as a function of drug loading (matrix thickness = $50 \mu m$).

tained is also of note, being strongly dependent on drug loading. At the lowest drug loading of the raw Eudraeit NE30D we find a coefficient of variation (Cv) for the diffusivity of approx. 10%. which increases sharply with greater dmg loading. After reaching some 75Yo for 13% drug loading, the CV then falls to approx. 23% at the highest drug loading examined. The CVs for the diffusivities for the purified Eudragit NE30Dmatrices do not show this same dependence on drug loading. They are fairly constant in value. never being more than appron. 10-19/o for any of the drug loadings examined. The more scattered release orotiles and diffusivities obtained for the raw Eudragit NE30D-matrices are per**haps not surprising considering the evident uncontrolled nature of the phase separation of the contaminant within the polymer. Assuming that this contaminant is the stated surfactant, then the mechauism by which its presence leads to greater drug release rates may be related to improved** wetting of the matrix surface or greater water up**take into the matrix. It is. however, of note that the presence of such a small quantity (approx. 3%) ofthis cndogenous conlaminant has such a strong influence on the rate of drug release.**

Conclusions

Matrices prepared from thin films of Eudragit NE30D arc anisotropic systems due to the presence of a chase-separated. water-soluble contaminant that is incompatible with the polymer. This is in all probability an o-substituted nonyl phenol surfactant used during the manufacture ofthe polymer. The removal ofthis surfactant by **a simple aqueous extraction process yields an isotropic material. Although the rate of drug release (clenbuterol) is thereby reduced by almost two thirds in magnitude, the degree of scatter in both the release profiles and calculated diffusivities within the matrix is substantially improved.**

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